

Transistor Probes Local Potassium Conductances in the Adhesion Region of Cultured Rat Hippocampal Neurons

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Adhesion interactions of neurons in a tissue may affect the ion conductance of the plasma membrane, inducing selective localization and modulation of channels. We studied the adhesion region of cultured neurons from rat hippocampus as a defined model where such effects could be observed electrophysiologically, taking advantage of extracellular recording by a transistor integrated in the substrate. We observed the K^+ current through the region of soma adhesion under voltage-clamp and compared it with the current through the whole cell. We found

that the specific A-type conductance was depleted, even completely, in the region of adhesion, whereas the specific K-type conductance was enhanced up to a factor of 12. The electrophysiological approach opens a new way to investigate targeting of ion channels in the cell membrane as a function of adhesion processes.

Key words: transistor; potassium; conductance; channel, localization; A-type; K-type; adhesion

Specific sorting of potassium conductances in the plasma membrane is essential for the integrative properties of hippocampal neurons (Storm, 1990; Debanne et al., 1997; Hoffman et al., 1997; Magee, 1998; Martina et al., 1998). Biochemical and genetic studies suggest that voltage-gated ion channels are localized in appropriate domains through direct or indirect interactions with extracellular adhesion molecules (Isom et al., 1995; Irie et al., 1997; Sheng and Wyszynski, 1997; Thomas et al., 1997; Zito et al., 1997). Until now, however, it was not possible to measure the local electrophysiological properties of the cell membrane in a region of adhesion.

With respect to the complex cell–cell and cell–extracellular matrix contacts *in vivo*, neurons cultured on a coated solid substrate represent a simple model in which the membrane interacts with known adhesion molecules. In the present paper we examine the following question: are there different ion conductances on the upper and lower membrane of a neuron in culture that are exposed, respectively, to the culture medium on one side and in contact with the substrate on the other side? To answer the question, the membrane conductance of the attached membrane of a cultured neuron was studied without disturbing its adhesion to the substrate. We took advantage of the novel method of transistor recording (Fromherz et al., 1991; Fromherz, 1999). There a field-effect transistor is integrated in a silicon substrate beneath a continuous surface of inert silica. It detects the local extracellular voltage in the cleft between the substrate and a cultured cell as it arises from ionic currents through the adherent cell membrane that flow along the resistance of the cleft (Schätz-

thauer and Fromherz, 1998; Vassanelli and Fromherz, 1998). We chose cultured neurons from rat hippocampus (Banker and Cowan, 1977). They had been characterized in detail with respect to their potassium currents by impaled microelectrodes (Segal and Barker, 1984; Segal et al., 1984) and by whole-cell patch-clamp (Ficker and Heinemann, 1992; Klee et al., 1995, 1997). We focused on the fast-inactivating A-type and the slow-inactivating K-type currents, which were discriminated by electrophysiological and pharmacological methods (Storm, 1990; Ficker and Heinemann, 1992; Klee et al., 1995). These currents seem to be related to the expression of various voltage-gated potassium channels (Sheng et al., 1992, 1994; Maletic-Savatic et al., 1995; Veh et al., 1995; Bossu and Gähwiler, 1996; Murakoshi and Trimmer, 1999).

MATERIALS AND METHODS

Neurons. Neurons were dissociated from the hippocampi of Wistar rats (Thomae, Biberach, Germany) at 18 d gestation (Banker and Cowan, 1977). They were preplated twice to get rid of glia cells and suspended in DMEM with glutamax I (no. 61965026, Gibco, Eggenstein, Germany) supplemented with 10% (vol) fetal bovine serum (10106078, Gibco) and 1% (vol) penicillin (15140114, Gibco) (Brewer et al., 1993; Vassanelli and Fromherz, 1998). The final concentration was 350,000 cells per milliliter.

Cell culture on chips. A chamber of perspex (bottom diameter 3 mm) was attached to a silicon chip (1 cm × 1 cm) with integrated transistors. The surface of the chip was wiped carefully with a 1% solution of a liquid dish detergent, rinsed with milli-Q water (Millipore, Bedford, MA), dried, and sterilized with UV light. The chips were coated with poly-L-lysine (molecular weight >300,000; Sigma, Heidelberg, Germany) by adsorption from a 20 μ g/ml aqueous solution for 1 h and dried. Fibronectin (Sigma) was adsorbed from a 10 μ g/ml solution in PBS at 4°C overnight, with subsequent rinsing. We applied 350 μ l of the cell suspension to a chamber. Leibovitz L-15 medium (100 μ l) with glutamax I (31415029, Gibco) supplemented with 5% fetal bovine serum were added. The density of cells was \sim 100,000 cm^{-2} . The chips were kept at 37°C and 10% CO_2 for 2 h. Then the medium was removed, and the cells were cultured in a serum-free medium (Brewer et al., 1993; Evans et al., 1998; Vassanelli and Fromherz, 1998) using 450 μ l neurobasal medium (Gibco, 21103049) supplemented with 2% (vol) B27-medium (17504036, Gibco) and 1% (vol) glutamax I (35050038, Gibco) for 4–7 d. The density of cells was \sim 100,000/ cm^2 . The measurements were performed with

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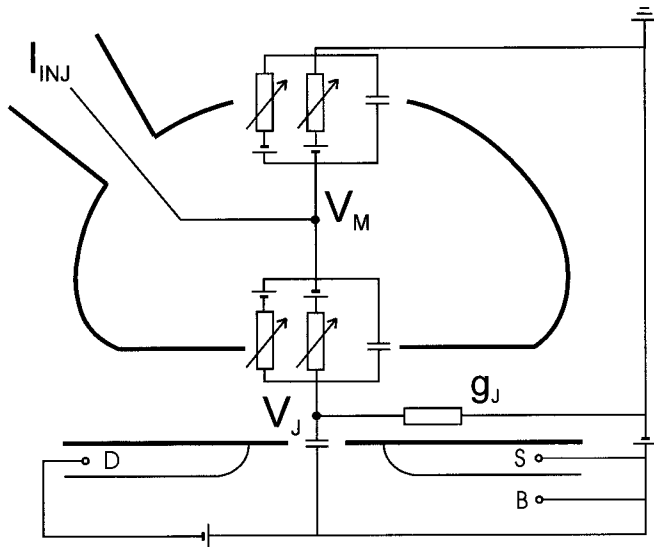


Figure 1. General scheme of transistor recording. The cell membrane with patch pipette and the silicon dioxide on the silicon chip are marked as *heavy lines*. The actual width of the cleft between oxide and membrane is ~35–70 nm. P-type source (S) and drain (D) of the transistor are in a bulk substrate (B) of n-type silicon with appropriate bias voltages. The modulation of the source drain current probes the extracellular voltage V_J in the cleft. The intracellular voltage V_M is measured and controlled through a patch pipette with an injection current I_{INJ} . g_J is the seal conductance of the junction per unit area. The current balance is described by a two-compartment circuit with capacitances and voltage-dependent conductances of the free and of the attached membrane driven by reversal voltages, and with a capacitance of the silicon dioxide.

neurons maintained for a minimum of 4 d to a maximum of 7 d in culture when the number of glia cells was still small. The electrophysiological and pharmacological characteristics of the conductances were in agreement with other preparations (Ficker and Heinemann, 1992).

Electromicroscopy. The cells cultured on the silicon chips were fixed by a slow, drop-by-drop addition of 2.5% glutaraldehyde in 150 mM sodium cacodylate buffer, pH 7.4, for 1 h (Rothman and Cowan, 1981). The fixation was performed at room temperature. After washing in 150 mM cacodylate, the specimen was refrigerated for 3 d. It was then post-fixed with 1% osmium tetroxide in 100 mM cacodylate for 1 h at 4°C, rinsed with 100 mM cacodylate and double-distilled water, and dehydrated by the gradual addition of acetone. After critical-point drying with liquid carbon dioxide, the cells were coated with gold and examined with a scanning electron microscope (SM300, Topcon, Tokyo, Japan).

Extracellular and intracellular recording. A calibrated transistor records the extracellular voltage V_J in the cleft between the silica surface and the attached cell as illustrated in Figure 1. This voltage in the junction arises from the current flowing along the cleft to the bath. The intracellular voltage V_M is controlled by the injection current I_{INJ} through a patch pipette. The current balance is described by a two-compartment circuit as shown in Figure 1 (Fromherz et al., 1993; Weis and Fromherz, 1997; Schätzthauer and Fromherz, 1998; Vassanelli and Fromherz, 1998) (point-contact model). Under voltage-clamp, the voltage in the junction V_J is determined by the current through the specific conductances g_{JM}^i of the membrane in the junction with the reversal voltages V_0^i and the specific conductance of the cell-silicon junction g_J (total conductance of the cleft divided by contact area):

$$g_J V_J = \sum_i g_{JM}^i (V_M - V_0^i). \quad (1)$$

Equation 1 is valid for weak coupling when the extracellular signal is small and when the reversal voltages V_0^i are identical in the attached and free membrane (Fromherz, 1999). The injection current I_{INJ} through the

pipette is given by the average specific conductances \bar{g}_M^i of the membrane according to Equation 2 with the area A_M of the cell membrane:

$$\frac{I_{INJ}}{A_M} = \sum_i \bar{g}_M^i (V_M - V_0^i). \quad (2)$$

A simultaneous measurement of V_J and I_{INJ} with known scaling factors g_J and A_M indicates whether the attached membrane differs from the average membrane in its specific conductances.

Electrophysiology. Patch pipettes were pulled with a three-stage puller (Zeitz-Instrumente, Augsburg, Germany) from borosilicate glass capillaries with 1.5 mm external and 1.05 mm internal diameter (GB150T-10, Science Products GMBH, Hofheim, Germany) and fire-polished. They were coated with Sylgard to reduce their capacitance and to avoid the formation of a meniscus of extracellular solution disturbing the visualization of cells under the stereomicroscope (FS-60FC, Mitutoyo, Kawasaki, Japan). The pipette filling solution was (in mM): 140 KCl, 1 CaCl₂, 2 MgCl₂, 10 EGTA, 5 HEPES, adjusted to pH 7.3 with KOH. The external solution consisted of (in mM): 135 NaCl, 5.4 KCl, 1.8 CaCl₂, 1 MgCl₂, 10 D-glucose, 5 mM HEPES, adjusted to pH 7.4 with NaOH. All measurements were performed in the presence of 1.5 μM tetrodotoxin (TTX; Sigma).

The patch-clamp recording system consisted of a single-electrode amplifier (SEC-10L, npi electronic GMBH, Tamm, Germany) and a computer running a homemade acquisition program. The current was sampled at 5 kHz and filtered at 2 kHz with a four-pole low-pass Bessel filter. Because of careful setting of the amplifier, the voltage error was below 5% as estimated with cell models. (The cell parameters were determined without filtering at a sampling frequency of 100 kHz.) Traces were corrected off-line for residual leak and capacitive currents as estimated from 20–40 mV hyperpolarizing voltage pulses from the holding potential. No inward rectifier currents were elicited during these pulses. The final current traces were obtained by averaging 20–50 sweeps. In the experiments in which TEA inhibition was investigated, the standard external solution was replaced through continuous perfusion with a solution with 10 mM TEA. The total amount of TEA solution perfused before recording was at least five times the volume of the chamber.

Recordings were undertaken at room temperature between 4 and 7 d after plating. Pyramidal-looking cells were preferred. Cell membrane parameters and access resistance were estimated by applying 20 mV hyperpolarizing voltage pulses from a holding potential of -80 mV (Lindau and Neher, 1988). Because of the modest dendritic arborizations at this stage in culture, most neurons could be well simulated with a one-compartment equivalent circuit. In a few cases a two-compartment circuit was used. Typically the cell membrane capacitance was approximately $C_M = 10$ pF. The capacitance was used to determine the effective area $A_M = C_M/c_M$ with a specific capacitance $c_M = 1$ μF/cm². Only the experiments where the access resistance was <20 MΩ were accepted. Access resistance and cell parameters were regularly monitored during the experiment and checked so that they remained constant. Voltages were not corrected for junction potentials, which were negligible for our purposes in these experimental conditions.

Transistor records. We used chips with an all-oxide surface with p-type field-effect transistors in n-type silicon (Fromherz et al., 1991). The area of a gate was 2.0×2.4 μm. The fabrication of the chips was described previously (Weis et al., 1996; V. Kiessling, B. Müller, and P. Fromherz, unpublished observations). We kept the bulk silicon and the common source at a voltage +1 V with respect to the bath. The drain-source voltage was -0.5 V. A voltage change by +1 mV on the gate induced a modulation of the source-drain current by -0.02 μA. This working point was chosen to optimize the signal-to-noise ratio. The rms-noise was ~100 μV at a bandwidth of 10 kHz. We averaged 20–50 records. There was a response only of those transistors that were precisely under the selected cell.

The specific seal conductance g_J between neuron and silicon was measured using an approach described previously (Vassanelli and Fromherz, 1997; Weis and Fromherz, 1997). Sinusoidal voltages (1000–1500 Hz, 3.5 mV rms) were applied across the cell membrane (V_M) modulating the holding potential (-80 mV). A lock-in amplifier (SR850, Stanford Research Systems, Sunnyvale, CA) was used to measure (1 Hz sampling rate) the corresponding voltages (V_J) in the neuron-silicon cleft detected by the transistor. The squared amplitude of the experimental transfer function $h = V_J/V_M$ was plotted against the squared angular frequency of the command voltage. The data were fitted by linear regression; the slope

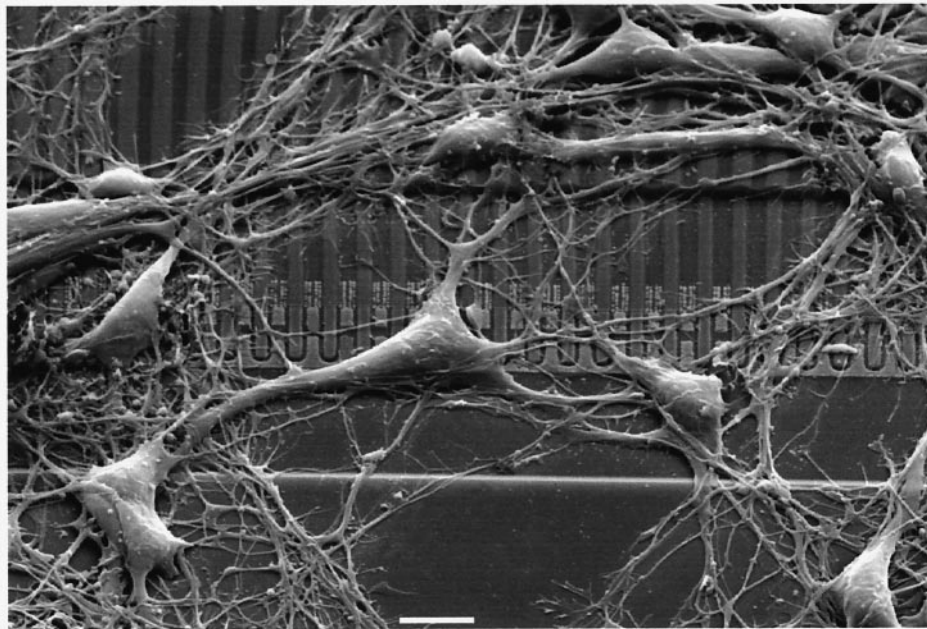


Figure 2. Scanning electron micrograph showing neurons from rat hippocampus cultured for 4 d in serum-free medium on a silicon chip with a silica surface coated with poly-L-lysine. Scale bar, 10 μm . The linear array of open transistors is seen in the center, with the drains and the lanes of field oxide directed upward and with the common source at the bottom.

of the fit defined the square of a time constant $\tau_j h_\infty$ (Vassanelli and Fromherz, 1997). The seal conductance was obtained from the relation $g_j = c_M/\tau_j/h_\infty$ with $c_M = 1 \mu\text{F}/\text{cm}^2$.

Usually the transistor signals under voltage-clamp were fading away after a few minutes of recording. For that reason we could not measure families of voltage-dependent gating curves. Concomitantly, recordings of AC voltages decreased, too. This indicates that there was not a selective rundown of ionic currents, but that the coupling of the cell was getting worse because of an enhanced seal conductance g_j , which may be caused by slight movements or by shrinking of a cell when contacted by the patch pipette.

RESULTS

Culture on chip

An electronmicrograph of a chip with neurons kept in serum-free medium for 4 d is shown in Figure 2. There were 96 transistors on the chip with a distance of 3.5 μm in a linear array. The size of the voltage-sensitive gate areas was $2.0 \times 2.4 \mu\text{m}$ (Weis et al., 1996; Kiessling, Müller, and Fromherz, unpublished observations). The diameter of a cell soma was 10–20 μm . One to three pyramidal neurons per chamber were well positioned on the array and well separated from other cells such that a defined transistor record could be expected. The distance between cell membrane and surface was in a range of 35–70 nm as determined by fluorescence interference contrast microscopy (Braun and Fromherz, 1998).

A-type and K-type current

We selected a neuron that was well placed on one of the transistors and made an electrical contact with a patch pipette in whole-cell configuration (Hamill et al., 1981; Sakmann and Neher, 1995). We applied an intracellular holding voltage of -50 mV and used a prepulse of -110 mV to remove the inactivation of the A-type and K-type potassium currents (“prepulse protocol”) (Ficker and Heinemann, 1992). We activated the potassium conductances by applying a pulse to $+20 \text{ mV}$ and recorded the current through the pipette and the extracellular voltage on the transistor. Because of the noise of the transistor we had to average 20–50 signals. An example is shown in Figure 3. We observed a transient outward current that decayed within 40 msec to an almost stationary current of 0.25 nA. Quite in contrast, the

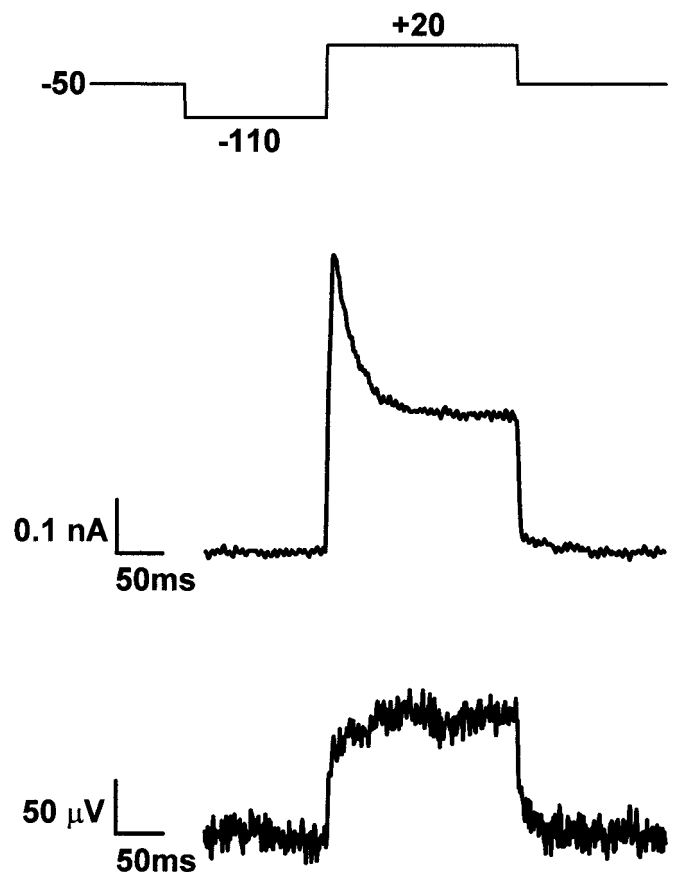


Figure 3. Voltage-clamp experiment of cultured neuron. *Top*, Protocol of intracellular voltage with a holding voltage of -50 mV , a prepulse of -110 mV , and an activation pulse of $+20 \text{ mV}$. *Center*, Whole-cell current with constant K-type signal and transient A-type component. *Bottom*, Transistor voltage with K-type signal and without A-type response. Shown is an average of 30 records. The interval between the records was 5 sec.

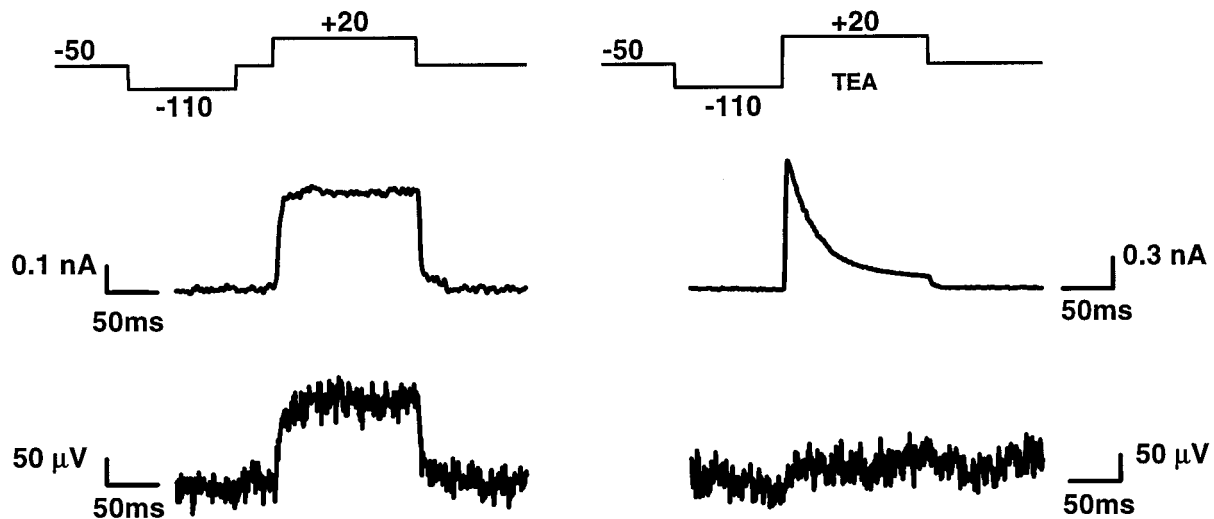


Figure 4. Voltage-clamp experiment was selective suppression of A-type current (*left*) and K-type current (*right*). *Top*, Protocol of intracellular voltage. *Center*, Whole-cell current. *Bottom*, Transistor voltage. The A-type signal is suppressed by application of a 50 msec prepulse of -50 mV before activation (*left*). Nineteen records were averaged. The K-type signal is suppressed by application of 10 mM TEA (*right*). Twenty-five records were averaged. The interval between the records was 5 sec.

voltage on the transistor approached directly a stationary value of $+120$ μ V. No signal was detectable in neighboring transistors.

The response of the pipette current corresponds to the well known superposition of A-type and K-type potassium current with fast and slow inactivation, respectively (Numann et al., 1987; Ficker and Heinemann, 1992; Klee et al., 1995). Usually in our experiments an inactivation of the K-type current was hardly visible within 200 msec. The result may indicate that only a K-type conductance with very slow inactivation was expressed (Ficker and Heinemann, 1992). This K-type signal was recorded also by the transistor. However, there was no A-type component visible in the response of the transistor.

We suppressed the A-type current selectively by holding the cell for 50 msec at -50 mV before activation of the potassium conductances ("delayed prepulse protocol") (Ficker and Heinemann, 1992). An example is shown in Figure 4. The record was from the same cell as that of Figure 3. Indeed there was no A-type transient in the pipette current, whereas the K-type current was unaffected. The record of the transistor was unchanged. The result proves that there was no A-type potassium current in the attached membrane. Of course, we cannot determine whether the channels responsible for A-type current are not present in the junction or whether their voltage sensitivity is blocked in the region of adhesion. We suppressed the K-type current selectively by extracellular application of 10 mM TEA (Ficker and Heinemann, 1992). An example is shown in Figure 4. We observed a typical A-type transient in the pipette current with inhibition of the K-type component. The transistor response was inhibited too. The result proves that the transistor record is indeed attributable to the channels that cause the usual K-type potassium current.

Conductances

We evaluated the conductances of the adhesion region and of the whole membrane from the data of Figure 3. The specific potassium conductance \bar{g}_M^K of the cell membrane on average was obtained from the pipette current by division through the membrane area A_M and the driving potential $V_M - K_0^K$ according to Equation 2 with a reversal voltage $V_0^K = -80$ mV. From a

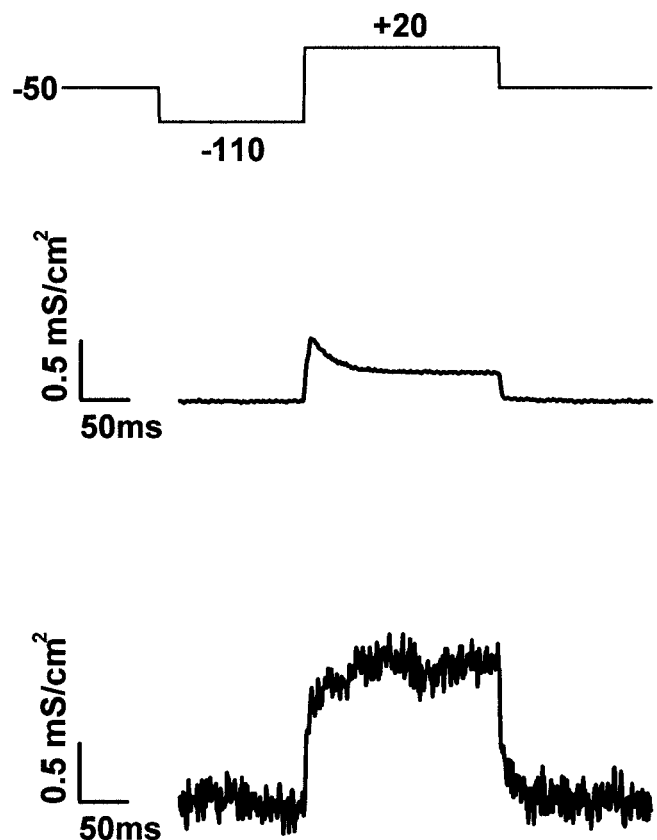


Figure 5. Specific membrane conductance. *Top*, Protocol of intracellular voltage. *Center*, Average specific potassium conductance \bar{g}_M^K of the cell membrane with K-type and A-type conductance. *Bottom*, Specific potassium conductance \bar{g}_M^K of attached membrane region with enhanced K-type and without A-type conductance. Scaled records are from Figure 3.

membrane capacitance $C_M = 11$ pF we obtained the area $A_M = 1100 \mu\text{m}^2$ using a specific capacitance $c_M = 1 \mu\text{F}/\text{cm}^2$. The result is shown in Figure 5. The amplitude of the transient A-type conductance was $\bar{g}_M^{K(A)} = 0.24$ mS/cm². The stationary K-type conductance was $\bar{g}_M^{K(K)} = 0.21$ mS/cm². These relatively low values are attributable to the short time the cells are held in culture. It should also be considered that the lack of astroglia in serum-free culture may impair the expression of channels (McFarlane and Cooper, 1993; Wu and Barish, 1994).

The specific potassium conductance $g_{JM}^{K(K)}$ in the attached membrane was obtained from the transistor voltage by multiplication with the specific conductance g_J of the cleft and by division through $V_M - V_0^K$ according to Equation 1. The result is shown in Figure 5 with $g_J = 1000$ mS/cm² as obtained from AC measurements for that particular cell. There was no significant A-type conductance in the attached membrane with $g_{JM}^{K(A)} \approx 0$. The stationary K-type conductance in the junction was $g_M^{K(K)} = 1.2$ mS/cm². The ratio of conductance in attached membrane and average membrane was $g_{JM}^{K(K)}/\bar{g}_M^{K(K)} = 5.7$.

The specific conductance of the junction depends on the geometry of adhesion by the relation $g_J = 5 d_J/\rho_J a_J^2$ with the distance d_J of membrane and substrate, the radius a_J of a circular adhesion area, and the specific resistance ρ_J of the extracellular medium in the region of adhesion (Vassanelli and Fromherz, 1997; Weis and Fromherz, 1997). The measured conductance $g_J = 1000$ mS/cm² corresponds to a circular junction with $a_J = 6 \mu\text{m}$ at a distance $d_J = 60$ nm—estimated from fluorescence interference contrast microscopy (Braun and Fromherz, 1998)—and a specific resistance $\rho_J = 80 \Omega\text{cm}$ as in the bulk electrolyte, in good agreement with the actual shape of the cells (Fig. 1). The effective area of adhesion was then $A_{JM} = 110 \mu\text{m}^2$. There were approximately 55 channels in a junction with a channel conductance of 20 pS (Storm, 1990; Bossu and Gähwiler, 1996).

The ratio $g_{JM}^{K(K)}/g_{FM}^{K(K)}$ of specific conductance in the attached membrane and free membrane may be considerably larger than the ratio $g_{JM}^{K(K)}/\bar{g}_M^{K(K)} = 5.7$. With the fraction of attached area $\alpha = A_{JM}/A_M$ and the general relation $\bar{g}_M = \alpha g_{JM} + (1 - \alpha)g_{FM}$ we obtain with $A_{JM} = 110 \mu\text{m}^2$ and $A_M = 1100 \mu\text{m}^2$ a factor of enhancement $g_{JM}^{K(K)}/g_{FM}^{K(K)} = 12$.

A successful experiment required a good whole-cell contact, a sufficient A-type and K-type current, and a tight contact between cell and transistor. In that sense we obtained successful records with 10 neurons where the specific seal conductance g_J was between 600 and 1700 mS/cm². The suppression of the A-type conductance was complete in six cells and partial in three cells. In one case we observed an enhancement of the A-type conductance. The K-type conductance was enhanced in all cases with $g_{JM}^{K(K)}/\bar{g}_M^{K(K)}$ in a range between 1.5 and 6. A correlation of the results with the age of the cells in culture was not observed.

The whole-cell records may include a contribution of proximal dendrites with an enhanced A-type current there (Hoffman et al., 1997), although the arborization was modest in our culture. We determined, however, that somatic A-type current did exist in our cells by taking nucleated patched from the upper side of cell somata (Rizzo and Nonner, 1992; Hoffman et al., 1997; Martina et al., 1998). Thus the data indeed indicate a depletion of somatic A-type conductance in the junction.

We repeated the experiments on chips coated with fibronectin to determine whether the suppression of A-type and the enhancement of K-type current was related to the chemical nature of adhesion. With respect to K-type conductance we found a similar effect as on poly-lysine in all eight neurons recorded. The A-type

conductance appeared with a delay in these cultures. It was expressed clearly only in one of the eight cells studied. In that case the A-type conductance was completely suppressed.

DISCUSSION

We used a new electrophysiological approach to characterize the adhesion region of rat hippocampal neurons in culture under voltage-clamp. The conductance of the attached membrane was probed by a field-effect transistor in the substrate. In parallel the conductance of the whole-cell membrane was observed by conventional whole-cell patch-clamp technique. We focused our attention on two well characterized potassium currents, the A-type (transient) and the K-type (sustained). By comparing the transistor records with the whole-cell records we found that the A-type conductance was highly depleted in the region of adhesion and that the K-type conductance was enhanced there. A similar distribution was observed in neurons cultured on both poly-lysine and fibronectin.

Our results are compatible with observations by Rizzo and Nonner (1992) who found that in membrane spheres (“blebs”) excised from the soma of cultured neurons from hippocampus, the A-type conductance was present in the membrane blebs whereas the K-type conductance was low. We may infer that in cultured neurons the voltage-gated channels responsible for the A-type and K-type conductances are distributed differently in the somatic membrane, the K-type channels being preferentially in the adhesion region and the A-type channels in the free membrane. Interestingly the Kv2.1 channel, identified as a major contributor to the K-type conductance in hippocampal neurons (Murakoshi and Trimmer, 1999), has been shown to be preferentially localized at cell–cell or cell–substrate adhesion zones using immunostaining (Sharma et al., 1993; Scannevin et al., 1996; Du et al., 1998). Therefore the Kv2.1 channel may be considered a possible candidate for the enhancement of the K-type conductance in the adhesion region of cultured hippocampal neurons. How the ion channels become localized in the right domain of the membrane is still an open question. Increasing evidence suggests that adhesion interactions could play a pivotal role, with a direct or indirect binding of ion channels to extracellular adhesion molecules (Isom et al., 1995; Irie et al., 1997; Sheng and Wyszyński, 1997; Thomas et al., 1997; Zito et al., 1997). The fact that switching from poly-lysine to fibronectin did not change substantially the distribution pattern of potassium conductances could suggest that highly specific adhesion interactions are required to localize and cluster ion channels.

Another possibility is that the channel molecules are distributed homogeneously all over the somatic membrane but that their activity is regulated differently in the two domains. A direct effect of poly-lysine on channel activity is unlikely because neurons cultivated on fibronectin showed a similar distribution of conductances. However, there may be a modulation from the intracellular side. One might argue that the depletion of A-type and the enhancement of K-type conductance is only apparent because the fast inactivation of A-type channels is inhibited selectively in the adhesion region such that a sustained conductance appears that mimics the K-type conductance. However, we showed that TEA, a specific blocker of the K-type conductance, is able to suppress completely the sustained conductance in the adhesion region.

The localization of ion conductances in specific domains of a neuronal membrane is essential for electrical signaling. A-type

and K-type potassium conductances represent a good example because their different distribution in somata and neuronal processes could account for a modulation of the propagation of action potential and of the integrative properties of a neuron (Storm, 1990; Debanne et al., 1997; Hoffman et al., 1997; Magee, 1998; Martina et al., 1998). On the other hand it should be considered that the major role of the attached membrane of cultured neurons could be to control cell migration rather than to contribute to an electrical integrative function. Therefore in this region, well protected from synaptic contacts, the peculiar distribution of potassium conductances found in this study could be important for cell motility. In fact, it has been proposed that potassium conductances are involved in the migration process of embryonic neurons during development (Hallows and Tempel, 1998).

In respect to the complex adhesion interactions in a tissue, neurons cultivated on adhesion molecules on inert silica represent a simple experimental system. The neuronal membrane in its adhesion region interacts with defined adhesion molecules, and their effect on the ion conductances can be investigated by a direct electrophysiological measurement. Transistor recording opens a way to study targeting and modulation of ion channels in a plasma membrane as a function of their interactions with adhesion molecules. An improvement of the signal-to-noise ratio will be important to avoid signal averaging and to detect the noise of channel dynamics in the region of adhesion.

Accumulation and depletion of ion channels in the region of an extracellular electrode determines the magnitude and shape of the extracellular record of an action potential (Schätzthauer and Fromherz, 1998; Vassanelli and Fromherz, 1998; Fromherz, 1999). Because A-type and K-type potassium channels have distinct effects on the shape of an action potential, a selective accumulation and depletion—as we detected it now—affects the shape of extracellular records in culture and in brain tissue.

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