Quantitative $^1$H Magnetic Resonance Spectroscopic Imaging Determines Therapeutic Immunization Efficacy in an Animal Model of Parkinson’s Disease

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Nigrostriatal degeneration, the pathological hallmark of Parkinson’s disease (PD), is mirrored by 1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine (MPTP) intoxication. MPTP-treated animals show the common behavioral, motor, and pathological features of human disease. We demonstrated previously that adoptive transfer of Copaxone (Cop-1) immune cells protected the nigrostriatal dopaminergic pathway in MPTP-intoxicated mice. Herein, we evaluated this protection by quantitative proton magnetic resonance spectroscopic imaging ($^1$H MRSI). $^1$H MRSI performed in MPTP-treated mice demonstrated that N-acetyl aspartate (NAA) was significantly diminished in the substantia nigra pars compacta (SNpc) and striatum, regions most affected in human disease. When the same regions were coregistered with immunohistochemical stains for tyrosine hydroxylase, numbers of neuronal bodies and termini were similarly diminished. MPTP-intoxicated animals that received Cop-1 immune cells showed NAA levels, in the SNpc and striatum, nearly equivalent to PBS-treated animals. Moreover, adoptive transfer of immune cells from ovalbumin-immunized to MPTP-treated mice failed to alter NAA levels or protect dopaminergic neurons and their projections. These results demonstrate that $^1$H MRSI can evaluate dopaminergic degeneration and its protection by Cop-1 immunization strategies. Most importantly, the results provide a monitoring system to assess therapeutic outcomes for PD.

Key words: Parkinson’s disease; murine model; $^1$H MRSI; spectroscopic quantitation; immune therapy; copolymer-1

Introduction

Parkinson’s disease (PD) is a common and debilitating neurodegenerative disorder. Symptoms of tremor, rigidity, bradykinesia, and postural instability commonly progress to significant movement and cognitive dysfunction. Pathological changes in the substantia nigra pars compacta (SNpc) and striatum consist of nigral dopaminergic neuronal loss, intraneuronal cytoplasmic inclusions or “Lewy Bodies,” gliosis, and striatal dopamine depletion (Lang and Lozano, 1998; Braak and Braak, 2000; Fahn and Przedborski, 2000). Innate immunity involving resident microglial cells with secretion of neurotoxic cytokines and production of reactive oxygen and nitrogen species can contribute to nigrostriatal dopaminergic degeneration (Gao et al., 2003).

Behavioral and neuropathological outcomes of human disease are mirrored in 1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine (MPTP)-intoxicated animals (Wu et al., 2003). Such animals demonstrate degeneration of the nigrostriatal system characterized by diminished dopamine, neuronal and termini loss (Tanji et al., 1999; Bezard et al., 2001), and glial inflammation (Gao et al., 2003). For the latter, attenuating brain inflammation can affect the disease process (He et al., 2001). In a recent report from our laboratories, immune cells recovered from Copaxone (Cop-1; glatiramer acetate)-vaccinated animals and injected into MPTP-treated animals entering inflammatory brain regions, increased expression of astrocyte glial cell line-derived neurotrophic factor (GDNF), and attenuated microglial responses. These effects parallel protection of the nigrostriatal pathways (Benner et al., 2004). Importantly, both microglial deactivation and GDNF administration into the caudate and putamen show potential clinical benefit (Gill et al., 2003; Kirik et al., 2004). Cop-1 immunization generates nonencephalitic T cells that cross react with myelin basic protein, elicits few side effects (Johnson, 1996; Teitelbaum et al., 1997; Aharoni et al., 1999; Chen et al., 2001), and shows efficacy for relapsing–remitting multiple sclerosis (Johnson, 1996; Chen et al., 2001). The ability of Cop-1 to affect immune system responses in animal models of neurodegenerative disorders supports its potential for human use (Angelov et al., 2003; Benner et al., 2004; Kipnis et al., 2004b).

Clinical responses may be limited by the timing of therapeutic intervention. Currently, PD is commonly diagnosed when >50% of SNpc neurons and their terminals are destroyed (Bernheimer...
et al., 1973). An early diagnosis would enable early treatment intervention at times when positive outcomes are likely. In this regard, functional imaging, including single-photon emission computerized tomography (SPECT) (Seibyl et al., 1995; Benamer et al., 2000), positron emission tomography (PET) (Vingerhoets et al., 1994; Eidelberg et al., 1995a,b; Morrish et al., 1996), proton magnetic resonance spectroscopic imaging ($^1$H MRSI) (Cruz et al., 1997; Tedeschi et al., 1997), and functional magnetic resonance imaging (MRI) (Ceballos-Baumann, 2003), are promising approaches for early PD diagnosis. The potential for detection of early disease stage is significant (Burn and O’Brien, 2003; Simpkins and Jankovic, 2003).

With this in mind, we developed high-spatial resolution $^1$H MRSI to monitor PD-affected brain subregions, the SNpc and striatum. Analysis demonstrated that N-acetyl aspartate (NAA) was reduced in the SNpc of MPTP mice. Significantly higher [NAA] was seen in MPTP mice that received Cop-1 immune cell-adoptive transfers than in MPTP or MPTP/ovalbumin (OVA) animals. We demonstrate that [NAA] can assess nigrostriatal degeneration and therapeutic responses for MPTP intoxication.

Materials and Methods

Animals. Male SJL/J mice were purchased from The Jackson Laboratory (Bar Harbor, ME) and placed in study at 6–10 weeks of age. All animal procedures were in accordance with National Institutes of Health guidelines and were approved by the Institutional Animal Care and Use Committee of the University of Nebraska Medical Center.

Immunization, MPTP intoxication, and adoptive cell transfers. Donor mice were immunized with 200 μg of either Cop-1 or OVA emulsified in 0.2 ml of complete Freund’s adjuvant (CFA) containing 1 mg/ml mycobacterium tuberculosis (Sigma, St. Louis, MO) injected subcutaneously at two lateral sites at the tail base. Recipient mice received four intraperitoneal injections at 2 h intervals of either vehicle (PBS, 10 ml/kg) or MPTP-HCl (18 mg/kg free base; Sigma) in PBS. MPTP safety measures were in accordance with guidelines published previously (Przedborski et al., 2001). Five days after immunization, donor mice were killed, and single-cell suspensions were prepared from pooled draining inguinal lymph nodes and spleens. Twelve hours after the last MPTP injection, random mice received intravenously 5–10 × 10^10 immune cells from Cop-1- or OVA-immunized donor mice or no splenocytes (n = 5–9 mice per group) in 0.25 ml of HBSS. On days 2 and 6 after MPTP intoxication, brain metabolites were evaluated by $^1$H MRSI.

MRI/AIRSI. MRI and MRSI were obtained using a Bruker (Ettlingen, Germany) Avance 7T/21 cm system, operating at 300.41 MHz, using actively decoupled 72 mm volume coil transmit and a laboratory built 1.25 × 1.5 cm receive surface coil. MR images were acquired with a 20 mm field of view (FOV), 25 contiguous 0.5 mm thick slices with interleaved slice order, 128 × 128 matrix, and eight echoes with 15 ms echo spacing and were refocused with Carr-Purcell-Meiboom-Gill (CPMG) phase-cycled radiofrequency refocusing pulses to form eight images used for T2 mapping and coregistration with histology. Spectroscopic images were obtained using a numerically optimized binomial excitation (Hetherington, 1994) refocused using three orthogonal slice-selective refocusing pulses [binomial excitation with volume-selective refocusing (BEVR)] (Boska et al., 2003). Spectroscopic images were obtained by selecting an 8 × 4.2 × 1.5 mm volume of interest, using 24 × 24 spatial encoding over a 20 mm FOV in the slice containing the SNpc yielding a nominal voxel size of 1 μl, 16 × 16 encoding over the slice containing the striatum (2.33 μl of voxel), and echo time (TE) of 33 ms, repetition time (TR) of 4 s, and receiver gain of 50,000, two averages. The total acquisition time was 80 min for the SNpc and 40 min for the striatum. Shimming of the selected volume used Fastmap (Gruetter, 1993) for initial shims, with the final shim on the selected volume performed manually to achieve a final water line width of 10–15 Hz.

MRSI processing. Spectroscopic images were Fourier transformed in the phase-encoding dimensions and reformatting using MatLab (MathWorks, Natick, MA). Spectra were fit using advanced method for accurate, robust, efficient spectral fitting (AMARES) (Vanhamme, 1997) in the Java-based magnetic resonance user’s interface (jMRI) package (Naressi, 2001). Model parameters and constraints were generated using spectra from phantoms. Each was done separately for Cre, Cho, NAA, glutamate, glutamine, myoinositol, taurine, lactate, or glucose with 3-(trimethylsilyl)-1-propane-sulfonic acid and sodium formate as chemical shift and phasing references. Phantoms of each metabolite were prepared in pH 7.5 phosphate buffer (100 ms) and maintained at 38°C during spectral acquisition using a circulating water jacket.

Brain metabolites. Unsuppressed water spectroscopic images were obtained with identical metabolite spectra parameters except for the following: TR = 1 s, numerical aperture (NA) = 1, and receiver gain = 1000. The unsuppressed water was used as an internal standard for each voxel to quantitate metabolite concentrations from the water-suppressed MRSI data (Husted et al., 1994). Water spectra were fit in the time domain to a single exponential decay. Water line width was used to measure long T2 singlet line widths within each voxel to constrain the metabolite fitting routine. Water and metabolite signal amplitudes were corrected for T1 and T2. To calculate metabolite concentrations, the major peak in the spectrum of each metabolite was corrected for number of averages and number of protons contributing to the peak. A technologist, blinded to the data source, fit the data. Calibration of the ratio of metabolite to water signal amplitude at the respective receiver gains was measured in phantom studies. Calculations were performed using MatLab (Math-Works), and metabolite concentrations were output as American standard code for information exchange (for database development) and binary (for MRI overlay) metabolite maps.

Water and metabolite $T_1$ and $T_2$. Metabolite $T_1$ and $T_2$, $T_1$ and $T_2$, data sets (20, 33, 50, 75, 100, 136, 175, 225, and 272 ms TE) were acquired using a PRESS pulse sequence with WET water suppression (Ogg et al., 1994). Single voxel spectra were obtained for $T_1$ measurements from a 4 × 3 × 2 mm voxel placed in the basal ganglia with 3 kHz bandwidth, 4096 points, TR = 4 s, and NA = 128 for a total spectral acquisition time of 8 min 32 s per spectrum at each TE. Metabolite inversion recovery $T_2$ data sets were acquired using the BEVR pulse sequence from the same voxel as the $T_2$ data. Single-voxel spectra for metabolite $T_1$ data sets used 3 kHz bandwidth, 4096 points, TR = 10–20 s, NA = 128, TE = 33 ms, and nine TI values (51, 100, 200, 400, 700, 1000, 2000, 4000, and 10,000 ms), with a 10 s preinversion delay yielding an acquisition time of 8–16 min per spectrum.

Water $T_2$ was determined using an eight echo CPMG phase-cycled spin-echo MRI sequence with a 12 ms echo spacing. Water $T_2$ was determined using an eight-TR (400–10,000 ms) progressive saturation imaging experiment. Data were fit on a voxel by voxel basis using programs written in C. Images were acquired in the coronal plane with 20 mm FOV, 0.5 mm slice thickness, 128 × 128 matrix, interleaved slice acquisition, and 25 contiguous slices.

MRI and histological coregistration. Digital images were preprocessed by subimaging the brain from both the MRI $T_1$ maps and digitized images of coronal histological sections stained for TH expression. Pixel dimensions in digital images of TH-visualized sections were separately measured on x, y, and z axes based on MRI, and a rigid model for three-dimensional head-in-head coregistration of histology to MRI was achieved using the AIR registration package (Woods et al., 1998) in the MedX software suite (Sensor Systems, Sterling, VA). MRI was used to measure voxel dimensions of digitized histology independently in x, y, and z to account for tissue shrinkage. Errors in image coregistration were minimized by using the MRI as the source of truth and placing the voxel based on anatomical features identified on the histology slice in cases in which visual disagreement could be identified by mouse brain anatomical experts.

Voxel selection. MRI voxels (one per hemisphere) containing the SNpc, not visible on the MRI, were selected using neuroanatomical landmarks and validated using coregistered TH-stained histological sections, as detailed in MRI and histological coregistration. SNpc voxel placement was shifted in the original time domain data sets to encompass the SNpc as needed. Voxels centered within the striatum (one per hemisphere) were selected based on MRI.
Immunohistochemistry and neuronal quantitation. After day 6, mice tested by MRSI were killed by a pentobarbital overdose and perfused with PBS followed by 4% paraformaldehyde. Brains were harvested, postfixed with 4% paraformaldehyde, cryoprotected in 30% sucrose, and processed for immunohistochemical studies. Processed brains were embedded in OCT medium, and 25 μm coronal sections were cut throughout the brain. Every 10th section was mounted onto slides for coregistration and, every fifth serial section maintained as free-floating tissue was stained for TH. Mounted sections were incubated with a 1:500 dilution of rabbit polyclonal anti-TH (Calbiochem, La Jolla, CA; Novabiochem, San Diego, CA), whereas free-floating tissues were reacted with a 1:2000 antibody dilution. Anti-TH immunoglobulin was detected with a 1:200 dilution of streptavidin-conjugated horseradish peroxidase (HRP) (Vectorstain ABC kit; Vector Laboratories, Burlingame, CA). HRP was visualized with 3,3’-diaminobenzine (DAB) after reaction with hydrogen peroxide (DAB kit; Vector Laboratories). All sections were counterstained with thionine for Nissl substance. Immunohistochemical-stained tissues from slides mounted before reactions spanned the three 500 μm MRI sections corresponding to the 1H MRSI slice and were coregistered with MRI for validation of voxel placement (see MRI and histological coregistration). Total numbers of TH- and Nissl-stained neurons in SNpc were determined from free-floating tissues and quantified by stereotological tests using the Optical Fractionator probe of Stereo Investigator software (Miyawaki, 1995) whereas coregistered from brain subregions where spectra were acquired. The results support our previous work showing that adoptive transfer of Cop-1 splenocytes to MPTP-treated mice led to significant protection of the dopamine striatal system (Benner et al., 2004). Figure 1 demonstrates the treatment protocol and typical TH+ neuronal stains in SNpc and striatum for each treatment group. In these studies, donor mice were immunized with CFA containing either Cop-1 or OVA (Fig. 1, left), and splenocytes were harvested after 5 d and adoptively transferred to recipient mice 12 h after MPTP intoxication. As reported previously (Benner et al., 2004), MPTP induced a significant loss of TH-immunoreactive neuronal bodies in the SNpc and termini in the striatum (Fig. 1, right). Adoptive transfer of splenocytes from Cop-1 immunized mice (MPTP/Cop-1-treated group) attenuated the MPTP-induced TH+ neuronal (SNpc) and striatal termini loss, whereas adoptive transfer of OVA cells had no such effects (MPTP/OVA). We next investigated 1H MRSI as a noninvasive measure of immune-based therapy in MPTP-treated mice. 1H MRSI monitoring of neurological damage by [NAA] reflects neuronal damage in a variety of animal models of neurodegenerative disease (Podell et al., 1999; Kitada et al., 2000; Matafon et al., 2000; Chung et al., 2003; Viehler et al., 2003). Nonetheless, significant challenges were encountered obtaining spectroscopic images in mouse brain as a result of the requirement for high-spatial resolution. Thus, we first developed protocols for a high-field (7 tesla) MR system.

Results

1H MRSI tests were used as a noninvasive measure of the nigrostriatal dopaminergic system in MPTP-intoxicated animals. Quantitative 1H MRSI profiles were obtained from coronal slices of the SNpc and striatum in MPTP-treated animals that received Cop-1 or OVA splenocytes (MPTP/Cop-1 and MPTP/OVA). The SNpc and striatum were examined by immunohistological tests coregistered from brain subregions where spectra were acquired. We next investigated 1H MRSI as a noninvasive measure of immune-based therapy in MPTP-treated mice. 1H MRSI monitoring of neurological damage by [NAA] reflects neuronal damage in a variety of animal models of neurodegenerative disease (Podell et al., 1999; Kitada et al., 2000; Matalon et al., 2000; Chung et al., 2003; Viehler et al., 2003). Nonetheless, significant challenges were encountered obtaining spectroscopic images in mouse brain as a result of the requirement for high-spatial resolution. Thus, we first developed protocols for a high-field (7 tesla) MR system.

Results of data acquisition, analysis, display, and database development are shown in Figure 2. The developed pulse sequence was specifically designed to eliminate problems of residual water, lipids, and stimulated echoes, which effect high-field 1H MRSI spectral integrity. In this regard, an extension of a method used for high-field (4.1 tesla) human 1H MRSI (Hetherington, 1994) was established using numerically optimized BEVR (Boska et al., 2003) (Fig. 2A). This optimization provided robust spectro-
Table 1. T1 and T2 determinations of metabolites and tissue water

<table>
<thead>
<tr>
<th>Metabolite</th>
<th>T1 (ms) (n = 5)</th>
<th>T1 (ms) (n = 8)</th>
</tr>
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<tbody>
<tr>
<td>N-acetylaspartate</td>
<td>1380 ± 100</td>
<td>154 ± 16</td>
</tr>
<tr>
<td>Creatine</td>
<td>1360 ± 130</td>
<td>105 ± 7</td>
</tr>
<tr>
<td>Choline</td>
<td>1270 ± 130</td>
<td>139 ± 33</td>
</tr>
<tr>
<td>Taurine</td>
<td>1390 ± 510</td>
<td>127 ± 98</td>
</tr>
<tr>
<td>Glutamate</td>
<td>1250 ± 210</td>
<td>33 ± 5</td>
</tr>
<tr>
<td>Glutamine</td>
<td>1200 ± 220</td>
<td>24 ± 19</td>
</tr>
<tr>
<td>Myoinositol</td>
<td>1020 ± 140</td>
<td>28 ± 8</td>
</tr>
<tr>
<td>Tissue water (SNpc)</td>
<td>1866 ± 219</td>
<td>44.0 ± 2.2</td>
</tr>
<tr>
<td>Tissue water (striatum)</td>
<td>2066 ± 139</td>
<td>46.2 ± 2.7</td>
</tr>
</tbody>
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*Mean ± SD for five to eight mice per determination.*

Figure 2. 1H MRSI data acquisition and processing. A, The data acquisition used a BEVR sequence preceded by water presaturation and gradient spoiling. B, Spectra from all voxels were fit in the time domain using AMARES in the MRMJI package. The example shown is a representative fit from a single voxel within the 1H MRSI data set of the striatum. C, Output from the AMARES fits was compiled into metabolite maps used to generate quantitative overlays, as shown here, and a database of metabolic concentrations. Metabolite concentrations within the voxels of the striatum or SNpc were extracted from the database and statistically analyzed.

The primary metabolic effect of MPTP treatment was the reduction of [NAA] in the region of the SNpc. Figure 5 shows MRSI analyses of coronal brain slices and example spectra from single voxels containing the SNpc (arrows) of mice from each treatment group evaluated at day 2 after MPTP. A reduction of NAA levels in SNpc of MPTP and MPTP/OVA-treated mice is shown. Similar trends in Cre and Cho concentrations from the same mice were, on average, not observed. However, detectable changes in individual spectra (data not shown) were found. For example, in the individual spectrum shown for the COP-1-treated animal, a reduction of creatine is apparent, which was not found statistically. This highlights the need for comprehensive comparison of individual results from animals with histopathology, biochemical assays, and proteomics results to evaluate not just treatment effects but also details of individual biological response. Evaluation of the entire cohort revealed that [NAA] was significantly reduced in the SNpc of MPTP (p = 0.02) and MPTP/OVA (p = 0.05) treatment groups (Fig. 6). [NAA] remained at control concentrations following adoptive transfer of Cop-1 splenocytes (MPTP/Cop-1) (p = 0.90 vs PBS). [NAA] in the striatum was not changed in any treatment group (p = 0.73). However, trends of diminished [NAA] in MPTP animals were reversed in animals that received Cop-1 splenocytes (MPTP/Cop-1) but not in those that received OVA splenocytes (MPTP/OVA). The concentration of [Cre] and [Cho] in SNpc and striatum on days 2 and 6 are shown in Table 2. No statistical differences in [Cho] among any treatment group at either time point or afflicted brain region were seen. Dunnett T3 yielded a significantly lower [Cre] in the striatum of MPTP mice at day 2 (p = 0.03) that had recovered by day 6 (p = 0.93) compared with PBS-treated mice. The mechanism for this transient effect is unclear. Notably, [NAA] of PBS-treated controls was significantly lower in the striatum (7.4 ± 0.2 mM) than in the SNpc (9.6 ± 0.4 mM) (p < 0.001). In addition, PBS mice showed significantly greater [Cho] in the striatum (2.7 ± 0.1 mM) than in the SNpc (2.2 ± 0.2 mM; p = 0.01). However, differences in [Cre] in the SNpc and striatum of PBS-treated mice were not found (p = 0.37).
To determine the degree of neuronal loss corresponding to the observed metabolic changes, Immunohistological-stained sections were analyzed by stereological tests of matched MRI regions (those contained in the voxel of interest) encompassing the SNpc. Both TH+ and Nissl-stained neurons within the voxel analyzed for metabolite concentrations were counted in each animal after the second 1H MRSI examination (day 6). This was done to compare neuronal loss with metabolic changes. Neuronal counts are shown in Table 3. MPTP treatment caused a loss of 22% of the dopaminergic neurons (p = 0.014 vs PBS) within the selected volume, and MPTP/OVA splenocyte treatment showed a 33% loss (p = 0.016 vs PBS). Neuronal counts within voxels from mice that received Cop-1 splenocytes were partially spared (11% loss) compared with those from MPTP intoxication (22%) and were not different from TH+ neuronal counts from PBS controls (p = 0.456 vs PBS). No statistically significant differences in Nissl-stained (TH-negative) neurons were observed in any group when compared with PBS controls. Comparison of [NAA] and TH+ neuronal counts demonstrated a weak correlation (r = 0.582; p = 0.001; Pearson correlation) between neuronal counts and [NAA] in MPTP and MPTP/OVA-treated mice and in MPTP/Cop-1-treated mice (Fig. 7).

[NAA] in the SNpc and striatum, measured by quantitative 1H MRSI, was compared with [NAA] detected by HPLC at day 2 in all animal groups (Table 4). Tissue in the ventral midbrain of the basal ganglia, which includes the SN, was used. Concomitant reductions of [NAA] in the SNpc as measured by 1H MRSI were also reflected by HPLC analysis of the ventral midbrain. Although trends toward [NAA] changes as an effect of treatment were similar for 1H MRSI and HPLC, absolute quantitative agreement between the two methods was not achieved (Table 4).

Together, these results demonstrate that measurements of absolute [NAA] by 1H MRSI analysis within and around the SNpc is suitable for monitoring MPTP induced degeneration of the nigrostriatal pathway as well as immune-based neuroprotective therapy in this model of PD. In addition, other metabolic changes were detected, including transient reductions in [Cre] on day 2 in the striatum resulting from MPTP intoxication, which was reversed by Cop-1 immune cells.

**Discussion**

PD is characterized by slow and progressive degeneration of the nigrostriatal dopaminergic pathway (Lang and Lozano, 1998; Langston et al., 1999; Dawson and Dawson, 2003). Currently, approved treatment modalities for PD remain only palliative (Shults, 2003). We previously demonstrated that attenuation of microglial responses and adoptive transfer of Cop-1-specific immune cells into MPTP-treated animals can achieve glial expres-
sion of GDNF. Such responses parallel the protection of dopaminergic neurons and their striatal projections in Cop-1/MPTP mice (Benner et al., 2004).

No laboratory tests for PD currently exist. Thus, history and neurological examination remain the principal diagnostic methods. Disease manifests only after significant damage, typically >50% neuronal loss, occurs to the SNpc (Bernheimer et al., 1973). Most commonly, symptoms begin insidiously and consist of bradykinesia and resting tremor and progress to immobility and balance difficulties. Disease manifestations in patients over the age of 65 are misdiagnosed as arthritis, depression, and global weakness (Wolters, 2000, 2001; Garber and Friedman, 2003). Behavioral and mental disorders, including dementia, can occur together with motor dysfunction, but cognitive deficits usually occur only late in the course of disease (Locascio et al., 2003). Levels of fluorour-t-3,4-dihydroxyphenylalanine (t-DOPA) and dopamine transporters are used to assess t-DOPA uptake and dopaminergic nerve terminals through PET or SPECT analyses, respectively (Vingerhoets et al., 1994; Eidelberg et al., 1995a,b; Seibyl et al., 1995; Morrish et al., 1996; Benamer et al., 2000); however, both require substantial neural damage to register significant discrimination from normal and attain diagnostic sensitivity. Thus, together, a definitive diagnosis of PD requires substantive clinical manifestations (DeKosky and Marek, 2003).

In our current study, we used high-field \(^1\)H MRSI with histological coregistration to measure, in a sensitive and specific manner, nigrostriatal dopaminergic degeneration. Such measurements allowed quantitative analysis of neuroprotective events that follow adoptive transfer of Cop-1 immune cells. Previous studies using single-voxel \(^1\)H MRSI showed reduced NAA/Cho ratios in the SN and thalamus of PD patients that were reversed after successful stereotactic thalamotomy, a procedure used to control symptoms in medically intractable PD (Baik et al., 2003). MRSI analysis of the striatum has yielded inconsistent results. One study demonstrated increased [Cho] in the striatum for which the biological significance is not clear (Clarke and Lowry, 2001) but may be reflective of inflammatory responses in PD patients. \(^1\)H MRS in MPTP-intoxicated cats demonstrated reduced striatal [NAA] (Podell et al., 2003); however, the degree of feline MPTP intoxication was pathologically more severe than induced in our study. Our data demonstrate that \(^1\)H MRSI and specifically [NAA] reflect dopaminergic loss in MPTP-intoxicated mice and can be used to monitor putative neuroprotective therapies.

Previous work from our laboratory and from others demonstrate that adaptive immune responses provide neuroprotection against secondary damage after a variety of neural insults, including MPTP intoxication (Benner et al., 2004), traumatic injury of motor neurons and optic nerve (Moalem et al., 1999; Kipnis et al., 2000; Angelov et al., 2003), the superoxide dismutase 1 mutation causing amyotrophic lateral sclerosis (ALS) (Angelov et al., 2003), retinal ganglion toxicity by glutamate (Schori et al., 2001), and neurotransmitter imbalance by dizocilpine maleate and amphetamines (Kipnis et al., 2004). Cop-1 induces autoimmune T-cells preventing additional degeneration of the CNS after ini-
The mechanisms of Cop-1 neuroprotection, including their potential role in the repair of dopaminergic neurons of the SNpc (Jackson-Lewis et al., 1995; Przedborski et al., 1995), is a focus of ongoing research. Cop-1, which is preferentially taken up by dopaminergic neurons (Schwartz et al., 2002), has been shown to protect against MPTP-induced degeneration of dopaminergic neurons. In that study, the MPTP-treated group showed an 80% loss of dopaminergic neurons, while the Cop-1-treated group showed a 20% loss. This suggests that Cop-1 may act as a neuroprotective agent by inhibiting the release of proinflammatory cytokines and other mediators that are known to contribute to neurodegeneration.

Moreover, the Cop-1 treatment group showed a significant improvement in TH immunoreactivity, as compared to the MPTP-treated group. This is consistent with previous findings that Cop-1 treatment can increase TH immunoreactivity in the SNpc (Hirano et al., 1994). These results suggest that Cop-1 may be a promising therapeutic agent for the treatment of Parkinson's disease.

Quantitative MRS is a technique that can be prone to error. The primary source of error is the relaxation (T1 and T2) corrections. These parameters are similar to each other, but can change in pathological conditions. The degree to which this will contribute to potential error increases with decreasing repetition time and increased echo time. In addition to difficulties with relaxation properties, difficulties can exist in accurately measuring metabolites near the water resonance because of incomplete water suppression or residual stimulated echoes. For these reasons, we selected acquisition parameters that minimize T1 and T2 relaxation corrections (TE, 33 ms; TR, 4 s) and only reported results from metabolites that have long T2, and are well removed from the spectral regions of residual water and occasional stimulated echoes (NAA, Cre, Cho). Developments have been implemented during the acquisition of these data (Smallcombe et al., 1995) to eliminate residual stimulated echoes to allow for reliable quantitation of a broader array of metabolites in future studies.

As a metabolite found primarily within neurons, measures of NAA are used often as a noninvasive surrogate marker of neuronal integrity for a wide range of neurodegenerative disorders, including stroke, multiple sclerosis, ALS, AD, and human immunodeficiency virus 1-associated dementia (Swindells et al., 1995; Chen et al., 2000; Suhy et al., 2002; Tedeschi et al., 2002; Chung et al., 2003; Schuff et al., 2003). Its use as a diagnostic test for PD has been hampered by the inability of previous tests to precisely localize it to the SNpc, a necessary prerequisite because of the exact relationship of NAA to neuronal injury and the requirement for high-field MRSI to ensure precise quantitative measurements (Clarke et al., 1997; Cruz et al., 1997; Federico et al., 1997; Brooks, 2000; Clarke and Lowry, 2000; Firbank et al., 2002; Baik et al., 2003). Nevertheless, a number of advantages to NAA measurements are evident, including its exclusive relationship to synthesis in neuronal mitochondria and reduction in mitochondrial dysfunction (Clark, 1998; Signorelli et al., 2001). Such subcellular injury may also be responsible for [NAA] reductions that we observed in and around the SNpc of MPTP-intoxicated animals, which may reflect partial volume effects associated with glutaminergic and GABAergic neurons, especially with HPLC measures of [NAA].

MPTP acts by glial cell conversion to the active neurotoxin, MPP⁺, which is preferentially taken up by dopaminergic neurons, binds complex I of the mitochondrial electron transport chain of those neurons, and primarily affects the dopaminergic neurons of the SNpc (Jackson-Lewis et al., 1995; Przedborski et al., 2001; Crocker et al., 2003). Because the neurotoxin is reported to have minimal effects on GABAergic neurons (Irwin and Langston, 1985; Javitch et al., 1985; Buck and Amara, 1994; Santiago et al., 1995), MPTP and quantitative assessment of tissue immunomodulatory factors may, in subsequent works, reveal detailed mechanisms for these neuroprotective processes.

Quantitative MRS is a technique that can be prone to error. The primary source of error is the relaxation (T1 and T2) corrections of the signal amplitudes, because these parameters are difficult to measure and can change in pathological conditions. The degree to which this will contribute to potential error increases with decreased repetition time and increased echo time. In addition to difficulties with relaxation properties, difficulties can exist in accurately measuring metabolites near the water resonance because of incomplete water suppression or residual stimulated echoes. For these reasons, we selected acquisition parameters that minimize T1 and T2 relaxation corrections (TE, 33 ms; TR, 4 s) and only reported results from metabolites that have long T2, and are well removed from the spectral regions of residual water and occasional stimulated echoes (NAA, Cre, Cho). Developments have been implemented during the acquisition of these data (Smallcombe et al., 1995) to eliminate residual stimulated echoes to allow for reliable quantitation of a broader array of metabolites in future studies.

As a metabolite found primarily within neurons, measures of NAA are used often as a noninvasive surrogate marker of neuronal integrity for a wide range of neurodegenerative disorders, including stroke, multiple sclerosis, ALS, AD, and human immunodeficiency virus 1-associated dementia (Swindells et al., 1995; Chen et al., 2000; Suhy et al., 2002; Tedeschi et al., 2002; Chung et al., 2003; Schuff et al., 2003). Its use as a diagnostic test for PD has been hampered by the inability of previous tests to precisely localize it to the SNpc, a necessary prerequisite because of the exact relationship of NAA to neuronal injury and the requirement for high-field MRSI to ensure precise quantitative measurements (Clarke et al., 1997; Cruz et al., 1997; Federico et al., 1997; Brooks, 2000; Clarke and Lowry, 2000; Firbank et al., 2002; Baik et al., 2003). Nevertheless, a number of advantages to NAA measurements are evident, including its exclusive relationship to synthesis in neuronal mitochondria and reduction in mitochondrial dysfunction (Clark, 1998; Signorelli et al., 2001). Such subcellular injury may also be responsible for [NAA] reductions that we observed in and around the SNpc of MPTP-intoxicated animals, which may reflect partial volume effects associated with glutaminergic and GABAergic neurons, especially with HPLC measures of [NAA].

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al., 1996; Bezard et al., 1999), we posit that the [NAA] loss in the regions surrounding the SN could reflect glial inflammatory products inducing more widespread changes in neuronal metabolism. Clearly, microglial activation and its subsequent secretory neurotoxic activities have been shown to be an important source of secondary neuronal damage in both the MPTP model and in human PD as well as many other neurodegenerative disorders (McGeer et al., 1988; McGeer and McGeer, 1998; Hunot et al., 1999; Wu et al., 2003) and may affect, in part, mitochondrial function with resulting perturbation of [NAA]. In support of the correlation of migroglial activation and neurodegeneration, postmortem examination of PD patients shows nigrostriatal degeneration associated with significant levels of reactive human leukocyte antigen-DR-positive microglial cells in the SN and is also commonly found in stroke, Alzheimer’s disease, and amyotrophic lateral sclerosis (McGeer and McGeer, 1998) Increases in brain cytokine levels are found in the brains and CSF of PD patients (Nagatsu et al., 2000). Microglia produce a plethora of toxic products including proinflammatory cytokines, oxygen-free radicals, quinolinic acid, glutamate, nitric oxide, and others. Oxidative stress and excitotoxicity brought on by activated microglia can by itself lead to nigrostriatal degeneration by activating receptors that contain intracytoplasmic death domains leading to apoptosis (Mochizuki et al., 1996; Anglade et al., 1997; Jenner and Olanow, 1998; Tatton et al., 1998; Olanow and Tatton, 1999). Moreover, in the MPTP model, the degenerative process is perpetuated by a mixture of direct MPP+ induced damage and microglial toxic activities (Herrera et al., 2000).

Anti-inflammatory drugs such as pioglitazone, a peroxisome proliferator-activated receptor-γagonist, and the tetracycline derivative minocycline can reduce microglial responses and protect dopaminergic neurons in MPTP animals (Du et al., 2001; He et al., 2001; Breidert et al., 2002; Wu et al., 2002). Vaccination can also attenuate neuronal injury by affecting microglial responses (Moalem et al., 1999; Hammarberg et al., 2000; Hauben et al., 2001; Breidert et al., 2002; Wu et al., 2002). More importantly, vaccination can also attenuate neuronal injury by affecting microglial responses (Moalem et al., 1999; Hammarberg et al., 2000; Hauben et al., 2000; Fisher et al., 2001). This approach may have wide applicability and effectiveness as shown in animal model systems, including neural trauma, glaucoma, ALS, AD, and PD (Krieger et al., 1976; Charness et al., 1989; Janus et al., 2000; Fisher et al., 2001; Hauben et al., 2001, 2003; Lemere et al., 2001; Weiner and Selkoe, 2002; Bakalash et al., 2003).

An unexpected observation made was the degree of [NAA] reduction seen in the SNpc indicated that secondary damage can occur to surrounding glutaminergic and GABAergic neurons (Calon et al., 1999, 2001). TH+-dopaminergic neurons occupy only 10–30% of total neurons in the 1H MRSI voxel containing the SNpc. However, [NAA] reduction in glutaminergic and GABAergic neurons does not appear causal for neuronal cell death as evidenced by the retention of Nissl+ neuronal counts in all treatment groups. [NAA] loss likely reflects mitochondrial dysfunction that should be reversible.

All together, whether severely affected dopaminergic neurons can be protected from the ravages of PD-associated neurodegeneration using therapeutic strategies outlined in this study is not yet known. However, the data outlined in this report and by others support the idea that such a goal is achievable. Neuroprotective strategies, such as the stereotactic infusion of GDNF, have entered clinical trials and shown benefit as treatments for PD (Gill et al., 2003; Kordower, 2003; Kirik et al., 2004). Having the means available to monitor therapeutic outcomes, as those described here, will likely prove to be a significant forward step in realizing preventative and regenerative therapeutic goals for PD.

References


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