Behavioral/Systems/Cognitive

Bistable Network Behavior of Layer I Interneurons in Auditory Cortex

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GABAergic interneurons in many areas of the neocortex are mutually connected via chemical and electrical synapses. Previous computational studies have explored how these coupling parameters influence the firing patterns of interneuronal networks. These models have predicted that the stable states of such interneuronal networks will be either synchrony (near zero phase lag) or antisynergy (phase lag near one-half of the interspike interval), depending on network connectivity and firing rates. In certain parameter regimens, the network can be bistable, settling into either stable state depending on the initial conditions. Here, we investigated how connectivity parameters influence spike patterns in paired recordings from layer I interneurons in brain slices from juvenile mice. Observed properties of chemical and electrical synapses were used to simulate connections between uncoupled cells via dynamic clamp. In uncoupled pairs, action potentials induced by constant depolarizing currents had randomly distributed phase differences between the two cells. When coupled with simulated chemical (inhibitory) synapses, however, these pairs exhibited a bimodal firing pattern, tending to fire either in synchrony or in antisynergy. Combining electrical with chemical synapses, prolonging $T_{\text{Decay}}$ of inhibitory connections, or increasing the firing rate of the network all resulted in enhanced stability of the synchronous state. Thus, electrical and inhibitory synaptic coupling constrain the relative timing of spikes in a two-cell network to, at most, two stable states, the stability and precision of which depend on the exact parameters of coupling.

Key words: inhibition; GABA_A; gap junctions; synchrony; neocortex; anesthesia

Introduction

In the auditory cortex (ACx), firing patterns distributed across populations of pyramidal cells are postulated to represent features of the acoustic environment (Lu et al., 2001; Mickey and Middlebrooks, 2003). We are interested in how GABAergic interneurons shape these firing patterns. Interneurons regulate spike timing by inhibiting target cells for brief periods of time, and they coordinate spike timing across cell populations via divergence (Cobb et al., 1995). These rules apply as well in interneuronal networks in which cells are coupled by inhibitory synapses and/or gap junctions (Whittington et al., 1995; Galarreta and Hestrin, 1999; Beierlein et al., 2000). Spike times in these networks are constrained by synaptic coupling parameters, the modulation of which alters the dynamics of observed firing patterns. For example, synchronous $\gamma$ oscillations (30–80 Hz) exhibited by interneuronal networks are modulated in frequency and coherence by anesthetic agents that prolong inhibition (Whittington et al., 1996; Faulkner et al., 1998). Indeed, it is postulated that general anesthetics impair cortical processing by modulating these firing patterns (Faulkner et al., 1998; Baker et al., 2002; John, 2002; Mashour, 2004). Because most anesthetic agents prolong GABA_A receptor-mediated IPSCs (Jones and Harrison, 1993; Banks and Pearce, 1999; Antkowiak, 2001), it is critical to understand how prolonging inhibition alters the functional output of interneuronal networks.

Interneurons in layer I (LI) form networks of cells coupled by both chemical and electrical synapses (Chu et al., 2003). Many LI interneurons have dense, horizontally extensive axonal projections, suggesting that LI interneurons may coordinate activity patterns across multiple cortical columns (Nieuwenhuys, 1994; Hestrin and Armstrong, 1996; Zhou and Hablitz, 1996). In the ACx, $\gamma$ oscillations occur spontaneously but can also be evoked by stimulation of intralaminar thalamic nuclei (Brett and Barth, 1997), which project preferentially to LI (Hu, 2003). These rhythmic firing patterns are also observed in vitro (Metherate and Cruikshank, 1999; Traub et al., 2005), indicating that intracortical circuitry is sufficient to underlie this network activity.

In theoretical and computational studies, networks of cells connected by weak inhibitory synapses and/or gap junctions exhibit two stable firing states, synchrony (zero phase lag) or anti-synchrony (phase lag of 0.5 on the unit circle) (van Vreeswijk et al., 1994; Wang and Buzsaki, 1996; Di Garbo et al., 2002; Lewis and Rinzel, 2003). Over some range of the parameter space, these networks exhibit “bistability,” converging toward either synchrony or anti-synchrony, depending on the initial conditions. Evidence for bistability has not been observed previously in bio-
logical networks, although a recent study showed that synchrony and antisynchrony can coexist at different mean firing rates (Gibson et al., 2005).

We hypothesized that networks of interneurons in LI would exhibit multiple preferred-activity patterns and that anesthetic agents would alter the stability of these patterns by modulating inhibition. To test this hypothesis, we recorded interneurons in LI coupled via dynamic clamp and investigated the firing patterns these two-cell networks generated using coupling parameters recorded under control conditions and in the presence of the general anesthetic isoflurane.

**Materials and Methods**

*Slice preparation.* All experimental protocols conformed to American Physiological Society/National Institutes of Health guidelines and were approved by the University of Wisconsin Research Animal Resources Committee. Male and female CBA/J mice (postnatal days 13–25) were decapitated under isoflurane anesthesia, and the brains were extracted and immersed in artificial CSF [ACSF; composed of (in mM) 126 NaCl, 26 NaHCO₃, 1.8 KCl, 2.1 CaCl₂, 1.4 MgSO₄, 1.2 KH₂PO₄, and 10 glucose] at 0–4°C. Slices (500 μm) were obtained from the left hemisphere in a plane 15° off the horizontal plane, as described for auditory thalamo-concentration in solutions bubbled with isoflurane gas, and in parallel determining the relationship between electrode potential and isoflurane concentration. Teflon tubing was used to connect gas exchange bags (catalog #10-923-5; Fisher Scientific, Hampton, NH) that contained ACSF bubbled with 95% O₂/5% CO₂. The isoflurane solution was prepared in 500 ml Teflon gas sampling bags at 0°C using pClamp version 9.0 (Molecular Devices).

Isoflurane (Novaplus; Abbott Labs, North Chicago, IL) was bath applied to slices as follows. Isoflurane was prepared as an aqueous solution from a saturated stock solution (15 mM in ACSF) (Firestone et al., 1986) and diluted to a final concentration in ACSF on the day of the experiment. The isoflurane solution was prepared in 500 ml Teflon gas sampling bags (catalog #10-923-5; Fisher Scientific, Hampton, NH) that contained ACSF bubbled with 95% O₂/5% CO₂. Teflon tubing was used between the ACSF reservoirs and the recording chamber to minimize loss of the volatile agent before it reached the tissue. Preliminary experiments in which isoflurane concentration was measured in the liquid phase using Ca⁺⁺-sensitive electrodes (Hagan et al., 1998) indicated that ~15% of the isoflurane was lost before it reached the center of the recording chamber, similar to a previous study using identical techniques and equipment (Banks and Pearce, 1999). We calibrated the Ca⁺⁺-sensitive electrode by determining the relationship between electrode potential and isoflurane concentration in solutions bubbled with isoflurane gas, and in parallel with solutions prepared as for our slices from stock concentrations assuming a saturating concentration of 15 mM (Hagan et al., 1998). We then measured the electrode potential in the slice chamber while perfusing with different isoflurane concentrations and calculated the percentage of loss according to the measured linear relationship between electrode potential and isoflurane concentration. This loss was accounted for in the reported values of the concentration of isoflurane used in these experiments.

After forming a gigahm seal and rupturing the membrane to achieve intracellular access, glutamate receptor antagonists were allowed to equilibrate for 5 min before recording a baseline control period of 15 min duration. Isoflurane was then bath applied for 20 min. Recovery data were recorded for >30 min after removal of isoflurane from the bathing medium. Recovery data were obtained in eight of nine recordings. Throughout the experiment, access resistance was monitored at least every 10 min, and compensation was adjusted as needed. Experiments in which access resistance changed by >25% were discarded.

For these and all experiments, data were amplified (MultiClamp-700A; Molecular Devices, Union City, CA), low-pass filtered (10 kHz), digitized (20 kHz; DigiData 1322A; Molecular Devices), and recorded using pClamp version 9.0 (Molecular Devices).

**Patch-clamp electrophysiology: current clamp.** Identical patch pipettes were used for these experiments as for the voltage-clamp experiments. The patch pipette solution contained the following (in mM): 140 K-glucuronate, 10 NaCl, 10 HEPES, 0.1 EGTA, and 2 MgATP, pH 7.2. A junction potential of ~12 mV was corrected off-line. Open tip resistances with this solution were 4–6 MΩ. Pairs of LI cells were tested for synaptic coupling by triggering action potentials in the putative presynaptic cell in current-clamp mode and recording from the putative postsynaptic cell in voltage-clamp mode, shifting the holding potential from ~100 to +20 mV. Functional conductance of electrical synapses was estimated by assuming that both cells were isopotential and connected only to each other.

**Dynamic-clamp recordings from cell pairs.** Patch pipettes and pipette solution were identical to those used for the current-clamp experiments above. Bath application of 4 mM kynurenic acid and 20 μM bicuculline was used to block ionotropic glutamate and GABA synaptic currents.

Dynamic-clamp recordings were implemented using Real-Time Linux Dynamic Clamp software developed at the Boston University Neuronal Dynamics Laboratory (Dorval et al., 2001) running under Red Hat Linux and connected to a MultiClamp amplifier (700A; Molecular Devices) via a data acquisition board (NI PCI-6052E; National Instruments, Austin, TX). To simulate chemical (inhibitory) synapses, the dynamic clamp generated a signal of the form I_syn = G_s(V_m - E_rev) = G_s(V_m - E_syn)/K_SF, where G_s is the maximal synaptic conductance (0.5 nS), I_syn is the synaptic conductance decay time constant (7, 14, and 21 ms), and E_syn is the synaptic reversal potential (~70 mV), and K_SF is a scale factor such that the peak of the current scales to unity when G_s = 1. This current was injected into either cell whenever a spike (defined as a threshold crossing, typically 0 mV, of positive slope) was detected in the opposite cell, with a synaptic delay of 1.2 ms from spike detection to event initiation. To simulate electrical synapses, the dynamic clamp applied a current of the form I_e = G_e(V_m - V_syn), to each cell continuously, where G_e is the gap-junction conductance (0.5 nS) and V_syn is the membrane potential of the opposite cell.

These signals were scaled appropriately, converted to analog signals, and passed to the current–drive channel of the bridge-balance amplifier. The measured values V_syn and V_m were updated, and new values of I_syn and I_e were calculated and delivered, at a clock rate of 5–10 kHz. The inhibitory synaptic coupling parameters used were based on sIPSCs observed in voltage-clamped LI cells under normal conditions (τ_syn = 7 ms) and in the presence of 0.2 and 0.4 mM isoflurane (τ_syn = 14 and ~21 ms, respectively) (Fig. 1). The electrical conductance parameter used was based on recordings from pairs of LI cells coupled with biological gap junctions (Fig. 1).

Square pulses of current (duration, 0.5–2 s) were injected to induce spiking in both cells, with the current amplitude in each cell adjusted to achieve a target interspike interval (ISI) between 10 and 120 ms. For each pair of cells, we tested the effect on relative spike times of changing τ_syn (7, 14, and 21 ms) with and without electrical coupling, typically at three

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**References**


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**Figures**

Fig. 1. Dynamic-clamp recordings from cell pairs. a) The dynamic clamp applied a current of the form I_syn = G_s(V_m - E_rev) = G_s(V_m - E_syn)/K_SF, where G_s is the maximal synaptic conductance (0.5 nS), I_syn is the synaptic conductance decay time constant (7, 14, and 21 ms), and E_syn is the synaptic reversal potential (~70 mV), and K_SF is a scale factor such that the peak of the current scales to unity when G_s = 1. This current was injected into either cell whenever a spike (defined as a threshold crossing, typically 0 mV, of positive slope) was detected in the opposite cell, with a synaptic delay of 1.2 ms from spike detection to event initiation. To simulate electrical synapses, the dynamic clamp applied a current of the form I_e = G_e(V_m - V_syn), to each cell continuously, where G_e is the gap-junction conductance (0.5 nS) and V_syn is the membrane potential of the opposite cell.

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different firing rates. A single trial consisted of the responses to a train of square current pulses eliciting >200 spikes in each cell when the cells were connected with one set of coupling parameters. Thus, in each cell pair, up to 24 trials were obtained. Trials in which either cell was unable to maintain a consistent ISI (SD/mean, >0.2) or in which the cells did not have similar ISIs [D = Mean1 − Mean2 / (Mean1 + Mean2) > 0.25] were discarded. In fact, the disparity measure, D, was usually much less than 0.25 (D = 0.1 for 316 of 436, ~72% of trials; D = 0.15 for 374 of 436, ~86% of trials; D = 0.2 for 431 of 436, ~99% of trials).

Firing properties of LI interneurons were heterogeneous, and the cells studied in these experiments included representatives of previously identified classes of cortical interneurons, including fast spiking, regular spiking, and low-threshold spiking cells (Kawaguchi and Kubota, 1997; Gibson et al., 1999; Markram et al., 2004). However, there was considerable overlap in the firing and membrane properties of the cells in our data set, and we could find no satisfactory quantitative method for assigning individual cells to classes in a nonarbitrary manner. Thus, we do not present an analysis of how membrane or firing properties affected the network behavior of interneuronal pairs.

Analysis. sIPSCs were analyzed using an automated event detection algorithm (Banks et al., 1998). In this algorithm, two windows were moved along the data, a “peak” window and a “baseline” window. At each time point, the data within each window were averaged, and the baseline point was subtracted from the peak. This yielded a “pseudo-differentiated” form of the data that was characterized by large, rapid peaks at the onset of GABA<sub>A</sub> IPSCs. Threshold-level crossings were identified in this pseudo-differentiated data, with threshold set as 3 × σ<sub>Noise</sub>, where σ<sub>Noise</sub> was measured during periods of no visually detectable events and was typically 3–5 pA. Because the baseline value was constantly updated during the analysis, slow changes in baseline had no effect on the accuracy of the algorithm. This algorithm successfully detected >99% of sIPSCs. Individual sIPSCs (n > 20 in each cell for each condition) were selected for averaging when no other detected events occurred within ±100 ms of the peak. The averaged sIPSCs were then used to measure 10–90% rise times (t<sub>Rise</sub>). Decay phases were best fit by two exponential components, and decay kinetics were characterized additionally by the weighted sum of the exponential decay components, t<sub>Dec,Wt</sub> = A<sub>1</sub>t<sub>1</sub> + A<sub>2</sub>t<sub>2</sub>. The time courses of individual, uncontaminated events were also characterized by the time to decay from peak to within 37% of the baseline.

For analyzing network activity in dynamic-clamp recordings, spike times were detected from the raw voltage traces using software written in Matlab. All spike times in a given trial were used, provided the trial satisfied the inclusion criteria mentioned above. Mean ISIs were computed from these raw spike times. Spike pairs in the network were defined by treating one cell as a reference cell and the other cell as a comparison cell, and for each spike in the reference cell finding the closest spike in time in the comparison cell. These spike pairs were then used to compute relative spike-time and phase histograms, fractions of spike pairs falling into particular phase ranges, and phase dynamics (i.e., trajectories of transitions between different phases). The phase variable, θ, of the network was defined by normalizing the time differential be-
between neighboring spikes in the two cells to the ISI of the reference cell (both cells were treated as the reference in separate analyses). Phase thus had a range of 0 \leq \phi \leq 1, but because this unit circle displayed symmetry about \phi = 0.5 (see Results), we folded it into a half-circle, so that 0.9 \leq \phi \leq 0.8 was equivalent to 0.1 \leq \phi \leq 0.2, 0.8 \leq \phi \leq 0.7 was equivalent to 0.2 \leq \phi \leq 0.3, and so on. We found that the ratio of \tau_{\text{decay}} to mean ISI (White et al., 1998) was a good predictor of the stability of the synchronous firing state (see Results). To investigate the effect of this “inhibitory ratio” on network firing behavior, we took all trials recorded under the conditions being considered and divided the data into quintiles of the inhibitory ratio, computing mean parameters within each quintile.

Data are presented as mean ± SD. Statistical comparisons were performed using SPSS for Windows version 12.0 (SPSS, Chicago, IL).

**Results**

**Synaptic coupling parameters in LI interneurons**

We assessed the incidence, type, and strength of synaptic coupling between LI interneurons using paired whole-cell recordings. In these experiments, the putative presynaptic cell was stimulated in current-clamp mode with a current pulse that depolarized the cell and triggered action potentials, and the putative postsynaptic cell was held at various potentials in voltage clamp (Fig. 1A). Near the reversal potential for GABA_\text{A} receptor-mediated IPSCs (V_m = −70 mV), electrical coupling was manifested as a slow change in the holding current in the postsynaptic cell during the slow sub-threshold depolarization in the presynaptic cell, and more rapid “spikelets” during action potentials in the presynaptic cell (Fig. 1A, left). When the postsynaptic cell was held depolarized to the reversal potential for GABA_\text{A} IPSCs, chemical coupling was manifest as slower, slightly delayed synaptic outward currents that, if electrical coupling was also present, rode on top of the electrical coupling response (Fig. 1A, right). Evidence for electrical coupling was found in 25% (16 of 65) of the pairs of LI interneurons tested, with a mean coupling strength of 0.43 ± 0.39 nS, and in all cases, the coupling was bidirectional. Evidence for chemical coupling was observed in 15% (10 of 65) of pairs, with one-half of these connections bidirectional. In most cases, chemical coupling (6 of 10 pairs) was observed in conjunction with electrical coupling. Interestingly, all five pairs with bidirectional chemical coupling were also coupled by electrical synapses.

In the four cell pairs coupled by chemical synapses in the absence of electrical coupling, IPSCs occurred with a synaptic delay of 1.16 ± 0.13 ms, had peak amplitudes of 0.44 ± 0.22 nS, had 10–90% rise times of 1.45 ± 0.95 ms, and had 63% decay times of 6.33 ± 5.64 ms. The small sample size and large variability of the kinetics parameter measurements led us to obtain additional parameter estimates by analyzing sIPSCs, and their modulation by the volatile anesthetic agent isoflurane, in single-cell recordings from LI interneurons under whole-cell voltage clamp. This approach was necessarily indirect, because the sIPSCs recorded in LI cells undoubtedly arose from multiple interneuron populations in the slice. However, given the homogeneity of sIPSCs that we observed (Fig. 1B), this approach is likely to give a good approximation to the parameters of inhibitory synapses connecting LI cells.

sIPSCs in LI cells occurred at rates of 1.86 ± 0.97 Hz and had mean amplitudes, rise times, and weighted decay time constants of 0.73 ± 0.34 nS, 0.74 ± 0.22 ms, and 7.0 ± 1.5 ms, respectively (n = 11 cells) (Fig. 1B). We observed no correlation between rise time and amplitude for individual sIPSCs (data not shown), indicating that sIPSCs were not grossly distorted by spatial filtering. Isoflurane at 0.1, 0.2, and 0.4 mM prolonged the decay of sIPSCs by 0.39 nS, and 2.2, 1.0-, and 3.4 ± 0.4-fold, respectively (Fig. 1C) (n = 3 cells for each concentration). No significant effects were observed on rise time, amplitude, and frequency of sIPSCs at any concentration (data not shown). For our dynamic-clamp experiments, we used conductance amplitudes of 0.5 nS for both electrical and GABAergic synapses. For GABAergic synaptic conductance waveforms, a synaptic delay of 1.2 ms was used, 10–90% rise times were set to 1.1 ms (i.e., \tau_{\text{rise}} = 0.5 ms), and decay time constants were set to 7, 14, and 21 ms, these corresponding to control, 0.2 mM isoflurane, and 0.4 mM isoflurane, respectively.

**Network activity in cell pairs coupled by inhibition alone**

To assess the firing patterns exhibited by a network of LI cells coupled with well defined synaptic parameters, we obtained whole-cell recordings from pairs of neurons that were not biologically coupled but functionally coupled using a dynamic-clamp system. The amplitude and time course of conductance waveforms implemented were based on measurements in biologically coupled cells as presented above. Network activity was...
and without electrical coupling, to probe the changes that GABA
	interneurons could make. Inhibitory coupling was usually tested for three
coupling conditions: electrical coupling, combined inhibitory and

trical coupling. In separate trials, we used tonic depolarizing cur-

tants to induce firing frequencies ranging from 75 to 175 Hz in
	these networks and recorded spike times in each cell under con-

Firing rate. The dotted line indicates fit of the function

\[ \chi_\varphi = \frac{1}{2} \left( 1 + e^{-k(\varphi - \varphi_0)} \right) \]

to the data, where \( A = 1.7 \) and \( k = 0.044 \).

Figure 3. Synchrony is sensitive to both inhibitory decay time and mean firing rate. A, Fraction of phase values falling into each

\( \chi_{\varphi} \) range 0 to 0.5 (synchrony) (Fig. 2B–D). To quantify the synchronous and antisynchronous distributions, we used an algo-

rithm that for each trial automatically detected the peaks and troughs in histograms like those plotted in Figure 2B, combined the “half-peaks” for \( \varphi = \pm 0.5 \), and computed the mean phase and its SD for the synchronous and antisynchronous phase distributions. For the synchronous distribution, the mean phase averaged across all trials and all cell pairs was \( \mu_\varphi = 0.0086 \pm 0.012 \), and the mean SD of phase averaged across all trials and all cell pairs was \( \sigma_\varphi = 0.037 \pm 0.021 \). For the antisynchronous peak, \( \mu_\varphi = 0.47 \pm 0.022 \) and \( \sigma_\varphi = 0.12 \pm 0.029 \); the smaller value of \( \sigma_\varphi \), for synchronous versus antisynchronous spike pairs reflects the more precise timing of syn-

chronous versus antisynchronous spike pairs (\( n = 191 \) trials in 26 cell pairs; \( p < 0.001 \); Student’s paired t test). Because the

phase range 0 \( \leq \varphi \leq 0.5 \) were “folded” to overlay with spike pairs in the range 0 \( \leq \varphi \leq 0.5 \) (see Materials and

Methods). We divided this half-circle into five equal ranges and defined spike pair distributions. For the synchronous distri-

butions, the fractions of spike pairs falling in the synchronous and antisynchronous phase ranges were defined as \( \chi_0 = \varphi < 0.1 \) and \( \chi_0.4 = \varphi < 0.5 \), respectively. Note that randomly distributed phases would have \( \chi_0 = \varphi < 0.1 \), \( \chi_0.4 = \varphi < 0.5 \), and \( \chi_0 = \varphi < 0.1 \).

Synchronous firing was not, on average, favored over antisyn-

chronous firing in mutually inhibitory cells (Fig. 3A), but syn-

chrony did become more prevalent as the decay time of IPSCs or

the firing rate of the network was increased (Fig. 3B, C). A two-

way ANOVA with repeated measures (\( \tau_{\text{decay}} \) as the repeated-

measure, within-subjects factor; mean ISI as the between-

subjects factor) showed a significant effect of \( \tau_{\text{decay}} \) on \( \chi_0 \leq \varphi < 0.1 \) (\( F_{3,53} = 7.51; p < 0.001 \)) but no interaction

between the two factors (\( F_{3,53} = 1.79; p = 0.11 \)). Post hoc tests showed significant differences in \( \chi_0 = \varphi < 0.1 \) with increasing \( \tau_{\text{decay}} \) (Tukey’s test; \( p < 0.001 \) for all comparisons). The degree to which inhibitory coupling promoted the synchronous firing state compared with the uncoupled regimen was also dependent on the mean firing rate of the network. At the fastest firing rates tested, inhibitory coupling generally yielded increases (relative to uncoupled) in synchronous firing (Fig. 3C, □), whereas at the slowest firing rates, inhibitory coupling generally yielded decreases in synchrony when inhibition was added (Fig. 3C, ◊). A similar trend is seen when fractional change in synchrony from uncou-

studied in 58 pairs of interneurons in LI of the mouse ACx coupled via dynamic clamp. Of these cell pairs, 26 satisfied our inclusion criteria (see Materials and Methods) and were tested with at least two values of inhibitory conductance \( \tau_{\text{Decay}} \). Nearly all cells were tested with three values of \( \tau_{\text{Decay}} \) at two or more firing rates. Twenty-three cell pairs were tested additionally with electrical coupling. In separate trials, we used tonic depolarizing currents to induce firing frequencies ranging from 10 to 75 Hz in these networks and recorded spike times in each cell under conditions of inhibitory coupling, electrical coupling, combined inhibitory and electrical coupling, and no coupling (control) between the cells. Inhibitory coupling was usually tested for three distinct IPSC decay time constants (7, 14, and 21 ms), both with and without electrical coupling, to probe the changes that GABA\( \gamma \)-specific modulators might produce in these networks. The total number of trials in 26 cell pairs coupled by inhibition alone was 191, and the total number of trials in 23 cell pairs coupled with combined electrical and inhibitory coupling was 160.

The phase relationship between spike pairs in these recordings, \( \varphi \), was obtained for all neighboring spikes in each of the trials described above. In the absence of any coupling, \( \varphi \) was always distributed uniformly (Fig. 2A). When the cells were coupled with inhibition, they entered a firing pattern in which they
tended to alternate between two distinct phase ranges: one distributed broadly about \( \varphi = \sim 0.5 \) (antisynchronous) and the other more tightly distributed about \( \varphi = \sim 0 \) and/or 1 (synchronous) (Fig. 2B–D). This

\( \Delta \chi_{\varphi}(\text{Decay}, \text{ISI}) \) is a function of the mean ISI, \( \Delta \chi_{\varphi}(\text{Decay}, \text{ISI}) = Ae^{-k(\varphi - \varphi_0)} \), where \( A = 1.7 \) and \( k = 0.044 \).
pled to coupled by inhibition ($\tau_{\text{decay}} = 7$ ms) is plotted as a function of mean ISI (Fig. 3D).

The similar effects of $\tau_{\text{decay}}$ and firing rate on network synchrony reflects the relative amount of time between spikes that inhibition can influence the trajectory of membrane potential in the two cells. To study this explicitly, we considered the fraction of spike pairs falling into the synchronous range in a given trial as a function of the ratio of the inhibitory decay time constant to the

Figure 4. Network synchrony and spike variability increase with $\tau_{\text{decay}}$/ISI. A, Fraction of spike pairs in the synchronous phase range ($\chi_{\varphi} < 0.1$) for each trial (n = 191) as a function of the ratio of synaptic conductance $\tau_{\text{decay}}$ to mean ISI in the network. See Results for exponential fit parameters. B, SD (within trials) of spike pairs occurring in the synchronous phase range ($\sigma_{\varphi} < 0.1$) as a function of the ratio of synaptic conductance $\tau_{\text{decay}}$ to mean ISI in the network. Linear fit has slope $(5.32 \pm 0.407) \times 10^{-2}$, y-intercept $(1.70 \pm 0.181) \times 10^{-2}$, p < 0.0001. C, Mean ± SD of normalized phase-range distributions for all pairs tested (n = 26) in the highest (O) and lowest (□) quintiles of $\tau_{\text{decay}}$/ISI (38 trials each). The asterisks indicate a significant difference between quintiles (p < 0.05; Tukey’s post hoc test).

Figure 5. Electrical coupling promotes synchrony in LI networks. A, Sample voltage and current traces from a pair of spiking cells when they are uncoupled (left) and electrically coupled (right). Vertical scale bar: 40 mV, 70 pA; horizontal scale bar, 50 ms. B, Normalized phase ($\varphi$) histograms for entire trials in each coupling regimen (columns arranged as in A). C, Raster plot of $\varphi$ between neighboring spikes for each coupling regimen (columns arranged as in A and B) according to the time in which they occurred during the trial. D, Fraction of spike pairs falling into the synchronous phase range ($\chi_{\varphi} < 0.1$) for pairs that are uncoupled and electrically coupled (61 trials from 26 cell pairs; trend lines show same-rate, within-pair comparisons). E, Fractional change in synchrony from uncoupled to electrically coupled ($\Delta \chi_{\varphi} < 0.1$; same-rate, within-pairs comparisons). Note that this change is not rate dependent (n = 61 trials).
mean ISI of the cells ($\tau_{\text{Decay}}/\text{ISI}$). According to general scaling principles, this inhibitory ratio should determine the capacity of the network to generate synchrony, regardless of whether the two variables ($\tau_{\text{Decay}}$ and ISI) are both large or both small. Indeed, we found that this ratio was positively correlated with the tendency of the network to generate synchronous action potentials (Fig. 4A). Because $X_0 = \phi < 0.1$ cannot be greater than unity, we fit a function of the form $1 - Ae^{-B\phi} \tau_{\text{Decay}}/\text{ISI}$ to the data of Figure 4A, where $X = \tau_{\text{Decay}}/\text{ISI}$, and both parameters $A (0.94)$ and $B (0.53)$ indicate the sensitivity of the network to changes in $\tau_{\text{Decay}}/\text{ISI}$ within the parameter ranges tested.

To assess the variability of spike pairs falling into the synchronous range, we obtained SD values for the distribution of spike pairs in the range $0 \leq \phi < 0.1$ for each coupled trial ($\sigma_0 \leq \phi < 0.1$).

An increase in $\sigma_0 \leq \phi < 0.1$ accompanied the enhancement of synchrony as the inhibitory ratio was increased (Fig. 4B), indicating that although faster firing rates and slower inhibitory decay times promoted spiking near synchrony, they also decreased the precision of this synchrony. In contrast, the SD of antisynchronous spike-pair phase differences exhibited a small but significant decrease with an increasing inhibitory ratio (linear regression slope, $-0.0159$; correlation coefficient, $-0.14; p < 0.01$; data not shown).

To summarize the phase-distribution of spike pairs in two-cell networks coupled by inhibition, and the importance of the inhibitory ratio to this distribution, we averaged the fraction of spike pairs occurring in each phase range across multiple cell pairs and compared network behavior within quintiles of the mean values of $\tau_{\text{Decay}}/\text{ISI}$ observed for each trial. These average distributions confirmed that although antisynchrony was the most common state of the network under inhibitory coupling, networks operating within the highest quintile of $\tau_{\text{Decay}}/\text{ISI}$ yielded more synchrony than did those operating within the lowest quintile (Fig. 4C). Furthermore, this promotion of synchronous firing behavior was accompanied by an increase in the incidence of firing in the near-synchronous phase range and a decrease in the incidence of firing in the middle and near-antisynchroneous phase ranges (Fig. 4C). There were significant effects of $\tau_{\text{Decay}}/\text{ISI}$ on the fraction of spike pairs in each phase range (one-way ANOVA with each phase range tested separately; $0 \leq \phi < 0.1$: $F(4,186) = 33.02; p < 0.001$; $0.1 \leq \phi < 0.2$: $F(4,186) = 12.94; p < 0.001$; $0.2 \leq \phi < 0.3$: $F(4,186) = 6.557; p < 0.001$; $0.3 \leq \phi < 0.4$: $F(4,186) = 17.34, p < 0.001$; $0.4 \leq \phi < 0.5$: $F(4,186) = 3.558; p < 0.01$). Post hoc tests showed that there were significant differences between the highest and lowest quintiles of $\tau_{\text{Decay}}/\text{ISI}$ for the synchronous, near-synchronous, and near-antisynchroneous phase ranges but not for the antisynchronous phase range (Fig. 4C).
the variability of synchronous range spike-pairs as a function of $\tau_{\text{Decay}}/\text{ISI}$ was observed, similar to the case of inhibitory coupling alone (Fig. 7B). Thus, combining electrical with inhibitory coupling in these networks resulted in a promotion of synchrony with little effect on its precision. Average phase distributions showed a promotion of synchrony when the cells were electrically coupled similar to the case of inhibition alone, with synchrony becoming as prevalent as antisynchrony in the highest range of $\tau_{\text{Decay}}/\text{ISI}$ (Fig. 7C). A one-way ANOVA showed significant effects of $\tau_{\text{Decay}}/\text{ISI}$ on the fraction of spike pairs in each phase range (phase ranges were tested separately; $0 \leq \varphi < 0.1$; $F(4,155) = 16.83$, $p < 0.001$; $0.1 \leq \varphi < 0.2$; $F(4,155) = 18.01$, $p < 0.001$; $0.2 \leq \varphi < 0.3$; $F(4,155) = 7.030$, $p < 0.001$; $0.3 \leq \varphi < 0.4$; $F(4,155) = 23.77$, $p < 0.001$; $0.4 \leq \varphi < 0.5$; $F(4,155) = 4.888$, $p < 0.01$). Post hoc tests showed that there were significant differences between the highest and lowest quintiles of $\tau_{\text{Decay}}/\text{ISI}$ for all phase ranges (Fig. 7C).

### Temporal dynamics of bistable networks

Most computational studies of mutually inhibitory cells have been deterministic (noise free) by design, yielding a single steady state that can be predicted, either numerically or analytically, by the initial phase condition of the network (van Vreeswijk et al., 1994; Lewis and Rinzel, 2003). The activity of biological cells, however, is subject to both intrinsic and extrinsic sources of noise. Throughout the course of trials in which LI cells were coupled by inhibition, $\varphi$ alternated between the synchronous and antisynchronous ranges, assuming values outside of either range as well. Because $\varphi$ did not coalesce to a single phase range but varied stochastically over time, we wanted to measure the stability of the synchronous and antisynchronous phase ranges and to characterize transitions between them over time.

To measure the stability of the synchronous and antisynchronous phase ranges, we counted clusters of spike pairs occurring consecutively in either range (Fig. 8A) and computed the likelihood that a synchronous or antisynchronous spike pair was part of a cluster of $n$ such spike pairs. The probability that a cluster of size $n$ would occur decreased with constant fractional decrement as cluster size increased (Fig. 8B), as in a geometric series of the form $P_n(n) = \rho_n^0$, $(0 < \rho_n < 1)$, where $P_n(n)$ is the probability that a given $\varphi$ value in phase range $R$ is part of a cluster of $n$ such $\varphi$ values and $\rho_n$ is the constant coefficient of decrement as $n$ increases. Because $\rho_n$ is between 0 and 1, the series $P_n(n)$ decreases exponentially, and $\log(P_n(n))$ decreases linearly with slope $= \log(\rho_n)$. Such linearity was evident in logarithmic plots of cluster distribution for both the synchronous (Fig. 8B, left) and antisynchronous (Fig. 8B, right) states, although antisynchrony was the more stable of the two (note the difference in vertical scale for the antisynchronous versus synchronous cluster plots in Fig. 8B).

The coefficient of decrement, $\rho_n$, was altered by changes in $\tau_{\text{Decay}}/\text{ISI}$, with increases in $\tau_{\text{Decay}}/\text{ISI}$ corresponding, in general, to increases in the stability of the synchronous state and decreases in the stability of the antisynchronous state (Fig. 8B). To investigate how the distributions of synchronous and antisynchronous cluster sizes change as a function of the ratio $\tau_{\text{Decay}}/\text{ISI}$, we computed the cumulative distribution function of synchronous and antisynchronous cluster sizes for each trial and averaged these functions across all trials within quintiles of the inhibitory ratio ($n = 191$ trials for inhibition alone; $n = 160$ trials for inhibition with electrical coupling) (Fig. 8C). In all cases, the highest and lowest quintiles differed significantly from each other ($p < 0.01$; Kolmogorov–Smirnov test), with synchronous cluster size increasing and antisynchronous cluster size decreasing, as $\tau_{\text{Decay}}/\text{ISI}$.
ISI increased. Similar results were obtained for inhibitory coupling and combined inhibitory and electrical coupling (Fig. 8C).

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chronous cluster sizes (i.e., rightward shift of cumulative distribution function) and smaller antisynchronous cluster sizes (i.e., leftward shift of cumulative probability function), compared with inhibition alone (Fig. 8C) [the data for inhibition alone are replotted for the first and fifth quintiles of $\tau_{\text{DECAY}}$/ISI as open squares in the bottom two panels (i.e., compare black squares with black solid line and red squares with red solid line in bottom left and bottom right panels)].

To characterize the transitions between the synchronous and antisynchronous states, we computed the fraction of such transitions occurring in $n$ steps for $n = 1, 2, \ldots, 9$. One-step transitions consisted of an instantaneous switch from one stable state at the $i$th spike pair in the trial to the other stable state at the $(i + 1)$th spike pair, whereas two-step transitions consisted of one stable state at the $i$th spike pair, followed by an intermediate phase value ($0.1 \leq \varphi < 0.4$) at the $(i + 1)$th spike pair, and finally the other stable state at the $(i + 2)$th spike pair. Thus, every $n$ step transition consisted of a chain of $n - 1$ intermediate $\varphi$ values linking one stable $\varphi$ value to another (Fig. 9A). The probability distribution of these transition lengths was described by a decreasing geometric series much like that describing the stability of the two stable states, with the frequency of $n$ step transitions decrementing by a constant coefficient for increasing values of $n$ (data not shown).

Transitions from synchrony to antisynchrony required fewer steps than did transitions from antisynchrony to synchrony, but electrical coupling did not alter transition probabilities for either transition type (Fig. 9B). Networks operating in the highest quintile of $\tau_{\text{DECAY}}$/ISI generally had more abrupt shifts from one stable phase state to the other, as indicated by the lower incidence of long transitions compared with networks operating in the lowest quintile of $\tau_{\text{DECAY}}$/ISI (Fig. 9B). This is consistent with the observation that the stability of the synchronous state is promoted at the expense of less stable intermediate phase states (Figs. 4C, 7C).

**Discussion**

**Comparison with model networks and previous biological studies**

The collective dynamics of mutually inhibitory and electrically coupled neurons has been investigated previously with a variety of analytical and computational approaches (van Vreeswijk et al., 1994; Wang and Buzsáki, 1996; Di Garbo et al., 2002, 2005; Lewis and Rinzel, 2003; Nomura et al., 2003). Such studies have usually predicted that networks of mutually inhibitory neurons will fall into either a synchronous or antisynchronous attractor state, depending on the amplitude and kinetics of inhibitory coupling, as well as on the firing rate of the cells and their initial phase condition. Here, we have taken a direct, experimental approach to determine the extent to which these activity patterns are realized in pairs of biological neurons, using a dynamic-clamp system to couple pairs of interneurons in brain slices of the ACx. As with deterministic models, we found that mutually inhibitory networks had two preferred states: one synchronous (phase lag, $\sim 0$) and the other antisynchronous (phase lag, $\sim 0.5$). Consistent with several of the modeling studies, we found that either increasing the firing rate or prolonging inhibition stabilizes the synchronous state (van Vreeswijk et al., 1994; Di Garbo et al., 2002, 2005; Lewis and Rinzel, 2003; Nomura et al., 2003). Because the basis for these preferred states has been shown in several different models to be a one-dimensional dynamical system with two stable fixed points, we conclude that the bimodal phase distribution we observed in mutually inhibitory cells was most likely generated by such a system. Although it is not possible to assess the stability of the points $\varphi = \sim 0$ and $\varphi = \sim 0.5$ in our experimental system analytically, our results are what one would predict in the case of a bistable system with noise. Thus, although the dynamics underlying these LI networks remain unknown, their behavior is best described as “bistable.”

Electrically coupled model networks usually predict that gap junctions will enhance synchronous firing in a population, although, in some cases, electrical coupling alone has produced bistability and/or antisynchronous phase-locking in models (Chow and Kopell, 2000; Di Garbo et al., 2002; Lewis and Rinzel, 2003; Pfeuty et al., 2003). We found that electrical coupling enhanced synchrony in networks of LI cells, both in the presence and in the absence of inhibitory coupling. Because gap-junction coupling has been shown only to promote antisynchrony in model networks when the suprathreshold component of this coupling was relatively small, we conclude that for the electrical coupling parameters we used, which were based on recordings made from biologically coupled LI cells, the spikes that LI cell pairs generated gave a large enough suprathreshold component to the electrical conductance as to promote synchrony only. This result is consistent with studies of biological gap-junction coupling between cortical cells in vitro (Gibson et al., 1999, 2005; Tamas et al., 2000; Galarreta and Hestrin, 2001; Szabadics et al., 2001; Traub et al., 2001).

A recent study of interneurons coupled by inhibitory chemical synapses and/or gap junctions in LIV of the somatosensory cortex showed that mutually inhibitory networks in this region usually exhibit antisynchrony, but when coupled with both gap junctions and inhibitory chemical synapses, they usually exhibit synchrony (Gibson et al., 2005). As with deterministic models, these LIV networks coalesce to a single phase state during individual trials. In contrast to somatosensory LIV networks and modeling studies, pairs of LI interneurons in the ACx alternated between their two favored states frequently during each trial and did not display precise synchrony or antisynchrony (i.e., $\varphi \equiv 0$ or $\varphi \equiv 0.5$) but instead yielded two distinct phase ranges centered about $\varphi = \sim 0$ and $\varphi = \sim 0.5$, respectively. This difference in the stability and precision of phase may be attributable to differences in the relative contributions of intrinsic membrane noise and coupling strengths, because noise can perturb a bistable network out of the basin of attraction of either stable state, but strong coupling can overcome noise to reinforce the stability of one state or the other. Indeed, electrical coupling in LIV somatosensory networks was reported to be severalfold stronger than in LI networks of the ACx (Fig. 1) (Gibson et al., 1999; Chu et al., 2003). The considerable heterogeneity of membrane and firing properties in LI of the ACx also may contribute to the inability of these networks to remain in a single stable state for long periods.

**Temporal evolution and stability of network phase states**

Because LI networks alternated between two states stochastically, the time evolution of $\varphi$ during these trials was a novel subject of consideration. We found that the temporal stability of the synchronous and antisynchronous phase ranges was described by a decrementing geometric series, with the constant factor of decrement being the probability that $\varphi$ would remain in the range of the state once the range had been entered (Fig. 7B). Because this probability was constant regardless of how many consecutive previous spike pairs had occurred within the range, the time evolution of $\varphi$ in these networks was essentially memoryless beyond one step, such that the phase state of the network at any spike pair in the trial was only dependent on the phase state at the immediately preceding spike pair. This property satisfies the Markov condition of random processes, hence the time evolution of $\varphi$.

Discussion
appears to be a Markov process (i.e., a “random walk” that is described completely by a fixed set of one-step transition probabilities). This was also supported by the observation that the number of unstable intermediate spike pairs occurring in the transition from one stable state to the other also had a distribution characteristic of a geometric series (data not shown).

The observation that LI networks are memoryless suggests that although interneuronal networks in LI have an intrinsic capacity to generate phase-locked oscillatory output, they cannot generate complex temporal firing patterns and may have limited capacity to reflect such patterns even if some are present in the inputs to this layer. Previous in vivo studies suggest that responses of cells in the thalamus that project to LI have poor representations of frequency and time information in the acoustic stimuli (Hu, 2003). Thus, activation of the afferent inputs to LI may reflect changes in the internal state rather than features of the external environment, and networks in this layer may be uniquely suited to modulating or constraining the firing of pyramidal cells with simple inhibitory oscillations. This is consistent with the observation that afferents selectively targeting LI trigger oscillations in the ACx (Brett and Barth, 1997).

**Implications for cortical function and its disruption**

Our results suggest that the modulation of GABAA-mediated IPSCs by endogenous or exogenous agents, such as anesthetic agents, can significantly alter the stability of the synchronous phase state in LI. They also suggest that, in the absence of GABAA receptor modulation, stronger excitatory inputs to LI can induce synchronous firing more readily than weaker inputs can.

Given these results, one might predict that in the non-anesthetized state, LI can respond to large, transient excitatory inputs with a brief period of synchronous firing, thereby synchronizing the activity of widespread cortical targets. Temporal binding mechanisms of this kind offer one possible mechanism by which the cortex might integrate information within and across sensory modalities (Engel and Singer, 2001). LI is also postulated to participate in “event holding” (Vogt, 1991), in which the responses of pyramidal cells in LII–VI to sensory input are temporally amplified by synaptic activation of their distal dendritic tufts in LI when the stimuli are novel or particularly salient. Interneuronal networks in LI might contribute to event holding by entraining the pattern of excitation in these dendritic compartments into a synchronized oscillation, both within and between distinct pyramidal cells. The synchronization properties of LI networks elucidated here, combined with the distinct anatomy of cells in this layer, suggest that LI could play significant roles in such mechanisms.

We found that prolonging the decay time of GABAA receptor-mediated IPSCs allowed more modest amounts of excitation to generate synchronous firing in LI. Because anesthetic agents can greatly suppress the activity of thalamocortical cells (Detsch et al., 1999; Ries and Puil, 1999; Alkire et al., 2000), we predict that in the anesthetized state, LI will respond to this reduced excitation with unusually slow patterns of synchronous inhibition onto its targets over a relatively long time course. Indeed, this may represent the cellular mechanism for the observation that moderate doses of anesthetic agents increase power in the α and β frequency bands (10–30 Hz) recorded from the frontal cortex in the EEG (Gugino et al., 2001). Instead of binding the activity of multiple cortical targets, this inhibition could disrupt the ability of pyramidal cells in the ACx to represent features of the acoustic environment by entraining them into an oscillatory firing pattern not amenable to sensory coding, temporal binding, or event holding. Thus, LI may play a significant role in both generating and, in the case of general anesthesia, disrupting cortical representations of the external environment.

**References**


