Gating Properties of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 Peripheral Nerve Sodium Channels

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Several distinct components of voltage-gated sodium current have been recorded from native dorsal root ganglion (DRG) neurons that display differences in gating and pharmacology. This study compares the electrophysiological properties of two peripheral nerve sodium channels that are expressed selectively in DRG neurons (Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8). Recombinant Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels were coexpressed with the auxiliary β\textsubscript{1} subunit in Xenopus oocytes. In this system coexpression of the β\textsubscript{1} subunit with Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 channels results in more rapid inactivation, a shift in midpoints of steady-state activation and inactivation to more hyperpolarizing potentials, and an acceleration of recovery from inactivation. The coinjection of β\textsubscript{1} subunit also significantly increases the expression of Na\textsubscript{v}1.8 by sixfold but has no effect on the expression of Na\textsubscript{v}1.7. In addition, a great percentage of Na\textsubscript{v}1.8+β\textsubscript{1} channels is observed to enter rapidly into the slow inactivated states, in contrast to Nav1.7+β\textsubscript{1} channels. Consequently, the rapid entry into slow inactivation is believed to cause a frequency-dependent reduction of Na\textsubscript{v}1.8+β\textsubscript{1} channel amplitudes, seen during repetitive pulsing between 1 and 2 Hz. However, at higher frequencies (>20 Hz) Na\textsubscript{v}1.8+β\textsubscript{1} channels reach a steady state to ~42% of total current. The presence of this steady-state sodium channel activity, coupled with the high activation threshold (V\textsubscript{a5} = −3.3 mV) of Na\textsubscript{v}1.8+β\textsubscript{1}, could enable the nociceptive fibers to fire spontaneously after nerve injury.

Key words: Na\textsubscript{v}1.7; Na\textsubscript{v}1.8; peripheral nerve sodium channels; expression; dorsal root ganglion; nociception; Xenopus oocytes

Voltage-gated sodium channels play an important role in the generation and propagation of action potentials in excitable tissues. At least 10 distinct isoforms of the sodium channel have been identified in brain and neuronal and striated muscle that differ in primary structure, pharmacology, permeation, and gating (Goldin et al., 2000). A major determinant of the functional difference among these isoforms is inherent in the α subunit that determines the selectivity and gating properties of these channels (Goldin et al., 1986). However, in vivo, most sodium channels are associated with auxiliary subunits (β1–β3), that are known to modulate gating and levels of expression (Isom et al., 1992; Morgan et al., 2000). For instance, the inactivation of rat brain sodium channels (Na\textsubscript{v}1.2) is accelerated and the gating is shifted toward more hyperpolarized voltages when coexpressed with the β1 subunit (O’Leary, 1998). Similar findings have been reported for the skeletal muscle sodium channels, indicating that these auxiliary subunits play an important role in determining the gating properties of these tetrodotoxin-sensitive sodium channels (Bennett et al., 1993; Wallner et al., 1993; Yang et al., 1993). In contrast, the tetrodotoxin-resistant cardiac sodium channels display only subtle changes in gating when coexpressed with the β1 subunit (Makita et al., 1994; Nuss et al., 1995; Makielksi et al., 1996).

In addition to changes in gating, the β1 subunit is known to enhance the expression of many sodium channels (Chahine et al., 1994; Nuss et al., 1995). The expression of functional Na\textsubscript{v}1.2 brain sodium channels increases by 2.5-fold when coexpressed with the β1 subunit (Isom et al., 1992). The β1 subunit also is believed to contribute to clustering and remodeling of sodium channels at the neuromuscular junction (Blackburn-Munro and Fleetwood-Walker, 1999; Caldwell, 2000). Such regulations may have important consequences for neuronal tissues such as dorsal root ganglion cells (DRG) in which multiple isoforms of the sodium channels are expressed in the same cell (Akopian et al., 1996; Black et al., 1996; Sangameswaran et al., 1996, 1997; Toledo-Aral et al., 1997).

At least five distinct components of voltage-gated sodium channels have been recorded from DRG neurons (Rush et al., 1998). Two components predominate in the small nociceptive neurons: a rapidly inactivating TTX-S current and a slowly inactivating TTX-R current (Kostyuk et al., 1981; Roy and Narahashi, 1992; Elliott and Elliott, 1993; Black et al., 1996). Recently, two peripheral nerve sodium channels have been isolated from the human and rat DRG (Sangameswaran et al., 1996; Toledo-Aral et al., 1997). Na\textsubscript{v}1.7 (PN1) is a TTX-S rapidly inactivating channel that is expressed widely in DRG neurons (Sangameswaran et al., 1997; Toledo-Aral et al., 1997). Na\textsubscript{v}1.8 (PN3) is a TTX-R slowly inactivating channel that is expressed predominantly in the small nociceptive C-type pain fibers (Akopian et al., 1996; Sangameswaran et al., 1996). Recently, a novel sodium channel Na\textsubscript{v}1.9 (Na9) was cloned and also may contribute to the TTX-R

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current of small DRG neurons (Dib-Haj et al., 1998). Differential expression of the Na\textsubscript{v}1.7, Na\textsubscript{v}1.8, Na\textsubscript{v}1.9, and several of the brain sodium channels (Na\textsubscript{v}1.1, Na\textsubscript{v}1.2, Na\textsubscript{v}1.3) contributes to the unique electrical excitability of nociceptive neurons (Porreca et al., 1999). Changes in the expression levels of these channels have been implicated in the alterations of neuronal excitability associated with acute and chronic pain syndromes (Rizzo et al., 1995; Gold et al., 1996).

The transcript encoding for the β\textsubscript{1} subunit is present in both large and small DRG neurons (Oh et al., 1995; Coward et al., 2001). However, previous studies indicate that the β\textsubscript{1} subunit does not alter the gating of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels (Sangameswaran et al., 1996, 1997). This finding is inconsistent with studies showing that, if not all, sodium channels are modulated by the β\textsubscript{1} subunit (Chahine et al., 1994; Isom et al., 1995). In addition, a recent study has shown that the inactivation of heterologously expressed Na\textsubscript{v}1.7 channels is accelerated when coexpressed with the β\textsubscript{1} subunit (Schwerbakto et al., 1999). Currently, little is known about the modulatory effects of the β\textsubscript{1} subunit on Na\textsubscript{v}1.8 channels. In this study the α subunits of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels were expressed in Xenopus oocytes, and the kinetics and voltage sensitivity were compared with and without the coexpressed β\textsubscript{1} subunit. The Xenopus oocyte system of expression was used in this study especially because the Na\textsubscript{v}1.8 sodium channels expressed, with or without the β\textsubscript{1} subunit, poorly in the mammalian cell systems (tsA201 and CHO cell line). Coexpression of Na\textsubscript{v}1.7 with the β\textsubscript{1} subunit in Xenopus oocytes causes a hyperpolarizing shift in gating and increases the rates of inactivation and recovery from inactivation. For Na\textsubscript{v}1.8 channels the β\textsubscript{1} subunit produces similar changes in the voltage sensitivity and kinetics of gating but, in addition, significantly increases the expression levels of these channels. The β\textsubscript{1} subunit modulates the gating of both the Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels. Differences in the gating and expression of these sodium channels are likely to have important consequences for the generation and propagation of action potentials in nociceptive neurons.

MATERIALS AND METHODS

Molecular biology: Construction of full-length rat α subunit Na\textsubscript{v}1.8 cDNA. Total RNA was isolated from Sprague Dawley rat DRG by using the Trizol reagent (Life Technologies, Burlington, Ontario, Canada). Rat DRG RNA was reverse transcribed (RT) with the use of Superscript (Life Technologies) and random primers to create a cDNA library. Total DRG RNA (5 μg) was heat denatured at 70°C for 10 min, followed by rapid cooling on ice. Reverse transcription was performed with 10 mM deoxynucleotide triphosphate (dNTPs), 0.1 mM dithiothreitol, and 50 ng/μl random primers in a total volume of 20 μl. The mixture was added to the denatured total RNA and incubated at 25°C for 5 min. Superscript (1 U: Life Technologies) was added, and the reactions were incubated at 37°C for 10 min and then at 42°C for 1 hr. Incubating the sample at 70°C for 15 min then terminated the reaction. Finally, the sample was incubated at 37°C with RNaseH for 20 min to remove the total RNA. The RT product was used directly for PCR.

Rat Na\textsubscript{v}1.8 α subunit-specific primers were designed to amplify 2–4 kb segments within the coding region of the gene. Primer sequences were based on the published sequence (GenBank number U53833). The rat Na\textsubscript{v}1.8 α subunit gene was amplified from the first ATG start codon; the 5’ untranslated region (UTR) sequence was not included in the clone. Primer set 1 (1–4247 bp) consisted of the following: primer position 1, sense, GAAAGATGAGAAGATGAGCTCCCC; primer position 2, antisense, GAAGTTCAAGCTGAAGAGGCCAC. Primer set 2 (3875–5940 bp) consisted of the following: primer position 3875, sense, GTCTCTGTCGTCTGCTCTTCTT; primer position 3940, antisense, GTCTGAGTCTCCTACTGAGTCCAG.

PCR was performed in a 50 μl reaction mixture containing PCR buffer, 10 mM dNTPs, 100 ng/μl of the specific set of primers, 2 μl of the rat DRG cDNA, and 1 U of Pfu-turbo Polymerase (Stratagene, La Jolla, CA). Amplification was performed with the following cycling: 3 min at 94°C, 1 min at 94°C, 1 min at 60°C, and then 2 min/kb at 55°C repeated for a total of 30 cycles. PCR amplicons were subcloned, and the full-length Na\textsubscript{v}1.8 was constructed in the pCRII-Tope vector (Life Technologies). Full-length Na\textsubscript{v}1.8 coding sequence was confirmed by fluorescent deoxyrobose terminus sequencing at the automated sequencing facility of Laval University, Sainte-Foy, Québec. The final Na\textsubscript{v}1.8 construct was subcloned into pSP64T (β-globin), suitable for high-yield transcription of complementary RNA (cRNA).

The rat Na\textsubscript{v}1.7 α subunit voltage-gated sodium channel, cloned into the pCDNA3a vector, was kindly donated by Gay Mandel (Department of Neurobiology, State University of New York, NY). cRNA was prepared by the T7 (pCDNA3a) or SP6 (pSP64T) mMessage mMACHINE kit (Ambion, TX).

Expression and electrophysiology in Xenopus oocytes. Xenopus laevis females were anesthetized with 1.5 mg/ml tricaine (Sigma, Oakville, Ontario, Canada), and two or three ovarian lobes were removed surgically. Follicular cells surrounding the oocytes were removed by incubation at 22°C for 2.5 hr in calcium-free oocyte medium [containing (in mM) 82.5 NaCl, 2.5 KCl, 1 MgCl\textsubscript{2}, and 5 HEPES, pH 7.6] containing 2 mg/ml collagenase (Sigma). The oocytes were washed first in calcium-free medium and then with a 50% Leibowitz’s L-15 medium (Life Technologies) enriched with 15 mM HEPES and 5 mM l-glutamine, supplemented with 10 mg/ml gentamycin, pH 7.6. The oocytes were stored in this medium until further use. Stage VI–V oocytes were selected and microinjected with 50 nl of cRNA encoding for the α subunit of Na\textsubscript{v}1.7 or Na\textsubscript{v}1.8. The amounts of Na\textsubscript{v}1.7 cRNA injected in the oocytes were less compared with the amounts injected for Na\textsubscript{v}1.8 channels. This is because the Na\textsubscript{v}1.7 channels express more readily compared with Na\textsubscript{v}1.8 channels. Sets of oocytes also were coinjected in parallel with equal ratios of Na\textsubscript{v}1.7 and β\textsubscript{1} subunit or Na\textsubscript{v}1.8 α subunit and β\textsubscript{1} subunit.

Oocytes were stored at 18°C and used for experiments depending on the level of expression of each channel type. Parallel sets of experiments with the rat skeletal muscle sodium channel (μ1) were used to confirm the functional association of the α and β\textsubscript{1} subunits in oocytes (data not shown).

The whole-cell sodium current from cRNA-injected oocytes was measured via two-microelectrode voltage clamp at room temperature ≈22°C. The oocytes were impaled with <2 MΩ electrodes containing 3 mM KCl and were voltage clamped with an OC-725 oocyte clamp (Warner Instruments, Hamden, CT). The bath Ringer’s solution contained (in mM) 90 NaCl, 2 KCl, 1.8 CaCl\textsubscript{2}, 2 MgCl\textsubscript{2}, and 5 HEPES, pH 7.6. Currents were filtered at 1.5 kHz with an eight-pole Bessel filter and were sampled at 10 kHz. Data were acquired and analyzed with pClamp software v7 (Axon Instruments, Foster City, CA).

The voltage dependence of activation was determined by eliciting depolarizing pulses from a holding potential of −100 mV to potentials ranging from −80 to +60 mV in 10 mV increments. Current activation curves of the channels were plotted following the Boltzmann equation: \( G_{Na}/G_{Na_{max}} = 1/(1 + (exp(V_{0.5} – V_k)/k)) \), for which the \( G_{Na} \) (conductance) values for each clamped oocyte were determined by dividing the peak sodium current by the driving force (\( V_{m} – E_{Na} \)). The reversal potential (\( E_{Na} \)) for each oocyte expressing the channels was estimated by extrapolating the linear ascending segment of decay gradient, between 0 and +20 mV for Na\textsubscript{v}1.7 and between +20 and +40 mV for Na\textsubscript{v}1.8, of an I–V curve to the voltage axis. \( V_{0.5} \) is the voltage at which the channels are half-maximally activated, and \( k \) is the slope factor. Conductance versus voltage data were fit with a two-state Boltzmann equation.

Statistical analysis. Results of representative measures were expressed as means ± SEM. The means of paired groups of oocytes injected with the α subunit of Na\textsubscript{v}1.7 or Na\textsubscript{v}1.8 were compared directly with those of oocytes coexpressed with the α and β\textsubscript{1} subunits; a repeated measurement ANOVA was performed. The homogeneity of correlation between repeated measures was tested with the sphericity test. The results were considered significant if p values were ≤0.05. The data were analyzed by the statistical package program SAS (SAS Institute, Cary, NC).

RESULTS

Effects of β\textsubscript{1} subunit on the expression of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels

The α subunit of the peripheral nerve sodium channel Na\textsubscript{v}1.8 was cloned from the DRG of Sprague Dawley rats via RT-PCR (see Materials and Methods). The fidelity of the Na\textsubscript{v}1.8 clone was...
verified by comparing its sequence with the published sequence (ACC number U53833). cRNA of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 clones was microinjected into stage IV–V *Xenopus* oocytes. The whole-cell sodium currents of oocytes expressing either the Na\textsubscript{v}1.7 or Na\textsubscript{v}1.8 sodium channel with and without the β\textsubscript{1} subunit. Currents were elicited by depolarizing steps between −50 and +65 mV in 5 mV increments from a holding potential of −100 mV (see inset). A, Whole-cell Na\textsubscript{v}1.7 currents measured in the absence (left) and presence (right) of the β\textsubscript{1} subunit. B, Na\textsubscript{v}1.8 sodium currents expressed without (left) and with (right) the β\textsubscript{1} subunit. Dashed lines are the zero current levels.

**Figure 1.** Effects of the β\textsubscript{1} subunit on Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels heterologously expressed in *Xenopus* oocytes. The data show the whole-cell sodium currents of oocytes expressing either the Na\textsubscript{v}1.7 or Na\textsubscript{v}1.8 sodium channel with and without the β\textsubscript{1} subunit. Currents were elicited by depolarizing steps between −50 and +65 mV in 5 mV increments from a holding potential of −100 mV. Currents were measured in the absence (left) and presence (right) of the β\textsubscript{1} subunit.

**Figure 2.** Effects of the β\textsubscript{1} subunit on the expression of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels. Shown are the whole-cell sodium currents of paired groups of oocytes expressing either the Na\textsubscript{v}1.7 or Na\textsubscript{v}1.8 channels with or without the β\textsubscript{1} subunit. Na\textsubscript{v}1.7 peak currents at −20 mV were measured from oocytes expressing Na\textsubscript{v}1.7 or Na\textsubscript{v}1.7+β\textsubscript{1} after 24 hr of incubation. For Na\textsubscript{v}1.8 channels, the peak currents measured at +20 mV were compared 6 d after cRNA injection. For Na\textsubscript{v}1.8 channels, the peak currents measured at +20 mV were compared 6 d after cRNA injection. Peak amplitude recorded 3 d after injection for Na\textsubscript{v}1.8 channels was small (38.1 ± 2.8 nA; n = 3), whereas the coexpression increased expression by 17-fold (695 ± 117 nA; n = 5; data not shown). The β\textsubscript{1} subunit significantly increased (p < 0.05) the currents of Na\textsubscript{v}1.8 (n = 7), but not the Na\textsubscript{v}1.7 (n = 6), sodium channels (p < 0.05). The holding potential was −100 mV.
Effects of the β1 subunit on kinetics of current decay of Na\textsubscript{1.7} and Na\textsubscript{1.8} channels

In addition to changes in expression levels, the β1 subunit also alters the gating properties of these channels. In the absence of the β1 subunit, the inactivation of Na\textsubscript{1.7} is slow, resulting in considerable residual current near the end of the 20 msec depolarizing pulse (Figs. 1A, 3A). When coexpressed with the β1 subunit, the inactivation is more rapid and the currents are inactivated completely during the 20 msec depolarization (Figs. 1A, 3A). The β1 subunit also accelerates the inactivation of Na\textsubscript{1.8} but to a much lesser extent than that observed for Na\textsubscript{1.7} (Fig. 3B). To quantitate the changes in decay rate, we fit the currents with single exponentials. At −20 mV the decay of Na\textsubscript{1.7} currents has a time constant (τ\textsubscript{d}) of 19.8 ± 3.6 msec (n = 6) and 1.8 ± 0.2 msec (n = 6) for Nav1.7+β1. Coexpression with the β1 subunit significantly accelerates the inactivation of Na\textsubscript{1.7} current (p < 0.05). Coexpression of Na\textsubscript{1.8} with the β1 subunit also significantly reduces τ\textsubscript{d} (p < 0.05). At +20 mV, Na\textsubscript{1.8} and Nav1.8+β1 currents decay with time constants of 4.3 ± 0.2 msec (n = 6) versus 2.6 ± 0.1 msec (n = 6), respectively (Fig. 3B). The β1 subunit reduces the τ\textsubscript{d} of Na\textsubscript{1.7} and Na\textsubscript{1.8} sodium currents over a wide range of voltages (Fig. 4A,B). Overall, the data indicate that coexpression with the β1 subunit accelerates the inactivation of both Na\textsubscript{1.7} and Na\textsubscript{1.8} sodium channels.

Effects of the β1 subunit on the gating of Na\textsubscript{1.7} and Na\textsubscript{1.8} channels

The effect of the β1 subunit on the voltage sensitivity of activation was investigated also. The relative conductance was determined from families of sodium currents similar to those shown in Figure 1 (see Materials and Methods). The normalized conductance of Na\textsubscript{1.7} and Na\textsubscript{1.8} channels with and without the β1 subunit was plotted versus voltage (Fig. 5A,B). The smooth curves are fits to a Boltzmann function with midpoint (V\textsubscript{0.5}) and slope factors (k) of −22.2 ± 2.7 and 5.4 ± 0.4 mV (n = 10) for Na\textsubscript{1.7} and of −27.7 ± 1.3 mV (V\textsubscript{0.5}) and 3.7 ± 0.2 mV (k; n = 11) for Na\textsubscript{1.7}+β1 (Fig. 5A). Coexpression with the β1 subunit causes a significant −5.3 mV shift in the midpoint of steady-state activation (p < 0.05). For Na\textsubscript{1.8} the V\textsubscript{0.5} and k values are 4.7 ± 0.7 and 6.8 ± 0.1 mV (n = 8) and −3.3 ± 0.9 mV (V\textsubscript{0.5}) and 5.5 ± 0.1 mV (k) for Na\textsubscript{1.8}+β1 (n = 9) (Fig. 5B). The coexpression with the β1 subunit causes a significant −8 mV shift in midpoint (p < 0.05) and reduces the slope factor, consistent with an increase in the voltage sensitivity of the Na\textsubscript{1.8} sodium channels. Overall, the β1 subunit causes hyperpolarizing shifts in the midpoints of activation and increases the voltage sensitivity of both Na\textsubscript{1.7} and Na\textsubscript{1.8} channels.

The effect of the β1 subunit on the steady-state inactivation was investigated also. Steady-state inactivation was measured by using 500 msec conditioning pulses to voltages between −110 and +30 mV. The fraction of available current was determined by using standard test pulses, and the normalized currents were plotted versus the conditioning voltage (Fig. 5A,B). The smooth curves are Boltzmann fits with midpoints (V\textsubscript{0.5}) and slope factors (k) of −68.2 ± 0.4 and 6.4 ± 0.5 mV (n = 4) for Na\textsubscript{1.7} and of −69.8 ± 0.3 mV (V\textsubscript{0.5}) and 3.9 ± 0.2 mV (k; n = 4) for Na\textsubscript{1.7}+β1 (Fig. 5A). The β1 subunit only slightly alters the midpoint but signifi-
coexpression with the $\beta_1$ subunit also causes hyperpolarizing shifts in the midpoints and increases the voltage sensitivity of steady-state inactivation of both the Na$_{1.7}$ and Na$_{1.8}$ sodium channels.

**Effects of $\beta_1$ subunit on recovery from fast inactivation**

Effects of the $\beta_1$ subunit on the recovery from fast inactivation were examined with a standard two-pulse protocol consisting of a depolarizing pulse to $-20$ mV (Na$_{1.7}$) or $+20$ mV (Na$_{1.8}$) for 40 msec to inactivate the channels, followed by a variable duration (1 msec to 5 sec) step to $-100$ mV to promote recovery. The availability of the channels after the end of the recovery interval was assessed with a standard test pulse, and the normalized currents were plotted versus the recovery interval. Figure 5, C and D, illustrates the time dependence of recovery from fast inactivation of Na$_{1.7}$ and Na$_{1.8}$ channels. In the absence of the $\beta_1$ subunit the recovery of Na$_{1.7}$ is bi-exponential, with fast and slow time constants of $19.6 \pm 0.8$ msec ($\tau_S$) and $933.4 \pm 54.6$ msec ($\tau_C; n = 7$) (Fig. 5C). Coexpression with the $\beta_1$ subunit substantially increases the recovery kinetics and causes the channels to recover fully from inactivation. The fast and slow recovery time constants of Na$_{1.7} + \beta_1$ are $6.6 \pm 0.6$ msec ($\tau_S$) and $53.2 \pm 12.7$ msec ($\tau_C; n = 7$). The more complete recovery of Na$_{1.7} + \beta_1$ channels can be attributed primarily to a 2.9-fold increase in the fraction of channels recovering with the rapid time constant.

In contrast, the recovery from fast inactivation of Na$_{1.8}$ is slow in comparison with Na$_{1.7}$, and fitting the data required the sum of three exponentials to describe the time course accurately. The recovery time constants of Na$_{1.8}$ channels are $9.9 \pm 1.8$ msec ($\tau_S$), $168.6 \pm 52.2$ msec ($\tau_I$), and $787.6 \pm 112.6$ msec ($\tau_C; n = 5$) (Fig. 5D). The recovery time constants of Na$_{1.8} + \beta_1$ are $2.0 \pm 0.3$ msec ($\tau_S$), $243.8 \pm 85.4$ msec ($\tau_I$), and $1070.1 \pm 59.0$ msec ($\tau_C; n = 4$) (Fig. 5D). The $\beta_1$ subunit reduces $\tau_S$ but increases $\tau_C$, consistent with differential effects on the fast and slow components of Na$_{1.8}$ recovery from inactivation. Interestingly, the slow component of recovery ($\tau_C$) is observed only with Na$_{1.8}$ channels and is enhanced with the $\beta_1$ subunit. This suggests that the Nav1.8+\beta$_1$ channels may enter readily into a slow inactivated state during the short (40 msec) depolarizing prepulses used to inactivate the channels in these experiments. To test this hypothesis, we compared the development of slow inactivation of Na$_{1.7} + \beta_1$ and Na$_{1.8} + \beta_1$ channels (Fig. 6). The onset of slow inactivation was measured by depolarizing the oocytes to either $-20$ mV (Na$_{1.7} + \beta_1$) or $+20$ mV (Na$_{1.8} + \beta_1$) for a variable interval (0 msec to 10 sec) to induce inactivation. Then the voltage was returned to $-100$ mV for 20 msec to allow for the recovery of fast-inactivated channels ($\tau_r = 6.6$ msec for Na$_{1.7} + \beta_1$; $\tau_r = 2$ msec for Na$_{1.8} + \beta_1$) before a standard test pulse to assay availability was applied. The amplitudes of the test currents were normalized to controls and plotted versus the prepulse interval. In these experiments the progressive

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**Figure 4.** The $\beta_1$ subunit accelerates the inactivation of Na$_{1.7}$ and Na$_{1.8}$ channels. The decay of the Na$_{1.7}$ and Na$_{1.8}$ sodium currents (Fig. 1) was fit to an exponential function, and the time constants were plotted versus the test voltage: $I = A_i \cdot \exp (-t/\tau_i) + C$, where $I$ is the current, $A_i$ is the percentage of channels inactivating with time constant $\tau_i$, $t$ is time, and $C$ is the steady-state asymptote. The data are the means ± SEM of $n = 6$ for Na$_{1.7}$ and Na$_{1.7} + \beta_1$ and $n = 6$ for Na$_{1.8}$ and Na$_{1.8} + \beta_1$ channels. A, The inactivation time constants of Na$_{1.7}$ (filled squares) and Na$_{1.7} + \beta_1$ (open squares) plotted versus voltage. B, The time constants of Na$_{1.8}$ (filled circles) and Na$_{1.8} + \beta_1$ (open circles) plotted versus voltage.

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The recovery from inactivation of Na$_{1.8} + \beta_1$ displays a slow component that is not observed with Na$_{1.7} + \beta_1$ (Fig. 5C,D). The data suggest that, in addition to the fast and intermediate components of inactivation observed for both channels, Na$_{1.8} + \beta_1$ channels enter into a slow inactivated state during the short depolarizing prepulses used to inactivate the channels in these experiments. To test this hypothesis, we compared the development of slow inactivation of Na$_{1.7} + \beta_1$ and Na$_{1.8} + \beta_1$ channels (Fig. 6). The onset of slow inactivation was measured by depolarizing the oocytes to either $-20$ mV (Na$_{1.7} + \beta_1$) or $+20$ mV (Na$_{1.8} + \beta_1$) for a variable interval (0 msec to 10 sec) to induce inactivation. Then the voltage was returned to $-100$ mV for 20 msec to allow for the recovery of fast-inactivated channels ($\tau_r = 6.6$ msec for Na$_{1.7} + \beta_1$; $\tau_r = 2$ msec for Na$_{1.8} + \beta_1$) before a standard test pulse to assay availability was applied. The amplitudes of the test currents were normalized to controls and plotted versus the prepulse interval. In these experiments the progressive

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The inactivation time constants of Na$_{1.7}$ ($\tau_i$) is time, and $C$ is the steady-state asymptote. The data are the means ± SEM of $n = 6$ for Na$_{1.7}$ and Na$_{1.7} + \beta_1$ and $n = 6$ for Na$_{1.8}$ and Na$_{1.8} + \beta_1$ channels. A, The inactivation time constants of Na$_{1.7}$ (filled squares) and Na$_{1.7} + \beta_1$ (open squares) plotted versus voltage. B, The time constants of Na$_{1.8}$ (filled circles) and Na$_{1.8} + \beta_1$ (open circles) plotted versus voltage.
Figure 5. Effects of the \( \beta \) subunit on the activation, inactivation, and recovery of \( \text{Na}_1.7 \) and \( \text{Na}_1.8 \) channels. Activation was measured by applying a series of depolarizing voltage pulses between \(-80 \) and \(+60 \) mV from a holding potential of \(-100 \) mV. The peak currents were measured, and the relative conductance was calculated by using the standard procedures (see Materials and Methods). Also plotted is the steady-state availability curve that was determined by using 500 msec conditioning pulses to voltages between \(-110 \) and \(+30 \) mV and a standard test pulse to either \(-20 \) mV (\( \text{Na}_1.7 \) and \( \text{Na}_1.7+\beta_1 \)) or \(+20 \) mV (\( \text{Na}_1.8 \) and \( \text{Na}_1.8+\beta_1 \)). Test currents were normalized and plotted versus conditioning voltage. A, The normalized conductance versus voltage and steady-state inactivation plots of \( \text{Na}_1.7 \) (filled squares) and \( \text{Na}_1.7+\beta_1 \) (open squares) channels. The smooth curves are Boltzmann fits: \( G = \frac{1}{1 + \exp \left( \frac{V - V_{0.5}}{k} \right)} \), with midpoints \( (V_{0.5}) \) and slope factors \( (k) \) of activation of \(-22 \pm 2.7 \) and \(5.4 \pm 0.4 \) mV for \( \text{Na}_1.7 \) \( (n = 10) \) and \(-27.7 \pm 1.3 \) and \(3.7 \pm 0.2 \) mV for \( \text{Na}_1.7+\beta_1 \) \( (n = 11) \). For inactivation the \( V_{0.5} \) and \( k \) values are \(-68.2 \pm 0.43 \) and \(6.4 \pm 0.45 \) mV for \( \text{Na}_1.7 \) \( (n = 4) \) and \(-69.8 \pm 0.3 \) and \(3.9 \pm 0.2 \) mV for \( \text{Na}_1.7+\beta_1 \) \( (n = 4) \). B, Steady-state activation and inactivation of \( \text{Na}_1.8 \) channels. The smooth curves have \( V_{0.5} \) and \( k \) values for activation of \(4.7 \pm 0.7 \) and \(6.8 \pm 0.1 \) mV for \( \text{Na}_1.8 \) \( (n = 8) \) and \(-3.3 \pm 1.0 \) and \(5.5 \pm 0.1 \) mV for \( \text{Na}_1.8+\beta_1 \) \( (open \; circles; \; n = 9) \). The \( V_{0.5} \) and \( k \) values for inactivation are \(-54.8 \pm 1.7 \) and \(8.4 \pm 0.2 \) mV for \( \text{Na}_1.8 \) \( (n = 3) \) and \(-62.6 \pm 2.3 \) and \(6.3 \pm 0.7 \) mV for \( \text{Na}_1.8+\beta_1 \) \( (n = 6) \). C, D, The time course of recovery from inactivation of \( \text{Na}_1.7 \) and \( \text{Na}_1.8 \) channels. Inactivation was induced by depolarizing to \(-20 \) mV (\( \text{Na}_1.7 \) and \( \text{Na}_1.7+\beta_1 \)) or \(+20 \) mV (\( \text{Na}_1.8 \) and \( \text{Na}_1.8+\beta_1 \)) for 50 msec before returning to \(-100 \) mV for intervals between 1 msec and 5 sec. A standard test pulse was used to monitor recovery, and the normalized test currents were plotted versus the recovery interval. C. Recovery from inactivation of \( \text{Na}_1.7 \) (filled squares) and \( \text{Na}_1.7+\beta_1 \) (open squares) channels. The smooth curves are fits to the sum of two exponentials: \( I/I_{0} = A_F \cdot (1 - \exp(-t/\tau_F)) + A_S \cdot (1 - \exp(-t/\tau_S)) \), with time constants \( (\tau) \) and weighting factors \( (A) \) of -19.6 \pm 0.8 msec \( (\tau_1; A_F = 0.46 \pm 0.02) \) and 933.4 \pm 54.6 msec \( (\tau_2; A_S = 0.54 \pm 0.02) \) for \( \text{Na}_1.7 \) \( (n = 7) \) and 6.6 \pm 0.6 msec \( (\tau_1; A_F = 0.89 \pm 0.02) \) and 53.2 \pm 12.7 msec \( (\tau_2; A_S = 0.11 \pm 0.02) \) for \( \text{Na}_1.7+\beta_1 \) \( (n = 7) \). D. The recovery of \( \text{Na}_1.8 \) (filled circles) and \( \text{Na}_1.8+\beta_1 \) (open circles) channels is described best by the sum of three exponentials: \( I/I_{0} = A_F \cdot (1 - \exp(-t/\tau_1)) + A_I \cdot (1 - \exp(-t/\tau_2)) + A_S \cdot (1 - \exp(-t/\tau_3)) \), where \( \tau_1, \tau_2, \) and \( \tau_3 \) are the fast, intermediate, and slow recovery time constants, and \( A_F, A_I, \) and \( A_S \) are the relative weighting factors. \( t \) is the interpulse duration, and \( I/I_{0} \) is the normalized current amplitude. Data are the means \pm SEM. The time constants of \( \text{Na}_1.8 \) are 9.9 \pm 1.8 msec \( (\tau_1; A_F = 0.41 \pm 0.04) \), 168.6 \pm 52.2 msec \( (\tau_2; A_I = 0.28 \pm 0.04) \), and 787.6 \pm 112.6 msec \( (\tau_3; A_S = 0.28 \pm 0.04) \) \( (filled \; circles; \; n = 5) \). Recovery time constants of \( \text{Na}_1.8+\beta_1 \) are 20.0 \pm 3.3 msec \( (\tau_1; A_F = 0.32 \pm 0.05) \), 243.8 \pm 85.4 msec \( (\tau_2; A_I = 0.34 \pm 0.05) \), and 1070.1 \pm 59.0 msec \( (\tau_3; A_S = 0.34 \pm 0.02) \) \( (open \; circles; \; n = 4) \).
and is plotted versus the conditioning pulse interval. The decay of the currents pulse was used to assay availability. The test currents were normalized and inactivate the channels. A 20 msec pulse to Na\textsubscript{v}1.8 is the conditioning pulse duration, and $I_{\text{th}}$ is the normalized current. The data are the means ± SEM. The time constants of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels are $\tau_3 = 32.6 \pm 1.5$ msec ($\Delta F = 0.25 \pm 0.03$), $\tau_1 = 556.5 \pm 104.4$ msec ($\Delta F = 0.33 \pm 0.02$), and $\tau_2 = 4071.9 \pm 155.1$ msec ($\Delta F = 0.42 \pm 0.03$) ($n = 6$). For Na\textsubscript{v}1.8+β\textsubscript{1} (open circles) the time constants are $\tau_2 = 8.4 \pm 1.5$ msec ($\Delta F = 0.57 \pm 0.07$), $\tau_1 = 200.0 \pm 30.0$ msec ($\Delta F = 0.16 \pm 0.07$), and $\tau_3 = 8880.0 \pm 1150.0$ msec ($\Delta F = 0.27 \pm 0.04$) ($n = 5$).

The $\beta_1$ subunit modulates levels of sodium currents of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8

The $\beta_1$ subunit selectively enhances the expression of Na\textsubscript{v}1.8 channels, but not Na\textsubscript{v}1.7 channels (Fig. 2). Comparing the average sodium current from paired groups of oocytes indicates that the expression of Na\textsubscript{v}1.8 increases by almost sixfold in the presence of the $\beta_1$ subunit versus 1.1-fold for Na\textsubscript{v}1.7. The selective regulation of Na\textsubscript{v}1.8 sodium channel expression by the $\beta_1$ subunit may play an important role in regulating TTX-R current in vivo (Cummins and Waxman, 1997; Novakovic et al., 1998; Gold, 1999). A similar modulation of Na\textsubscript{v}1.8 sodium channel expression was observed recently with another auxiliary ($\beta_3$) subunit (Shah et al., 2000).

The $\beta_1$ subunit alters gating and voltage sensitivity of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels

Coexpression with the $\beta_1$ subunit significantly alters the kinetics and voltage sensitivity of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium currents. In the absence of $\beta_1$, the inactivation of Na\textsubscript{v}1.7 is slow and incomplete. The $\beta_1$ subunit accelerates the current decay consistent with a more rapid rate of inactivation. At -20 mV the inactivation of Na\textsubscript{v}1.7 increases nearly 10-fold when the channels are coexpressed with the $\beta_1$ subunit. The $\beta_1$ subunit also alters the voltage sensitivity of the channels, shifting the midpoints of steady-state activation and inactivation by -5.3 and -1.6 mV, respectively.

Similar changes in current kinetics and voltage sensitivity are observed when the Na\textsubscript{v}1.8 channels are coexpressed with the $\beta_1$ subunit. Coexpression with the $\beta_1$ subunit decreases the time constant of current decay at +20 mV by 1.6-fold, consistent with more rapid inactivation. In the presence of the $\beta_1$ subunit the
midpoints of steady-state activation and inactivation of Na\textsubscript{v}1.8 channels are shifted significantly by \(-8\) and \(-7.8\) mV, respectively.

The \(\beta_1\) subunit alters the recovery from fast inactivation

The \(\beta_1\) subunit also significantly affects the time course of recovery from inactivation of the Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 sodium channels (Fig. 5C,D). The recovery from inactivation of Na\textsubscript{v}1.7 is well fit by two exponentials with time constants of 19 and 933 msec for Na\textsubscript{v}1.7 and time constants of 6.6 and 53 msec for Na\textsubscript{v}1.7+\(\beta_1\). The recovery of the Na\textsubscript{v}1.8 channels is also considerably slower and requires three exponentials to describe the time course adequately. Coexpression of Na\textsubscript{v}1.8 with the \(\beta_1\) subunit accelerates the fast component of recovery from inactivation but delays the intermediate and slow components of recovery from fast inactivation. The mechanism underlying this differential effect on the fast and slow components of inactivation is currently under investigation.

Our data indicate that the \(\beta_1\) subunit has significant effects on both the Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 channels, particularly on the kinetics of inactivation. A similar increase in inactivation rate with \(\beta_1\) coexpression recently has been reported for Na\textsubscript{v}1.7 channels (Shcherbatko et al., 1999). These findings are inconsistent with previous studies showing that the functional properties of Na\textsubscript{v}1.7 and Na\textsubscript{v}1.8 channels expressed in oocytes are not altered by the \(\beta_1\) subunit (Sangameswaran et al., 1996, 1997). Although we have no clear explanation for the differences between our data and those of these previous investigators, our data are consistent with studies showing that the \(\beta_1\) subunit modulates the gating and expression of many neuronal sodium channels (Isom et al., 1995; Shcherbatko et al., 1999).

Comparison with TTX-S and TTX-R sodium channels of DRG neurons

Multiple components of sodium current have been recorded from native DRG neurons that exhibit significant differences in gating and toxin sensitivity (Kostyuk et al., 1981; Roy and Narahashi, 1992; Ogata and Tatebayashi, 1993; Rush et al., 1998). The kinetics of the TTX-S currents are generally faster, and the steady-state activation and inactivation are shifted toward more hyperpolarized voltages in comparison with the TTX-R currents. These properties are qualitatively consistent with those of the Na\textsubscript{v}1.7 (TTX-S) and Na\textsubscript{v}1.8 (TTX-R) sodium channels observed...
in this study. For the Na$_{1.7} + \beta_1$ channels the midpoints of steady-state activation, inactivation, and the kinetics of inactivation are in reasonable agreement with the properties of TTX-S currents measured from acutely dissociated DRG neurons (Kostyuk et al., 1981; Roy and Narahashi, 1992; Ogata and Tatebayashi, 1993; Rush et al., 1998). The Na$_{1.7}$ channel, along with its associated $\beta_1$ subunit, is likely to contribute to TTX-S sodium currents of both large and small DRG neurons (Ogata and Tatebayashi, 1993; Rush et al., 1998).

In contrast, the midpoint steady-state inactivation of Na$_{1.8} + \beta_1$ (−62.6 mV) is more hyperpolarized than the native TTX-R sodium currents (−34 to −52 mV). The reasons for this discrepancy are unclear; however, a recent study has shown that at least three distinct components of TTX-R sodium current are present in the native cells (Rush et al., 1998). Variation in the relative expression levels of these different TTX-R sodium channels may explain the wide range of electrophysiological properties reported for the TTX-R currents of DRG neurons. In addition, the presence of additional $\beta$ subunits ($\beta_2, \beta_3$) or a variation in second messenger regulation may contribute further to the differences in the inactivation of heterologously expressed Na$_{1.8}$ and the TTX-R current of DRG neurons. In addition, our data show that the development of slow inactivation of the Na$_{1.8} + \beta_1$ channels is unusually rapid. This can influence the properties of steady-state inactivation by shifting the midpoint toward more hyperpolarized voltages (Ogata and Tatebayashi, 1992). Interestingly, a TTX-R3 component of sodium current of type D DRG neurons has been identified recently that has a midpoint of steady-state inactivation of −63 mV, identical to what we observed for the Na$_{1.8} + \beta_1$ channels (Rush et al., 1998). Despite some quantitative differences the data indicate that coexpression of Na$_{1.8}$ and the $\beta_1$ subunits in oocytes produces currents that have kinetics and voltage sensitivity similar to the TTX-R sodium currents of small DRG neurons.

Several studies have shown that the amplitudes of DRG neuron sodium currents are highly sensitive to the frequency of the applied voltage pulses (Rush et al., 1998; Scholz et al., 1998). In general, the TTX-R currents are reported to be more sensitive to rapid repetitive pulsing than the TTX-S sodium currents. These data suggest important differences in the repriming of these channels after a depolarizing voltage pulse. In this study the Na$_{1.8} + \beta_1$ channels display a significant reduction in current amplitude during repetitive stimulation at frequencies between 1 and 2 Hz (Fig. 7). This contrasts with Na$_{1.7} + \beta_1$ channels, which are considerably less sensitive to such low-frequency stimulation. The data suggest that during low-frequency repetitive stimulation (1–2 Hz) inactivated Na$_{1.8} + \beta_1$ channels fail to recover fully during the interval between pulses. At 2 Hz the rest interval between pulses (492 msec) is sufficient to permit full recovery of fast inactivated channels ($\tau_r = 2$ msec). The entry and recovery from fast inactivation cannot account for the observed frequency-dependent reduction of Na$_{1.8} + \beta_1$ currents. Rather, the data suggest that a fraction of Na$_{1.8} + \beta_1$ channels may enter into a slow inactivated state during the brief depolarizations. The time course of entry into the slow inactivated state has been measured directly by a double-pulse protocol (Fig. 6). The onset of slow inactivation of Na$_{1.8} + \beta_1$ channels ($\tau_r = 8.4$ msec) is considerably faster than that of the Na$_{1.7} + \beta_1$ channels ($\tau_r = 33$ msec). During the short depolarizations used in the repetitive pulsing protocol (8 msec), a significant fraction of the Na$_{1.8} + \beta_1$ channels, but not Na$_{1.7} + \beta_1$ channels, is predicted to undergo slow inactivation. Few of these slow inactivated channels recover ($\tau_r = 1070$ msec) during the short interval (492 msec) between pulses. The data indicate that the high sensitivity of the Na$_{1.8} + \beta_1$ channels to low-frequency repetitive stimulation results from the unusually rapid entry of these channels into the slow inactivated state. A similar mechanism has been proposed for the TTX-R sodium current of DRG neurons (Scholz et al., 1998). Na$_{1.7} + \beta_1$ channels are more resistant to slow inactivation and are significantly less sensitive to low-frequency repetitive stimulation.

**Physiological relevance**

Previous work suggests that the rapid repriming and high threshold of TTX-R sodium currents may play an important role in the sustained firing of C fibers after nerve injury (Elliott and Elliott, 1993; Jeftinija, 1994; Schild and Kunze, 1997). Although the majority of the Na$_{1.8} + \beta_1$ channels rapidly recovers from inactivation, these channels are also more likely to enter slow inactivated states. During sustained repetitive firing a significant fraction of the Na$_{1.8} + \beta_1$ channels is likely to accumulate in this slow inactivated state. However, at very high frequencies (>20 Hz) the amplitudes of Na$_{1.8} + \beta_1$ currents reach steady state, being reduced 58% in comparison with the initial current level (Fig. 7). This is nearly equivalent to the fraction of channels (58.3%) that rapidly enters into the slow repriming state in response to sustained depolarization (\(\tau_r = 8\) msec) (Fig. 7). The data suggest that during repetitive pulsing at high frequency (>20 Hz), or in response to sustained depolarization, 60% of the Na$_{1.8} + \beta_1$ channels rapidly enter into slow inactivated states; however, the other 40% of active channels will contribute to action potential firing.

In addition, the atypical kinetics and voltage sensitivity of the Na$_{1.8} + \beta_1$ sodium channels may contribute to the unusual electrical excitability of the small nociceptive neurons in which these channels are expressed preferentially (Caffrey et al., 1992; Arbuckle and Docherty, 1995; Novakovic et al., 1998). The relative contribution of the Na$_{1.8} + \beta_1$ channels to the total sodium current of nociceptive neurons may contribute to the high threshold (McLean et al., 1998) and slow firing frequency of C fibers (Harper and Lawson, 1985). The slow inactivation and recovery kinetics of the Na$_{1.8} + \beta_1$ channels would tend to broaden the action potential and reduce the firing frequency of these neurons. These unique properties of the Na$_{1.8} + \beta_1$ channels may play a role in the adaptation of nociceptive nerve impulses during low firing frequency. On the other hand, the resistance of Na$_{1.8} + \beta_1$ channels to enter fully into the slow inactivated state during high-frequency (>20 Hz) stimulation, coupled with the high threshold for activation (\(V_{\text{th}} = -3.3\) mV), could maintain a minimal level of sodium channel activity in rapidly firing or chronically depolarized neurons during sustained noxious stimuli. This may enable pain fibers to continue generating action potentials after peripheral nerve damage.

In conclusion, the present study shows that the modulatory effects of the $\beta$ subunit are likely to have important consequences for the electrical excitability of the DRG neurons expressing these channels. However, the existence of other auxiliary subunits ($\beta_2$ and $\beta_3$) in these nociceptive C fibers (Shah et al., 2000; Coward et al., 2001) could have complementary regulatory effects on Na$_{1.7} + \beta_1$ and Na$_{1.8} + \beta_1$ function. The possible roles of the other $\beta$ subunits need to be tested.

**REFERENCES**


