Neural Representation of a Rhythm Depends on Its Interval Ratio

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Rhythm is determined solely by the relationship between the time intervals of a series of events. Psychological studies have proposed two types of rhythm representation depending on the interval ratio of the rhythm: metrical and nonmetrical representation for rhythms formed with small integer ratios and noninteger ratios, respectively. We used functional magnetic resonance imaging to test whether there are two neural representations of rhythm depending on the interval ratio. The subjects performed a short-term memory task for a seven-tone rhythm sequence, which was formed with 1:2:4, 1:2:3, or 1:2:5:3.5 ratios. The brain activities during the memory delay period were measured and compared with those during the retention of a control tone sequence, which had constant intertone intervals. The results showed two patterns of brain activations: the left prefrontal and parietal areas and right cerebellar anterior lobe were active for 1:2:4 and 1:2:3 rhythms, whereas the right prefrontal, premotor, and parietal areas together with the bilateral cerebellar posterior lobe were active for 1:2:5:3.5 rhythm. Analysis on individual subjects revealed that these activation patterns depended on the ratio of the rhythms that were produced by the subjects rather than the ratio of the presented rhythms, suggesting that the observed activations reflected the internal representation of rhythm. These results suggested that there are two neural representations for rhythm depending on the interval ratio, which correspond to metrical and nonmetrical representations.

Key words: rhythm; short-term memory; metrical representation; nonmetrical representation; interval ratio; cerebellar anterior lobe; cerebellar posterior lobe; right hemisphere; left hemisphere

Rhythm is a flow of time, a series of time intervals marked off by the onsets of sensory or motor events, such as tones, flashes of lights, and steps in dances. Thus, rhythm is a supramodal entity that is determined solely by time information. The fact that we can recognize, discriminate, and reproduce a large number of rhythms suggests that individual rhythms can be internally represented, but its neural mechanism has not been well understood.

To date, most of the studies on neural processing of rhythm have been based on brain-damaged patients. Rhythm processing can be selectively impaired without any deficit in melody processing, suggesting the presence of a neural system specialized for rhythm (Peretz and Kolinsky, 1993). A number of studies have shown that the left cerebral hemisphere is involved in rhythm processing (Gordon and Bogen, 1974; Robinson and Solomon, 1974; Brust, 1980; Majlov, 1980; Polk and Kertesz, 1993), but others indicated that the processing of rhythm is not clearly lateralized (Peretz and Morais, 1980; Peretz, 1990). The variation in the location and size of the lesions hampered the precise localization of the responsible neural structures.

The inconsistency among these studies may be attributable to the fact that they used actual music as a test stimulus, which contains various types of rhythms. In this respect, previous psychological studies have identified an important constraint. Essens (1986) has shown that rhythms formed with ratios expressed as small integer values (1:2, 1:3, or 1:4) can be reproduced precisely, whereas rhythms related with larger values (1:5) or noninteger values (1:2.5 or 1:3.5) may be represented inaccurately. Based on the finding, Essens and Povel (1985) have proposed two modes of rhythm representation: metrical and nonmetrical representations. Metrical representation is to map a rhythm onto a temporal reference frame called an internal clock, by which the series of time intervals are metricaly related with one another. Rhythms formed with small integer ratios belong to this class. However, this strategy cannot be applied to the rhythms formed with large ratios or noninteger ratios. These rhythms are represented in a nonmetrical manner with which the series of time intervals are maintained as independent, unrelated values. This theory predicts that the neural correlates for rhythm processing may be composed of separate neural networks depending on the interval ratio of the rhythm.

In the present study, we have used functional magnetic resonance imaging (fMRI) to identify the neural representation of rhythm and tested whether there are two types of neural representation of rhythm, which correspond to metrical and nonmetrical representations. For this purpose, we used rhythms with their time intervals formed with 1:2:4, 1:2:3, and 1:2:5:3.5 ratios. We took advantage of fMRI to make selective measurement of brain activations during the memory delay period, which would reflect...
and Ls (e.g., SISLLI), we created 90 (6C2 with 1:2:4 (1:2:4 rhythm), 1:2:3 (1:2:3 rhythm), or 1:2.5:3.5 (1:2.5:3.5 rhythm). The seven tones were determined to comprise two short (S), two inter-
msec; and intensity, 95 dB. The six intervals marked off by the onsets of
the tone had the same frequency: 1 kHz; rise–fall time, 5 msec; plateau, 20
msec of the memory delay period, the scans were performed. During the
subsequent 5.2 sec period, the subjects reproduced the maintained se-
quence by pressing a button. The intertone time intervals of the tone
sequence was related with 1:2:4 ratio (1:2:4 rhythm), 1:2:3 ratio (1:2:3
rhythm), or 1:2.5:3.5 ratio (1: 2.5: 3.5 rhythm), and the total duration of
the sequence was varied across trials ranging from 3220 to 3780 msec. The
control sequence consisted of seven tones separated by a fixed intertone
interval.

the neural activation underlying the internal representation of rhythm.

MATERIALS AND METHODS

Subjects
Six normal subjects participated in the study (four males and two females; age 27–44; all right-handed). None of them were professional musicians. Informed consents were obtained from all the subjects before the study. The experimental protocol was approved by the ethics committee of the Communications Research Laboratory (Kobe, Japan).

Behavioral paradigm
A sequence of seven short tone bursts was presented to the subjects. Each tone had the same frequency: 1 kHz; rise–fall time, 5 msec; plateau, 20 msec; and intensity, 95 dB. The six intervals marked off by the onsets of the seven tones were determined to comprise two short (S), two inter-
mediate (I), and two long intervals (L), where the S, I, and L were related with 1:2:4 (1:2:4 rhythm), 1:2:3 (1:2:3 rhythm), or 1:2.5:3.5 (1:2.5:3.5 rhythm) ratios (Fig. 1). By taking all the possible orders of the two Ss, Is, and Ls (e.g., SISLLI), we created 90 (C2 × C2 × C2) sequences for each of the three types of the rhythm sequence. The duration of the rhythm sequence, as measured by the time interval from the onset of the first tone to the onset of the last tone, was randomly chosen from 3220, 3360, 3500, 3640, and 3780 msec.

The subjects were asked to hold the presented rhythm sequence in memory for a period of 10.8 sec and then to reproduce it by pressing a button with the right index finger. Instruction was given to keep the relative relations of the time intervals, as well as the absolute time intervals of the presented sequence.

The memory performance was assessed based on the reproduced sequence of button presses. Three measures were used for this purpose: order of the time intervals classified as S, I, and L; ratio of the S, I, and L; and duration of the sequence.

Order. The six time intervals of button pressing in the reproduced sequence were classified into two Ss, two Is, and two Ls. The order of the three classes of the time intervals (e.g., SISLLI) was compared with that of the presented tone sequence. If the order was different, the trial was regarded as an error and was eliminated from the following behavioral data analysis.

Ratio. Subsequently, we calculated the ratios of the button press intervals of the reproduced sequence. The mean of the two Is and the mean of the two Ls of the reproduced rhythm was respectively divided by the mean of the two Ss. The ideal ratios would be 2 and 4 for 1:2:4 rhythm, 2 and 3 for 1:2:3 rhythm, and 2.5 and 3.5 for 1:2.5:3.5 rhythm.

Duration. Another index for the accuracy of retention was the duration of the sequence. The regression analysis was performed on the duration of the reproduced sequence with that of the presented tone sequence. Ideally, these durations should be correlated linearly with a slope of 1.0 and an intercept of 0.

In the present study, we were interested in the rhythm, which can be expressed by the order and ratio. To eliminate the effects of the processes required for retention of absolute time intervals (duration), we also presented the control tone sequences (control), which were formed with seven tones separated by a constant interval. The total duration of the control sequence was randomly chosen from 3220, 3360, 3500, 3640, and 3780 msec to match that of the rhythm sequences. The comparison between the rhythm sequence (order + ratio + duration) and control sequence (duration) would selectively reveal the processes for retention of the rhythm (order + ratio).

fMRI data acquisition
Before the fMRI experiments, the subjects underwent practice sessions using 10 of the 90 sequences for each type of the rhythm sequence. For fMRI experiments, the rhythm sequences were chosen from the remain-
ing 80 sequences. Each sequence was used only once in each experiment.

An experiment comprised 120 trials, each of which is composed of the tone presentation period (4 sec), memory delay period (10.8 sec), fol-
lowed by the reproduction period (5.2 sec) (Fig. 1). The subjects fixated
their gaze at the center spot on the screen and were not allowed to move
any body parts or to vocalize the rhythms throughout the experiment, except for button presses during the reproduction period. The motion of the subject’s head was minimized by using a strap around the forehead, bite bar, and ear fixation blocks. In the tone presentation period, the tone sequence was delivered to a headphone through a pair of plastic tubes (length, 180 cm), and the subjects kept the sequence in memory during the memory delay period. At the end of the delay period, a brief high-pitched tone (frequency, 2 kHz; duration, 30 msec) was presented, which served as a cue to reproduce the presented tone sequence with button presses. The subjects had to reproduce the sequence within the 2.5 sec reproduction period, after which the next trial started.

For measurement of brain activation, we used Siemens (Erlagen, Germany) Vision 1.5 tesla scanner equipped with a circular polarized head coil. Fourteen slices of T2*-weighted gradient-echo planar images [repetition time (TR), 20 sec; echo time (TE), 66 msec; inversion time (TI), 300 msec; flip angle (FA), 90 degree] were collected within the 1.8 sec period at the end of the TR with the use of clustered volume acquisition (Edmister et al., 1999; Talavage et al., 1999). The images of

7 mm thickness [field of view (FOV), 220 × 220 mm; matrix, 128 × 128] were obtained parallel to the line connecting the anterior and posterior commissure (AC-PC line). The AC-PC line was determined based on the structure images obtained before the functional experiments (Turbo FLASH; TR, 2.8 sec; TE, 4 msec; TI, 300 msec; FA, 15 degree; matrix: 256 × 256; FOV, 256 × 256 mm; slice thickness, 1 mm). The timing of the scans was adjusted to start 9 sec after the end of the tone presentation period. Therefore, even if we take into account the delay of hemody-
namic response, the auditory-related activity should have almost re-
turned to the baseline level at the time of scans (Kwong et al., 1992; Buckner et al., 1996). Indeed, our supplementary experiments conducted by using 2.5 sec interscan interval (using TR of 2.5 sec) have shown that no significant activation to rest was present in the primary auditory area 7.5 sec after the cessation of the auditory stimuli (unpublished observation). In the present study, a series of the volume of brain images was acquired with long interscan intervals (20 sec). This sparse temporal sampling procedure (Hall et al., 1999) was advantageous in that the scan noise did not hamper the perceptual and encoding processes for the presented rhythm. In addition, no movements occurred during the period for at least 13.0 sec before the time of the scans.
Therefore, the magnetic resonance signals obtained would reflect the brain activations specifically associated with the retention of rhythms.

The following two sets of functional MRI experiments were performed, with their orders counterbalanced across the six subjects.

**Experiment 1.** The experiment comprised 120 task trials: 40 trials of 1:2:4 rhythm, 40 trials of 1:2:3 rhythm, and 40 trials of control. Ten trials for each type of the sequence were performed successively in a block. The blocks for the three types of the sequence were alternated in a counterbalanced order and were repeated for four times (e.g., 1:2:4 rhythm × 10 trials → 1:2:3 rhythm × 10 trials → control × 10 trials → 1:2:3 rhythm × 10 trials → 1:2:4 rhythm × 10 trials → control × 10 trials . . .). After two dummy scans, the task procedure was started while a series of 120 scans separated by a 20 sec interscan interval were performed for the 120 trials.

**fMRI data analysis**

Location of active areas. First, we performed a statistical parametric analysis on the functional images of the six subjects to identify the brain areas associated with retention of rhythms. For each experiment, the 120 functional images were realigned to the first image of each subject and were stereotaxically normalized into the T2 template of the standard brain using the software of SPM96 (Welcome Department of Cognitive Neurology, London, UK, http://www.fil.ion.ucl.ac.uk) (Friston et al., 1995). The images were then smoothed with a gaussian filter of 4.5 mm full-width half-maximum (FWHM). After application of temporal high-
pass filter (400 sec) to the time course of magnetic resonance signals, the confounding effect of variation in the global magnetic resonance signal intensity across the subjects was removed by ANCOVA. Subsequently, the time series of magnetic resonance signals was cross-correlated with a boxcar reference function derived from the alternation of the task blocks. The reference function was not shifted because of the usage of long TR (20 sec). For experiment 1, 1:2:4 and 1:2:3 rhythms were respectively compared with control. For experiment 2, 1:2:4 and 1:2.5:3.5 rhythms were respectively compared with control. A statistical parametric map of the t statistics was constituted from the resulting voxel values and was transformed to the unit normal distribution (SPM(Z), thresholded at 3.09). Taking the spatial extent of activation into consideration, a corrected p value of 0.05 was then used as a final threshold for significance.

Correlation of activation with memory performance: The above statistical parametric analysis provides the averaged brain activations for the six subjects. However, as will be shown in the behavioral data in Results, the memory performance differed across the subjects. Therefore, we also analyzed the brain activation pattern for each subject and correlated it with the memory performance. Instead of normalizing the anatomical structures into the Talairach space (Talairach and Tournoux, 1988), the foci of significantly increased activation was mapped onto the anatomical echo-planar images for each subject. After application of a gaussian filter with FWHM of 4.5 mm, the brain areas with significantly increased activities for rhythm compared with control were identified using a cross-correlation method (thresholded at cross-correlation coefficient of 0.35).

RESULTS

Behavioral data

The memory performance was assessed based on the order, ratio, and duration of the reproduced rhythms (examples shown in Fig. 2a). None of the six subjects showed error rates above 10%. The error rates were not significantly different between 1:2:3 and 1:2:4 rhythms (experiment 1, t(1,5) = -2.891; p < 0.05). In Figure 2b are shown the reproduced ratios for the three types of rhythms, respectively, for the six subjects. The mean ratio for the six subjects was 1:2.06:4.04 and 1:2.02:3.18, respectively, for 1:2:4 and 1:2:3 rhythms in experiment 1, and 1:2.01:4.00 and 1:2.33:3.69, respectively, for 1:2:4 and 1:2.5:3.5 rhythms in experiment 2. For 1:2.5:3.5 rhythm, the reproduced ratio for 2.5 was significantly smaller than 2.5 (t(1,5) = -3.40; p < 0.05), and that for 3.5 was significantly larger than 3.5 (t(1,5) = 2.84; p < 0.05). In contrast, the reproduced ratios for 1:2:4 and 1:2:3 rhythms were not significantly different from the original ratios except for that for 3 in 1:2:3 rhythm, which was larger than 3 (t(1,5) = 6.76; p < 0.05) [for further analysis, see below (Correlation of activation with memory performance)]. The duration of the sequence was maintained fairly precisely for all the rhythms; all the six subjects showed significant linear correlation (r^2 > 0.5) between the total duration of the reproduced sequence and that of the presented sequence. For all the subjects and tone sequences, the slopes and intercepts of the regression lines were close to 1.0 and 0, respectively (Fig. 2b).

fMRI data

Location of active areas

Comparisons of 1:2:4, 1:2:3, and 1:2.5:3.5 rhythms with control revealed brain areas associated with retention of the rhythm components (Table 1). 1:2:4 rhythm was tested twice (experiments 1 and 2), and activations in the left premotor and parietal areas were consistently observed, confirming the reproducibility of the finding (Fig. 3a). In addition, almost the same set of brain areas was active for 1:2:3 rhythm. In contrast, the activation pattern for 1:2.5:3.5 rhythm was completely different; the right prefrontal, premotor, and parietal areas were active. The anterior part of the right prefrontal cortex was active only for 1:2.5:3.5

<table>
<thead>
<tr>
<th>Comparison</th>
<th>Region</th>
<th>Area</th>
<th>Coordinates</th>
<th>Z score</th>
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<tbody>
<tr>
<td>Experiment 1</td>
<td>1:2:4 rhythm</td>
<td>Frontal</td>
<td>PMC</td>
<td>-52</td>
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<tr>
<td>- control</td>
<td>Parietal</td>
<td>IPS</td>
<td>-36</td>
<td>-42</td>
</tr>
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<td></td>
<td>Cerebellar</td>
<td>Anterior</td>
<td>16</td>
<td>-48</td>
</tr>
<tr>
<td>1:2:3 rhythm</td>
<td>Frontal</td>
<td>PMC</td>
<td>-46</td>
<td>10</td>
</tr>
<tr>
<td>- control</td>
<td>Parietal</td>
<td>IPS</td>
<td>-52</td>
<td>-30</td>
</tr>
<tr>
<td></td>
<td>Cerebellar</td>
<td>Anterior</td>
<td>16</td>
<td>-52</td>
</tr>
<tr>
<td></td>
<td>Cerebellar</td>
<td>Posterior</td>
<td>34</td>
<td>-66</td>
</tr>
<tr>
<td>Experiment 2</td>
<td>1:2:4 rhythm</td>
<td>Frontal</td>
<td>PMC</td>
<td>-42</td>
</tr>
<tr>
<td>- control</td>
<td>Parietal</td>
<td>IPS</td>
<td>-56</td>
<td>16</td>
</tr>
<tr>
<td></td>
<td>Cerebellar</td>
<td>Anterior</td>
<td>36</td>
<td>-34</td>
</tr>
<tr>
<td>1:2.5:3.5 rhythm</td>
<td>Frontal</td>
<td>PFC</td>
<td>18</td>
<td>-52</td>
</tr>
<tr>
<td>- control</td>
<td>Parietal</td>
<td>IPS</td>
<td>42</td>
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<td>-32</td>
<td>-60</td>
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PMC, Premotor cortex; IPS, intraparietal sulcus; Anterior, anterior lobe; Posterior, posterior lobe; PFC, prefrontal cortex; STG, superior temporal gyrus.
rhythm but not for 1:2:4 and 1:2:3 rhythms (Fig. 3b). The analysis of individual subjects showed that this prefrontal activation focus was located within the anterior part of the middle frontal gyrus close to the inferior frontal gyrus (Fig. 4b, blue circle). Additional activation foci were found in the cerebellum; the right anterior lobe was active for 1:2:4 and 1:2:3 rhythms but not for 1:2.5:3.5 rhythm, whereas the bilateral cerebellar posterior lobe was active for 1:2.5:3.5 rhythm but not for 1:2:4 rhythm (Fig. 3b). Only the right posterior lobe was active for 1:2:3 rhythm. Individual subject analysis showed that the activation foci in the cerebellar anterior lobe were located in the quadrangular lobule [corresponding to hemispheric lobule IV (HIV)–HV] (Fig. 4a, pink circle), whereas the foci in the posterior lobe were located within the simplex lobule and the superior semilunar lobule of the cerebellum (corresponding to HVI–crus I of HVIIa) (Fig. 4b, green circle).

Correlation of activation with memory performance

As shown in Figure 2b, the memory performance for 1:2:4 and 1:2:3 rhythms was not different across the six subjects, whereas that for 1:2.5:3.5 rhythm considerably differed with respect to its reproduced ratios. The reproduced ratio for 2.5 ranged from 2.15 to 2.45, and that for 3.5 ranged from 3.52 to 3.92 among the six subjects. To further analyze the performance of each subject, we plotted the reproduced ratios for the 40 trials for 1:2:4 and 1:2.5:3.5 rhythms (experiment 2) in histograms and rasters (Fig. 4). Histograms for 1:2:4 rhythm revealed two peaks of the repro-
were consistently active, except for subject 2. In subjects 5 and 6, the prefrontal cortex (the right side was active in subjects 1–4, whereas the left side was active in subjects 5 and 6). The cerebellar posterior lobe (pink circle) was bilaterally active in subjects 1–3, whereas the right cerebellar anterior lobe (pink circle) was active in subjects 4–6.

DISCUSSION

Two modes of neural representation for rhythm

Earlier psychological studies have, based solely on the behavioral data, proposed two types of rhythm representation depending on the interval ratio of the rhythm (Essens, 1986). The aim of the present study was to test whether these metrical and nonmetrical representations recruit different sets of neural network. To elucidate the internal representation of rhythm, we used a short-term memory task in which the subjects maintained a rhythm internally during the delay period. However, MRI scans themselves produce rhythmic noise and would have severely disturbed the experiment if they had been performed during the tone presentation period or memory delay period. To eliminate the interactive effects of the scan noise on the perceptual and memory processes, we used a sparse temporal sampling procedure (Hall et al., 1999) with clustered volume acquisition (Edmister et al., 1999; Talavage et al., 1999) so that no scan was performed during the delay period. The dependence of brain activation patterns on the reproduced rhythm rather than the ratio of the presented rhythms.

The present study used three types of rhythm whose interval ratios were expressed as 1:2:4, 1:2:3, and 1:2.5:3.5, respectively. According to the theory proposed in the psychological literature (Povel, 1984; Essens and Povel, 1985; Povel and Essens, 1985), the former two rhythms are represented in a metrical form, whereas the latter one is represented in a nonmetrical form. The behavioral data in the present study were consistent with this idea; the reproduction of 1:2:4 and 1:2:3 rhythms was precise, whereas that of 1:2.5:3.5 rhythm was inaccurate, especially in its reproduced ratio. Interestingly, some subjects unintentionally transformed the 1:2.5:3.5 rhythm into 1:2:4 rhythm, which was consistent with the finding of Essens (1986). It has also been shown that voluntary motor behaviors tended to fall into a time sequence related with...
related to explicit temporal representation (Ivry et al., 1988; Ivry, 1993; Jupe et al., 1996; Mangels et al., 1998; Sakai et al., 1998). The cerebellar posterior lobe activation in the present study may reflect the retention of a series of time intervals for 1:2:5:3:5 rhythm. The posterior lobe activation was absent for 1:2:4 rhythm, perhaps because the time intervals of this rhythm were metronomically related and encoding of individual time intervals was not necessary.

Right versus left hemispheric predominance

We found that metrical representation for 1:2:4 or 1:2:3 rhythms was predominantly associated with left hemispheric activation, whereas the nonmetrical representation for 1:2:5:3:5 rhythm was associated with right hemispheric activation. Previous clinical studies have shown that rhythm deficits were found after left hemispheric lesions, especially when the left premotor and parietal areas were damaged (Brust, 1980; Mavlov, 1980; Polk and Kertesz, 1993). Considering that most of the music, especially from western countries, was metronomically related (Palmer and Kelly, 1992; Palmer, 1997), the present finding showing activations in the left premotor and parietal areas for metrical rhythms is consistent with these clinical studies. In contrast, the right hemispheric activations for rhythms related with complex ratios are consistent with an earlier study of Roland et al. (1981), which showed predominant right hemispheric activations in discrimination of two rhythm patterns related with complex ratios. The right frontoparietal areas may be involved in memory of time intervals (Harrington et al., 1998), which is necessary for the nonmetrical rhythm representation. Thus, the present results indicate that the processing of rhythm is not confined to one cerebral hemisphere, as Peretz (1990) has suggested.

Although we used auditory stimuli for presenting rhythms, the temporal lobes did not show significant activation; only a small portion on the right side was active for 1:2:5:3:5 rhythm. The frontoparietal network active in the present study would, thus, reflect the supramodal mechanism for rhythm processing, as suggested by Mavlov (1980). Indeed, it was shown that the ability in rhythm processing was preserved, even after the lesions in the temporal lobe (Peretz and Kolinsky, 1993; Peretz, 1996).

To summarize, we have shown that there are two modes of neural representation for rhythm. Their selection depends on the interval ratios of the rhythm or, more precisely, on the strategy used for encoding the rhythm, metrical or nonmetrical. Nonmetrical strategy may require explicit processing for the individual time intervals, whereas metrical strategy may operate automatically, and possibly implicitly, to allow hierarchical encoding of the whole rhythm. In this regard, the right and left hemispheric dissociation observed in the nonmetrical and metrical rhythm processing may be closely related to the finding of Hazeltine et al. (1997), who showed a similar hemispheric dissociation between explicit and implicit motor sequence learning.

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