Conditional Bistability, a Generic Cellular Mnemonic Mechanism for Robust and Flexible Working Memory Computations

Guillaume Rodriguez,¹ Matthieu Sarazin,¹ Alexandra Clemente,^{2,3} Stephanie Holden,^{2,3} Jeanne T. Paz,^{2,3,4,5} and Bruno Delord¹

¹Institut des Systèmes Intelligents et de Robotique, Sorbonne Université, Centre National de la Recherche Scientifique, UMR 7222, 75005 Paris, France,

²Gladstone Institutes, San Francisco, California 94158, ³Neurosciences Graduate Program, ⁴Department of Neurology, University of California,

San Francisco, California, 94158, ⁵Kavli Institute for Fundamental Neuroscience, University of California San Francisco

Persistent neural activity, the substrate of working memory, is thought to emerge from synaptic reverberation within recurrent networks. However, reverberation models do not robustly explain the fundamental dynamics of persistent activity, including high-spiking irregularity, large intertrial variability, and state transitions. While cellular bistability may contribute to persistent activity, its rigidity appears incompatible with persistent activity labile characteristics. Here, we unravel in a cellular model a form of spike-mediated conditional bistability that is robust and generic, and provides a rich repertoire of mnemonic computations. Under asynchronous synaptic inputs of the awakened state, conditional bistability generates spiking/bursting episodes, accounting for the irregularity, variability, and state transitions characterizing persistent activity. This mechanism has likely been overlooked because of the subthreshold input it requires, and we predict how to assess it experimentally. Our results suggest a reexamination of the role of intrinsic properties in the collective network dynamics responsible for flexible working memory.

Key words: conditional bistability; flexible; generic; memory; robust; working memory

Significance Statement

This study unravels a novel form of intrinsic neuronal property: conditional bistability. We show that, thanks to its conditional character, conditional bistability favors the emergence of flexible and robust forms of persistent activity in PFC neural networks, in opposition to previously studied classical forms of absolute bistability. Specifically, we demonstrate for the first time that conditional bistability (1) is a generic biophysical spike-dependent mechanism of layer V pyramidal neurons in the PFC and that (2) it accounts for essential neurodynamical features for the organization and flexibility of PFC persistent activity (the large irregularity and intertrial variability of the discharge and its organization under discrete stable states), which remain unexplained in a robust fashion by current models.

Introduction

Working memory (WM), the ability to maintain and manipulate information within seconds, is essential to cardinal brain func-

tions. Persistent neural activity represents a major neural correlate of WM, especially in the prefrontal cortex (PFC). The theory postulates that once triggered, persistent activity self-sustains through spiking reverberation in recurrent networks (Wang, 2001; Compte, 2006). Cortical architectures may provide sufficiently positive and nonlinear feedback for network dynamics to converge toward persistent activity (attractor dynamics; Cossart et al., 2003; MacLean et al., 2005). However, network reverberation as a unique causal origin remains controversial because it fails to robustly account for fundamental aspects of persistent activity such as the higher irregularity of spiking during the delay period of WM tasks, the large intertrial variability of

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Correspondence should be addressed to Bruno Delord, Institut des Systèmes Intelligents et de Robotique, Sorbonne Université, Centre National de la Recherche Scientifique, UMR 7222, 75005 Paris, France. E-mail: bruno.delord@upmc.fr.

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the discharge and its temporal structure under quasi-stationary states, and the ability to encode parametric information (Seidemann et al., 1996; Koulakov et al., 2002; Compte et al., 2003; Goldman et al., 2003; Shafi et al., 2007; Barbieri and Brunel, 2008).

As a non-mutually exclusive alternative, intrinsic properties of neurons may underlie persistent activity, in interaction with synaptic mechanisms, for object (Compte, 2006), spatial (Camperi and Wang, 1998), and parametric (Koulakov et al., 2002; Goldman et al., 2003) WM, and the interaction of WM with long-term memory (Egorov et al., 2002; Larimer and Strowbridge, 2010). The intrinsic bistability of neurons (i.e., the coexistence of stable states of quiescence and self-sustained spiking) is central to this proposal because it allows memorizing transient inputs in individual neurons (Booth and Rinzel, 1995; Delord et al., 1996, 1997; Marder and Calabrese, 1996; Shouval and Gavornik, 2011). Bistability is ubiquitous in peripheral (Lee and Heckman, 1998; Perrier and Tresch, 2005), subcortical (Rekling and Feldman, 1997; Kawasaki et al., 1999), and cortical (Krnjević et al., 1971; Schwindt et al., 1988; Silva et al., 1991; Tahvildari et al., 2007; Zhang and Séguéla, 2010) structures, and in the PFC (Haj-Dahmane and Andrade, 1997; Dembrow et al., 2010; Gee et al., 2012; Thuault et al., 2013).

This hypothesis has been criticized because intrinsic bistability is generally strongly stereotyped *in vitro*: it does not depend on the level of background depolarization [absolute bistability (AB)], requires long on- and off-stimuli (seconds), strong levels of pharmacological manipulations (e.g., neuromodulation), and displays extremely long (tens of seconds), high-frequency, highly regular discharges with partially inactivated spikes (Haj-Dahmane and Andrade, 1997; Egorov et al., 2002; Tahvildari et al., 2007; Zhang and Séguéla, 2010; Gee et al., 2012). These rigid features contrast with the flexibility of WM-related computational processes and persistent activity [e.g., high intertrial variability (Shafi et al., 2007) and irregular spiking (Compte et al., 2003)].

However, nonstereotyped, conditional forms of bistability, where self-sustained spiking depends on background depolarization, have been found in the cortex (Silva et al., 1991; Tahvildari et al., 2007) and other structures (Bourque, 1986; Rekling and Feldman, 1997; Lee and Heckman, 1998; Kawasaki et al., 1999; Perrier and Tresch, 2005). Conditional bistability (CB) has been observed in layer V (L5) PFC pyramidal neurons (Thuault et al., 2013), which is not surprising, since bistability is underlain in these neurons by two spike-mediated (i.e., suprathreshold) currents—the high-threshold L-type calcium (CaL) and the calcium-activated nonspecific cationic (CAN) current (Haj-Dahmane and Andrade, 1997; Gee et al., 2012; Thuault et al., 2013)—that correlate with CB in many other neuronal types (Bourque, 1986; Silva et al., 1991; Rekling and Feldman, 1997; Lee and Heckman, 1998; Kawasaki et al., 1999; Perrier and Tresch, 2005; Tahvildari et al., 2007). A spike-mediated form of AB was previously studied (Shouval and Gavornik, 2011), but spike-mediated CB remains unexplored hitherto. Yet, its mechanism may depart from more classical spiking-independent forms of bistability relying on dendritic calcium (Hounsgaard and Kiehn, 1993; Booth and Rinzel, 1995), NMDA (Milojkovic et al., 2005; Major et al., 2008; Larimer and Strowbridge, 2010), or subthreshold currents (Delord et al., 1996, 1997; Washburn et al., 2000; Genet and Delord, 2002; Loewenstein et al., 2005; Carrillo-Reid et al., 2009; Genet et al., 2010).

Here, we explore the computational and mnemonic consequences of spike-dependent CB in a model of a L5 PFC pyramidal neurons.

Materials and Methods

Design of the standard model. We consider an isopotential L5 PFC pyramidal neuron model that follows the Hodgkin–Huxley formalism. The neuron model is endowed with the leak (I_L) and action potential (AP) currents (I_{Na} , I_K) and a synaptic (I_{Syn} “*in vivo* condition”) or an injected (I_{Inj} “*in vitro* condition”) input current. Depending on the hypothesis tested, the model also comprises one or more calcium- and/or voltage-dependent suprathreshold currents, generically denoted I_{ion} . These currents can be depolarizing (I_{CaL} , I_{CAN}) or hyperpolarizing [afterhyperpolarization potential potassium current (I_{AHP})]. The standard version of the model comprises the following three currents: $I_{ion} = I_{CaL} + I_{CAN} + I_{AHP}$, with parameters described in the Parameter section (see below). The membrane potential evolves according to the following:

$$C \frac{dV}{dt} = -(I_L + I_{Na} + I_K + I_{ion} + I_{Syn}) + I_{Inj}. \quad (1)$$

Leak current I_L and action potential currents I_{Na} and I_K . The leak current is written as follows:

$$I_L = g_L(V - V_L), \quad (2)$$

and AP currents are taken from a previous model we devised to reproduce spike currents of excitatory regular-spiking neocortical neurons (Naudé et al., 2012).

High-threshold calcium current (I_{AHP}). The CaL current is derived from Delord et al. (1997) and follows as:

$$I_{CaL} = \bar{g}_{CaL} x_{CaL}^2 (V - V_{CaL}), \quad (3)$$

where the activation x_{CaL} follows first-order kinetics:

$$\frac{dx_{CaL}}{dt} = \frac{x_{CaL}^\infty(V) - x_{CaL}}{\tau_{CaL}(V)}, \quad (4)$$

with a voltage-dependent time constant:

$$\tau_{CaL}(V) = 10^{\alpha_{CaL} + \beta_{CaL}V}, \quad (5)$$

with α_{CaL} and β_{CaL} adapted to fit the time constant observed *in vitro* (Helton et al., 2005).

The activation follows:

$$x_{CaL}^\infty(V) = \left(1 + \exp \frac{-(V - V_{1/2, CaL})}{K_{CaL}}\right)^{-1}, \quad (6)$$

where $V_{1/2, CaL}$ and K_{CaL} , respectively, denote the half-activation potential and the e-fold slope of Boltzmann activation voltage dependence, and were estimated from the I – V curve obtained *in vitro* (Helton et al., 2005).

Calcium-activated nonspecific cation current (I_{CAN}). The CAN current obeys the following:

$$I_{CAN} = \bar{g}_{CAN} x_{CAN} (V - V_{CAN}), \quad (7)$$

where the activation x_{CAN} follows first-order kinetics depending on the intracellular calcium concentration, as follows:

$$\frac{dx_{CAN}}{dt} = \frac{x_{CAN}^\infty(Ca) - x_{CAN}}{\tau_{CAN}(Ca)}, \quad (8)$$

with

$$\tau_{CAN}(Ca) = \frac{1}{\alpha_{CAN}Ca + \beta_{CAN}}, \quad (9)$$

and

$$x_{CAN}^\infty(Ca) = \frac{\alpha_{CAN}Ca}{\alpha_{CAN}Ca + \beta_{CAN}}, \quad (10)$$

where α_{CAN} and β_{CAN} , respectively, denote activation and deactivation kinetic constants chosen to get significant activation in the micromolar range with time constants fitting those observed *in vitro* after large cal-

cium influx in L5 PFC pyramidal neurons (i.e., ~ 35 ms in the range 5–10 μM in the model and up to ~ 100 ms at lower $[\text{Ca}^{2+}]$ during interspike intervals (ISIs; Haj-Dahmane and Andrade, 1997)).

I_{AHP} . The AHP current modeled here corresponds to the SK potassium channel type and obeys the following:

$$I_{\text{AHP}} = \bar{g}_{\text{AHP}} x_{\text{AHP}}^2 (V - V_{\text{AHP}}), \quad (11)$$

where the activation x_{AHP} follows calcium-dependent first-order kinetics as follows:

$$\frac{dx_{\text{AHP}}}{dt} = \frac{x_{\text{AHP}}^{\infty}(\text{Ca}) - x_{\text{AHP}}}{\tau_{\text{AHP}}(\text{Ca})}, \quad (12)$$

with

$$\tau_{\text{AHP}}(\text{Ca}) = \frac{1}{\alpha_{\text{AHP}}\text{Ca} + \beta_{\text{AHP}}}, \quad (13)$$

and

$$x_{\text{AHP}}^{\infty}(\text{Ca}) = \frac{\alpha_{\text{AHP}}\text{Ca}}{\alpha_{\text{AHP}}\text{Ca} + \beta_{\text{AHP}}}, \quad (14)$$

where α_{AHP} and β_{AHP} , respectively, denote the activation and deactivation kinetic constants, fitted to account for the time constants of medium AHPs observed *in vitro* in L5 PFC pyramidal neurons (Villalobos et al., 2004; Faber and Sah, 2007).

Calcium concentration dynamics. In the model, calcium concentration dynamics results from the inward influx due to I_{CaL} and from first-order buffering/extrusion (Haj-Dahmane and Andrade, 1997) as follows:

$$\frac{d\text{Ca}}{dt} = -\frac{1}{2F} \frac{\text{Surf}}{\text{Vol}} I_{\text{CaL}} + \frac{\text{Ca}_0 - \text{Ca}}{\tau_{\text{Ca}}}, \quad (15)$$

where F is the Faraday constant, Ca_0 is the basal intracellular calcium concentration, τ_{Ca} is the buffering time constant, and the following:

$$\frac{\text{Surf}}{\text{Vol}} = r_1^{-1} \left(1 - \frac{r_1}{r_0} + \frac{r_1^2}{3r_0^2} \right)^{-1}, \quad (16)$$

is the surface area-to-volume ratio of an idealized intracellular shell compartment of thickness r_1 situated beneath the surface of a spherical neuron soma of radius r_0 . Calcium dynamics possesses an intrinsic asymmetry resulting from the inward influx due to rapid increases of I_{CaL} and the slower first-order buffering process.

Synaptic currents. In *in vivo* conditions (see Protocols), synaptic activity is simulated with fluctuating excitatory AMPA and inhibitory GABA_A conductances as studied in L5 PFC pyramidal neurons (Destexhe and Paré, 1999), and the synaptic current is modeled as follows:

$$I_{\text{syn}} = g_{\text{E}}(V - V_{\text{E}}) + g_{\text{I}}(V - V_{\text{I}}), \quad (17)$$

where V_{E} and V_{I} are the reversal potentials, and the fluctuating conductances g_{E} and g_{I} are given by two Uhlenbeck–Ornstein processes, as follows:

$$\frac{dg_{\text{E}}}{dt} = (g_{\text{E}} - g_{\text{E}_0})/\tau_{\text{E}} + \sigma_{\text{E}}x_{\text{E}}(t), \quad (18)$$

$$\frac{dg_{\text{I}}}{dt} = (g_{\text{I}} - g_{\text{I}_0})/\tau_{\text{I}} + \sigma_{\text{I}}x_{\text{I}}(t), \quad (19)$$

where τ_{E} and τ_{I} are the respective time constants of the temporal evolution of conductances, g_{E_0} and g_{I_0} are the mean conductances (that depend on the considered protocol), σ_{E} and σ_{I} are the SDs, and $x_{\text{E}}(t)$ and $x_{\text{I}}(t)$ are Gaussian stochastic processes with zero mean and unit SDs.

Determination of afterdepolarization potential amplitudes. The amplitude of afterdepolarization potentials (ADPs) is determined using a specific stimulation protocol composed of a 15 ms phasic current of fixed amplitude set to elicit a single action potential. The ADP amplitude is calculated as the maximal membrane potential difference between con-

ditions in the presence and the absence of the tested supraliminal current (I_{CaL} , I_{CAN} , or both). This difference was calculated in a window starting 10 ms after the action potential peak (to avoid the influence of different action potential lengths due to the presence/absence of suprathreshold currents) and ending 1 s later, far after complete relaxation to resting potential.

Standard model parameters. Unless indicated in figure legends, standard parameter values are as follows: for the leak current, $g_{\text{L}} = 0.05 \text{ mS} \cdot \text{cm}^{-2}$, $V_{\text{L}} = -70 \text{ mV}$; AP current parameters are as in a previous model that we developed of excitatory regular-spiking neocortical neurons (Naudé et al., 2012), with $\bar{g}_{\text{Na}} = 24 \text{ mS} \cdot \text{cm}^{-2}$, $V_{\text{Na}} = 50 \text{ mV}$, $\bar{g}_{\text{K}} = 3 \text{ mS} \cdot \text{cm}^{-2}$, and $V_{\text{K}} = -90 \text{ mV}$. For supraliminal ionic currents, parameters are $\bar{g}_{\text{CaL}} = 0.0045 \text{ mS} \cdot \text{cm}^{-2}$, $V_{\text{CaL}} = 150 \text{ mV}$, $V_{1/2, \text{CaL}} = -12 \text{ mV}$, $K_{\text{CaL}} = 7 \text{ mV}$, $\alpha_{\text{CaL}} = 0.6$, $\beta_{\text{CaL}} = -0.02 \text{ mV}^{-1}$, $\bar{g}_{\text{CAN}} = 0.025 \text{ mS} \cdot \text{cm}^{-2}$, $V_{\text{CAN}} = 30 \text{ mV}$, $\alpha_{\text{CAN}} = 0.0056 \mu\text{M}^{-1} \cdot \text{ms}^{-1}$ and $\beta_{\text{CAN}} = 0.0125 \text{ ms}^{-1}$, $\bar{g}_{\text{AHP}} = 0.2 \text{ mS} \cdot \text{cm}^{-2}$, $V_{\text{AHP}} = -90 \text{ mV}$, $\alpha_{\text{AHP}} = 0.05 \mu\text{M}^{-1} \cdot \text{ms}^{-1}$, and $\beta_{\text{AHP}} = 0.2 \text{ ms}^{-1}$. Geometrical and intracellular calcium dynamics parameters are as follows: $F = 96,500 \text{ mol} \cdot \text{s}^{-1} \cdot \text{A}^{-1}$, $r_0 = 4 \mu\text{m}$, $r_1 = 0.25 \mu\text{m}$, $\text{Ca}_0 = 0.1 \mu\text{M}$, $\tau_{\text{Ca}} = 100 \text{ ms}$. Synaptic parameters are $g_{\text{E}_0, \text{BACKGROUND}} = 0.0325 \text{ mS} \cdot \text{cm}^{-2}$, $g_{\text{E}_0, \text{EVENT}} = 0.065 \text{ mS} \cdot \text{cm}^{-2}$, $g_{\text{E}_0, \text{DELAY}} = 0.040 \text{ mS} \cdot \text{cm}^{-2}$, and independently of the period considered, $\sigma_{\text{E}} = 0.0125 \text{ mS} \cdot \text{cm}^{-2}$, $g_{\text{I}_0} = 0.1 \text{ mS} \cdot \text{cm}^{-2}$, $\sigma_{\text{I}} = 0.0075 \text{ mS} \cdot \text{cm}^{-2}$, $\tau_{\text{E}} = 2.5 \text{ ms}$, $\tau_{\text{I}} = 10 \text{ ms}$, $V_{\text{E}} = 0 \text{ mV}$, and $V_{\text{I}} = -75 \text{ mV}$.

Numerical procedures. The models were numerically integrated using the forward Euler method with a $1e^{-2}$ ms time step. Bifurcation diagrams were obtained using the XPP software for qualitative analysis of dynamical systems (<http://www.math.pitt.edu/~bard/xpp/xpp.html>). Spikes were detected as a maximum of the membrane potential above -20 mV .

In *in vitro* protocols, the behavior maps (see Figs. 2, 3) were built as follows: the discharge during a 10 s delay period was classified as (1) memoryless, when no spike occurred during the delay period or when one spike occurred at $< 25 \text{ ms}$ after the onset of the delay period; (2) transient memory, when an unstable discharge occurred during the delay period and lasted at least 25 ms after the delay period onset (to exclude cases where an ultimate spike is blown just after the phasic current pulse due to the activation of a fast sodium current in the last milliseconds of the phasic current pulse); and (3) stable memory, when the last spike of the discharge occurred after 9.5 s and the mean relative absolute difference between successive ISIs was $< 5\%$ during the last 2 s of the delay period.

In *in vivo* protocols, spikes were defined as belonging to a burst when they were part of a succession of at least three spikes with all ISIs $< 100 \text{ ms}$ (instantaneous frequencies $> 10 \text{ Hz}$). Other spikes were defined as not belonging to a burst [i.e., isolated spikes or doublet of spikes (with an intradoublet ISI inferior to 100 ms) that were separated from the rest of the spike train by ISIs $> 100 \text{ ms}$]. Bursting episodes were defined as contiguous periods of time within which all spikes belonged to a burst. Nonbursting episodes were defined as the periods outside the bursting episodes. The choice of 100 ms as a cutoff ISI value was arbitrarily set to separate periods with frequency inferior to 10 Hz, which are typical of the spontaneous state of activity in the awake cortex from periods of activity taking part in coding (Destexhe et al., 2001). This exact value is not important to the conclusions drawn in the present study.

Statistical methods. We used a two-tailed Wilcoxon rank-sum test to compare the medians of the CV distributions in the event and delay periods of the event/delay protocol, because the CV distributions were not normal, according to Kolmogorov–Smirnov goodness-of-fit hypothesis tests. A similar procedure was used to compare the medians of the CV₂ distributions in the event and delay periods of the event/delay protocol.

Results

Mimicking synaptic inputs during WM

Our main goal was to determine whether depolarizing spike-mediated currents can maintain the memory of an event at the level of the discharge of an individual neuron, while producing realistic spiking patterns, as observed during WM. To that end, we designed a realistic isopotential model of a L5 pyramidal PFC neuron endowed with high-threshold CaL (I_{CaL}), calcium-activated nonspecific cationic (I_{CAN}), afterhyperpolarization potassium (I_{AHP}),

Figure 1. Conditional bistability is a hidden property in neurons endowed with a suprathreshold conductance in response to standard protocols applied *in vitro*. **a1–a3**, The response of monostable (**a1–a3**; $g_{CAN} = 0.003 \text{ mS} \cdot \text{cm}^{-2}$), absolute bistable (**b1–b3**; $g_{CAN} = 0.03 \text{ mS} \cdot \text{cm}^{-2}$), and conditional bistable (**c1–c3**; $g_{CAN} = 0.02 \text{ mS} \cdot \text{cm}^{-2}$) neurons (standard model) to an event protocol with a 0.2 s suprathreshold current step (**a1**, **b1**, **c1**) and to the event-delay protocol, in which the event is followed by a 1 s subthreshold depolarizing current mimicking background activity in PFC networks during the delay of a working memory task (**a2**, **b2**, **c2**). Note that the discharge is continuing after the delay stimulus in the absolute bistable neuron (**b2**, star symbol). Note the ADP (**c2**, void symbol) following spiking in the conditional bistable neuron. The thresholds for initiating (θ_{ON}) and terminating (θ_{OFF}) spiking are represented as green and red dotted lines, respectively, and the bistability domains are shown in lavender. Red arrows denote the positive feedback loop among spiking, CaL activation (x_{CaL}), increased $[\text{Ca}^{2+}]$, and CAN activation (x_{CAN}). **a3**, **b3**, **c3**, Right panels, Bifurcation diagrams illustrating the stable fixed point (resting potential, green solid curve) and the minimal/maximal potentials of action potentials during the limit cycle (rhythmic spiking, red solid curves), the thresholds for initiating (θ_{ON} , green dotted lines) and terminating spiking (θ_{OFF} , red dotted lines), and the I_{inj_delay} during the delay (black arrows). Bistability domains are shown in lavender. Black dotted lines indicate unstable fixed points of the models.

action potential and leak currents, and intracellular calcium ($[\text{Ca}^{2+}]$) linear dynamics (see Materials and Methods). In the model, I_{CaL} and I_{CAN} are spike mediated because I_{CaL} activates at membrane potentials above the spike threshold and is the unique source of intracellular calcium activating I_{CAN} , as found in PFC neurons exhibiting spike-mediated bistability (Haj-Dahmane and Andrade, 1997). Parameters were set such that I_{CAN} was the sole spike-mediated charge carrier between these two currents (Haj-Dahmane and Andrade, 1997).

To test whether spike-mediated currents contribute to persistent activity in the model, we used two stimulation protocols. The event protocol, classically used to assess bistability, consisted of a single, short (0.2 s) suprathreshold current pulse mimicking the arrival of an input (e.g., perceptive or motor) event. In the event/delay protocol, the event was followed by a longer (1 s) subthreshold depolarizing current mimicking background activity from the PFC network to the neuron during the delay of a WM task. This input may correspond to persistent activity reverberating within local PFC recurrent connections to maintain information about the event or to ongoing inputs related to motivational, attentional, anticipatory, or executive aspects of WM processes.

Conditional bistability is invisible with classical protocols

At low levels of the maximal CAN conductance (g_{CAN}), the neuron discharged only during the event (Fig. 1a1, event protocol),

even when the event was followed by a background subthreshold delay current (Fig. 1a2, event/delay protocol). A bifurcation analysis as a function of the I_{inj} indicated that the neuron was monostable (M): it admitted either a stable fixed point corresponding to the resting potential (Fig. 1a3, green solid curve) or, above the spiking threshold θ_{ON} , to a stable limit cycle corresponding to rhythmic spiking (Fig. 1a3, red solid curves).

At large g_{CAN} values, the event induced a self-sustained discharge that outlasted the triggering event, providing a cellular form of memory, with both protocols (Fig. 1b1, b2). Mechanistically, self-sustained spiking arose from the positive feedback among spiking, CaL activation, increased $[\text{Ca}^{2+}]$, and CAN activation (Fig. 1b1, red arrows), which did not operate at low g_{CAN} levels (compare with Fig. 1a1). Here, the neuron was bistable: the resting potential coexisted with rhythmic spiking in a bistability domain situated between θ_{ON} , the threshold for initiating spiking, and θ_{OFF} , the threshold for terminating spiking (Fig. 1b3, lavender domain). The bistability domain included $I_{inj} = 0 \text{ } \mu\text{A} \cdot \text{cm}^{-2}$ ($\theta_{OFF} < 0 < \theta_{ON}$), so that cellular memory did not require any background subthreshold input. Hence, the spike-mediated bistability was absolute, as observed in a previous model (Shouval and Gavornik, 2011) and in PFC neurons under pharmacological manipulations (Dembrow et al., 2010; Gee et al., 2012). Therefore, persistent activity outlasted the delay period (Fig. 1b2, star;

Figure 2. Existence and expression of conditional bistability *in vitro*. **a**, Discharge behaviors of the standard neuron model in response to the event/delay protocol ($I_{\text{inj-event}} = 0.6 \mu\text{A}\cdot\text{cm}^{-2}$) as a function of the g_{CAN} and the $I_{\text{inj-delay}}$. M, CB, and AB indicate the monostability, conditional bistability, and absolute bistability domains, respectively. The memoryless and transient memory, stable conditional memory and stable absolute memory behaviors are indicated, respectively, as yellow, orange, lavender, and purple domains (bottom) and discharges (top panels). **b**, **c**, Heat maps of the duration of memoryless and transient memory behaviors (**b**) and of the mean firing frequency of stable memory behaviors (**c**) during the delay period, as a function of the g_{CAN} and the $I_{\text{inj-delay}}$. Note that above θ_{ON} , the tonic current is suprathreshold and the neuron fires even when no event precedes the delay period. Sawteeth at the border between memoryless and transient regions correspond to the discharge of one spike occurring at >25 ms after the onset of the delay period, while the main part of the transient memory region corresponds to the discharge of several spikes during the delay period (see definition of transient memory behavior in Materials and Methods).

i.e., memory was infinite), unless a specific inhibitory input terminated it.

At intermediate g_{CAN} levels, we observed that bistability was conditional: spiking during the delay depended on the level of subthreshold depolarization, as found in several neural structures and in the PFC (Bourque, 1986; Silva et al., 1991; Reklung and Feldman, 1997; Lee and Heckman, 1998; Kawasaki et al., 1999; Perrier and Tresch, 2005; Tahvildari et al., 2007; Thuault et al., 2013). After the event, spiking stopped in the event protocol (Fig. 1c1) but persisted during the entire delay in the event/delay protocol (Fig. 1c2) even though the background delay current ($I_{\text{inj-delay}}$) was subthreshold (i.e., below θ_{ON} ; Fig. 1c3, black arrow). This was possible because $I_{\text{inj-delay}}$ was above θ_{OFF} (i.e., in the bistability domain; $0 < \theta_{\text{OFF}} < \theta_{\text{ON}}$; Fig. 1c3). The background current was needed under CB, by contrast to AB, because the spike-mediated positive feedback was not sufficient to support autonomous self-sustained spiking at moderate g_{CAN} levels. This explains why persistent activity terminated at the end of the delay when I_{inj} values returned to zero, below θ_{OFF} and the bistability domain (Fig. 1c2, void symbol), being followed by an ADP (Fig. 1c2, black arrow), as found in PFC neurons expressing spike-mediated currents and/or bistability (Haj-Dahmane and Andrade, 1997; Dembrow et al., 2010; Gee et al., 2012). Thus, under CB, the duration of cellular memory adapted to the duration of network memory (i.e., reverberation), alleviating the requirement for a dedicated inhibitory stimulus to terminate persistent activity. Note also that triggering spiking-dependent bistability did not require long stimulations, because of the moderate time constant of I_{CAN} (~ 100 ms; see Materials and Methods), as found in PFC neurons (Haj-Dahmane and Andrade, 1997).

CB is robust using the event/delay protocol

To assess the robustness of CB mnemonic properties, we parametrically explored the model in response to the event/delay protocol (Fig. 2a), as a function of $I_{\text{inj-delay}}$ and g_{CAN} , which is

important because it reflects the regulation history of spike-mediated excitability and dictates the possible existence of CB (Fig. 1). We found that CB existed in a large range of g_{CAN} values (Fig. 2a, CB domain). Moreover, the ranges of CB and AB domains were much wider than M domains, indicating the prevalence of mnemonic properties with spike-mediated excitability in the model. We also found that cellular memory expressed differentially, depending on delay stimulation conditions. In the g_{CAN} range of CB, there was no firing during the delay at the lowest $I_{\text{inj-delay}}$ values (i.e., discharge was memoryless; Fig. 2a, yellow domain and trace). In contrast, delay firing was slowly decaying in a significant $I_{\text{inj-delay}}$ range below θ_{OFF} , underlying a transient memory (Fig. 2a, orange), whereas above θ_{OFF} a stable conditional memory was observed (compare Figs. 2a, lavender, 1c). In addition, we observed a stable absolute memory (i.e., sustained activity without self-termination) in the range of AB (compare Figs. 2a, purple, 1b). Under CB, memory typically lasted hundreds of milliseconds when transient (Fig. 2b) and firing frequency was generally moderate (<50 Hz), in contrast to AB (Fig. 2c). These results indicated that spike-mediated CB is robust, multiform, with long durations and low frequencies, which is consistent with persistent activity in the PFC during WM tasks (Compte, 2006). Moreover, parametrically, CB lies between M and AB, which have both largely been observed (Haj-Dahmane and Andrade, 1997; Dembrow et al., 2010; Gee et al., 2012). This suggests that CB, although rarely observed in the PFC (Thuault et al., 2013), may have been previously overlooked, because the event/delay protocol, which is mandatory to reveal it, is almost never used in intracellular recordings.

CB generically emerges from spike-mediated excitability

We wondered whether CB mnemonic properties were generic in essence, or specific to the model considered. Spike-mediated biophysical determinants—CaL and CAN current gating variables and the intracellular calcium $[\text{Ca}^{2+}]$ —share a common dynamical trait. Their spike-triggered activation operates faster, compared with

Figure 3. Conditional bistability is a generic mnemonic property of neurons endowed with depolarizing spike-mediated mechanisms. **a–e**, Thresholds for initiating (θ_{ON} , green lines) and terminating spiking (θ_{OFF} , red lines) for models with fixed (i.e., voltage- or calcium-independent) time constants suppressing the dynamic asymmetry of the CaL current (**a**), the CAN current (**b**), or both (**c**), or for models endowed with the sole CaL current with a voltage-dependent (**d**) or a fixed (**e**) time constant as a function of the suprathreshold maximal conductance and background delay current. **f**, ADP amplitudes of the five alternative models presented in **a–e**. Line colors match the respective panel titles, and the orange line applies to the standard model. Note that for ADP amplitudes (**f**) suprathreshold maximal conductances were normalized by the boundary value defining the transition between conditional and absolute bistability for each model. M, CB, and AB indicate the monostability, conditional bistability, and absolute bistability domains, respectively. Sawteeth at the border between memoryless and transient regions correspond to the discharge of one spike occurring at >25 ms after the onset of the delay period, while the main part of the transient memory region corresponds to the discharge of several spikes during the delay period (see definition of transient memory behavior in Materials and Methods).

their relaxation timescale during the ISI. This asymmetry produces interspike traces that form a memory after each spike, favoring the firing of the following spike and, in turn, self-sustained spiking. We tested whether the dynamic asymmetry of these determinants was essential to cellular memory. We found that considering fixed (i.e., voltage- or calcium-independent) time constants to suppress the dynamic asymmetry of the CaL, the CAN, or both currents had no effect on cellular memory (compare Figs. 3*a–c*, 2*a*), indicating that $[Ca^{2+}]$ dynamic asymmetry was sufficient to support cellular memory. We also found that, in the absence of both calcium dynamics and the CAN current, CaL asymmetry alone was both sufficient (Fig. 3*d*) and necessary (Fig. 3*e*). Therefore, while cellular memory required the asymmetry between activation/relaxation time constants of a least one determinant, it was independent of its exact nature. This demonstrated that dynamic asymmetry was generic in underlying the positive feedback of spike-mediated CB. Remarkably, we found that CB coexisted with marked ADP amplitudes (~ 2.5 to 15 mV) after spiking (Fig. 3*f*, above horizontal lines), contrasting with the smaller ADP of monostable neurons (<2.5 mV).

CB mnemonic properties under *in vivo* conditions

In vivo, PFC neurons continuously receive asynchronous synaptic inputs inducing strong membrane-potential fluctuations. These fluctuations may disrupt conditional memory, which relies on a minimal subthreshold depolarization. Thus, we assessed cellular memory with stochastic synaptic excitatory (AMPA) and inhibitory (GABA_A) inputs driving fluctuations as found *in vivo* in the PFC (i.e., several millivolts; Fellous et al., 2003). Here, we tested the response of the neuron to the protocols considered *in vitro* and to a delay protocol (i.e., devoid of event). The latter was

used as a control, since stochasticity may induce spiking during the subthreshold delay input. We found that at $\bar{g}_{CAN}$ levels providing CB *in vitro*, the neuron responded *in vivo* to the event/delay protocol with a persistent activity (Fig. 4*a*, right) that was absent after the event protocol (left) and initially weaker during the delay protocol (middle). As a general rule, activity included episodes during which spikes clustered in bursts and spike-mediated currents were significantly activated (Fig. 4*a*, lavender). During bursting episodes, the positive feedback characterizing CB ensured self-sustained spiking, which was irregular and terminated because of synaptic fluctuations. Bursting episodes alternated with nonbursting episodes essentially characterized by single spiking at lower frequency and smaller spike-mediated current activation (Fig. 4*a*, yellow; i.e., during which the positive feedback was disengaged). A raster plot across trials (Fig. 4*b*) illustrates stronger activity, a larger bursting propensity, and important variability in the temporal structure of the discharge during the event/delay protocol.

While firing slowly increased during the delay protocol (Fig. 4*c*, fuchsia) and rapidly decayed after the event protocol (Fig. 4*c*, light blue), it persisted longer during the delay in the event/delay protocol (Fig. 4*c*, lavender; $\tau_{memory} \sim 900$ ms), with a frequency exceeding the sum of firing frequencies triggered by event or delay inputs alone (Fig. 4*c*, salmon). Thus, persistent activity is an emergent property arising from nonlinear interactions between spike-mediated currents and the delay background input. Persistent activity with τ_{memory} in the range of hundreds of milliseconds to seconds (i.e., consistent with WM) was robustly evoked for a large domain of event input parameters (Fig. 4*d*) and a thinner domain of the delay input parameters (Fig. 4*e*). Large τ_{memory} values were observed when the event was stronger than the delay

Figure 4. Conditional bistability confers robust event memory under strongly fluctuating synaptic inputs *in vivo*. **a**, Membrane potential, CaL and CAN activation, calcium dynamics, and AHP activation traces of the standard neuron model in response to the event, delay, and event/delay protocols for a realization of the excitatory (green) and inhibitory (red) synaptic fluctuating conductances. Spikes belonging to bursting and nonbursting episodes are indicated in lavender and yellow, respectively. Small activation buildups of spike-mediated currents during nonbursting episodes and larger buildups during bursting episodes are signaled by yellow and lavender stars, respectively. See Materials and Methods for criteria that define bursting episodes. **b**, Spike raster plot for 250 trials of the protocol depicted in **a**, with different realizations of synaptic fluctuations. Color code as in **a**. **c**, Frequency poststimulus time histogram (PSTH) of the discharge (250 trials) after the onset of event (light blue), delay (fuchsia), and event/delay (lavender) protocols; difference between the PSTH during the event/delay protocol, and the sum of PSTHs during the event and delay protocols (salmon). The mean $\pm$ SEM frequency values are displayed. The memory time constant is defined as the time constant of firing frequency relaxation to its steady-state value in the event/delay protocol. **d**, Memory time constant map of persistent activity, as a function of the mean and SD of the excitatory fluctuating conductance of the event input during the event/delay protocol. The red dot indicates conductance parameters of the delay background input. When the event mean conductance is smaller than that of the delay input (left part of the map), the activity builds up to the steady state during the delay from the lower event trigger initial frequency (e.g., pink curve in **c**, for a null event mean conductance) and the time constant is smaller. **e**, Memory time constant map of persistent activity, as a function of the mean and SD of the excitatory fluctuating conductance of the delay input during the event/delay protocol. **d–e**, Means across 100 trials; other synaptic parameters as in the standard model (see Materials and Methods). **f**, Probability distribution of onset times of bursting episode as a function of their order of occurrence during the delay period (20 s) of the event/delay protocol, across 250 trials. **g–i**, CAN conductance activation (**g**), mean duration (**h**), and mean spiking frequency (**i**) during bursting (lavender) and nonbursting (yellow) episodes, as a function of their order of occurrence during a delay period (20 s) in the event/delay protocol. Mean $\pm$ SEM values across 250 trials. **j**, Probability of being in a burst episode during the delay period (2.5 s) in the event/delay protocol. **k**, Mean instantaneous spiking frequency as a function of the normalized time within bursting and nonbursting episodes (normalized time equals 0 at the beginning of episodes, 1 at their end). Mean $\pm$ SEM values across 100 trials.

(Fig. 4*d*, right part of the map), with persistent activity decaying during the delay (Fig. 4*c*, lavender).

Mechanistically, the excitation provoked by the event favored the rapid engagement of the positive feedback during the delay, as reflected by the strong synchronization of the onset of the first bursting episode across trials (Fig. 4*f*). This first episode displayed a larger recruitment of spike-mediated currents (Fig. 4*g*)

and an increased duration (Fig. 4*h*) and frequency (Fig. 4*i*), compared with the following bursting episodes. As a result, the probability of being in a bursting episode (i.e., at a higher firing frequency) remained high at the beginning of the delay and progressively decreased toward its steady state (Fig. 4*j*), accounting for the decreasing pattern of firing frequency (Fig. 4*c*, lavender). Note that the instantaneous firing frequency remained globally

Figure 5. Conditional bistability promotes irregular discharge under *in vivo* conditions. **a, b**, CV (**a**) and CV₂ (**b**) measures of the ISI distribution of the discharge in monostable (black dots; $g_{\text{CAN}} = 0 \text{ mS} \cdot \text{cm}^{-2}$) and conditionally bistable (colored dots; $g_{\text{CAN}} = 0.025 \text{ mS} \cdot \text{cm}^{-2}$) neurons, in response to the input of an event protocol (x -axis) and to the 2.5 s delay input of an event/delay protocol (y -axis). The color code for conditionally bistable neurons indicates the firing frequency during the delay. Both inputs have the same excitatory input parameter taken in the ranges 0–0.05 $\text{mS} \cdot \text{cm}^{-2}$ for the mean and 0–0.025 $\text{mS} \cdot \text{cm}^{-2}$ for the SD, to limit the effect of firing frequency, which affects CV/CV₂ measures in a nontrivial fashion (Compte et al., 2003). In both protocols, the event input lasts 0.5 s, as in the study by Compte et al. (2003). In the event/delay protocol, the event input has a 0.065 $\text{mS} \cdot \text{cm}^{-2}$ mean and a 0.0125 $\text{mS} \cdot \text{cm}^{-2}$ SD. **c, d**, In the conditionally bistable neuron, the highest discharge irregularity during the delay, measured by the CV (**c**; y -axis) and the CV₂ (**d**; y -axis) is observed at intermediate memory time constants (~ 300 –600 ms; x -axes) and frequencies of transitions between bursting and nonbursting episodes (color code). **e, f**, At moderate memory time constants (400–600 ms), the means of CV (**e**) and CV₂ (**f**) probability density functions during the delay are significantly higher in the CB neuron during the delay (thick black curve), compared with those during the event (thin black curve); $p < 10^{-9}$ (***) on two-tailed Wilcoxon rank-sum tests for both the CV and CV₂ distributions (distributions were not normal, according to Kolmogorov–Smirnov goodness-of-fit hypothesis tests; for the CV distribution: $n_{\text{event}} = 29,092$, $n_{\text{delay}} = 5448$, median (CV_{event}) = 0.5478, and median (CV_{delay}) = 1.0142; for the CV₂ distribution: $n_{\text{event}} = 26,755$, $n_{\text{delay}} = 5345$, median (CV_{2,event}) = 0.5634, and median (CV_{2,delay}) = 0.8043). **g, h**, Irregularity of the discharge plotted as a function of firing frequency for the conditionally bistable (lavender) and monostable neurons (black) in response to stationary synaptic inputs, as measured by the CV (**g**) and the CV₂ (**h**).

constant within episodes (i.e., the discharge was quasi-stationary; Fig. 4*k*).

CB promotes irregular discharge under *in vivo* conditions

In WM tasks, spiking irregularity is larger during the delay than during stimulus presentation (i.e., event; Compte et al., 2003), with a higher coefficient of variation (CV) of ISIs over 1 and a CV₂ (a version of CV based on successive ISIs) of ~ 1 , which has been difficult to reproduce robustly in theoretical models (Barbieri and Brunel, 2008). In our model, irregularity was generally higher during the delay, compared with the event (Fig. 5*a,b*, dots above first bisector), independently of whether neurons were M (Fig. 5*a,b*, no I_{CAN} , black dots) or CB (Fig. 5*a,b*, colored dots). Indeed, at a given similar firing mean frequency, the longer delay (2.5 s) allowed longer ISIs that could not occur during the shorter event (0.5 s). Thus, during the event, the sampling of the ISI distribution was truncated at low frequencies, and the apparent ISI variance was therefore decreased, compared with the delay. This effect was moderate for M neurons (Fig. 5*a,b*, black dots), but it dramatically increased for CB neurons firing at low frequency (< 15 Hz; Fig. 5*a,b*, colored dots), since, in the latter neurons, alternations of bursting episodes (with smaller ISIs) and nonbursting episodes (with larger ISIs) strongly increased the variance of the ISI distribution during the delay. At such low-frequency firing, the CV was largely > 1 and the CV₂ was ~ 1 , as found during WM delays (Compte et al., 2003). Moreover, CV/CV₂ culminated for inputs leading to intermediate memory time constants in the range of ~ 400 –600 ms (Fig. 5*c,d*) and transition frequencies between episodes at ~ 1 Hz (color code). In these

conditions, both the CV and CV₂ were significantly larger during the delay (Fig. 5*e,f*, thick black trace), compared with the event (Fig. 5*e,f*, thin black trace). Remarkably, consistent with data (Compte et al., 2003), the CV distribution during the delay was broadened, compared with that during the event, which did not occur for the CV₂.

To fully confirm the genuine effect of depolarizing spike-mediated currents on spiking irregularity, we compared CV/CV₂ with and without CB (1) upon stationary stimuli to avoid the interference of frequency time variations due to the protocol and (2) at identical mean firing frequencies to avoid the nontrivial effects of frequency on these measures (Compte et al., 2003). In these conditions, where computing these observables admits its plain significance, we found that, compared with M neurons (Fig. 5*g*, black), the CV was systematically superior in CB neurons (Fig. 5*g*, lavender) < 20 Hz and was > 1 below 10 Hz. In CB neurons, the CV₂ was also superior below 2 Hz, situated at ~ 1 , whereas it was essentially similar to M neurons > 2 Hz (Fig. 5*h*). Thus, although the mean local irregularity measured by the CV₂ was the same on average (because local increases of frequency regularity within bursting episodes compensated for the local frequency irregularities at transitions between bursting and nonbursting episodes), we found that the global irregularity of the discharge (measured by the CV; i.e., the normalized ISI SD) was increased in CB neurons due to the presence of spike-mediated currents.

Discussion

Here, we show that spike-mediated CaL and CAN currents of L5 pyramidal PFC neurons (Haj-Dahmane and Andrade, 1997; Gee

et al., 2012; Thuaud et al., 2013) support CB. Moreover, our study suggests that CB is prevalent for several reasons. First, CB relies on suprathreshold mechanisms that are ubiquitous in pyramidal PFC neurons and operate robustly, independent of biophysical details, which are generic. Second, CB parametrically situates between M and AB regimes, both extensively observed in the PFC and other areas (Krnjević et al., 1971; Schwindt et al., 1988; Yang et al., 1996; Haj-Dahmane and Andrade, 1997; Dembrow et al., 2010; Zhang and Séguéla, 2010; Gee et al., 2012). AB is often observed under strong neuromodulatory manipulation that upregulates depolarizing spike-triggered conductances, yielding unrealistic stereotyped discharges inconsistent with WM firing patterns (Compte et al., 2003; Shafi et al., 2007). This suggests that neuromodulation regulates conductances below the range for AB in behaving animals. Below AB, the probability of being in CB is largely predominant (a much wider range than M; Fig. 2a). Moreover, minimal neuromodulation is crucial for optimal PFC computations (Wang et al., 2007), whereas M lies at the lowest neuromodulation (conductance) levels. Thus, CB is likely encountered in PFC pyramidal neurons under physiological neuromodulatory levels. Third, we show that ADP represents a generic marker distinguishing CB from M neurons. ADPs are ubiquitous across L5 PFC pyramidal types (Yang et al., 1996; Haj-Dahmane and Andrade, 1997) and share specific common features with CB neurons (>5 mV; durations up to ~100 ms, occurrence even at low frequencies, CAN/calcium dependence; Yang et al., 1996; Haj-Dahmane and Andrade, 1997; Boudewijns et al., 2013), suggesting that PFC neurons displaying ADP are conditionally bistable. Hence, CB was observed without artificial pharmacological activation in L5 PFC pyramidal neurons with prominent ADPs (Thuaud et al., 2013). Altogether, these lines of evidence indicate that CB likely constitutes a prevalent property in PFC L5 pyramidal neurons in physiological conditions during WM tasks.

So, why has CB remained scarce in the PFC? CB requires a triggering suprathreshold input followed by a subthreshold input (or applied upon a depolarized subthreshold holding potential). Therefore, CB neurons are undetectable using the classic protocol ubiquitously used, which consists of a single suprathreshold input applied from the resting potential. Consequently, neurons can be categorized as M (Fig. 1c1), while actually displaying genuine CB (Fig. 1c2). Such misclassification should be frequent given the much larger CB domain (compared with M), and systematically applying event/delay protocols should unravel CB in a significant fraction of neurons. Remarkably, event/delay protocols are meaningful physiologically, mimicking the temporal profile of inputs during WM: a strong behaviorally relevant (e.g., perceptive) signal followed by a lower background input during the delay (e.g., reverberating persistent activity or WM-related feedforward inputs).

Information maintenance in CB neurons relies on the asymmetry between fast buildup/activation and slower relaxation/deactivation dynamics of spike-activated mechanisms. This asymmetry maintains spike-to-spike excitability through the positive feedback between depolarization and suprathreshold activation. Noticeably, the slow CAN deactivation time constant of ~100 ms (Haj-Dahmane and Andrade, 1997) allows the maintenance of self-sustained activity down to ~10 Hz. Slower CAN in the PFC (Sidiropoulou et al., 2009) may support lower frequencies, at some expense (see below). Under asynchronous inputs, CB generates bursting/nonbursting episodes. Bursting episodes can be triggered by—and form a memory of—incoming events, when a background input follows the event. Statistically, this per-

sistent activity fades at the second timescale across trials, consistent with WM, reflecting the stochastic disruption of bursting episodes due to synaptic fluctuations. By contrast, firing frequency is steady within bursting episodes, so that information maintenance is constant within individual trials for the duration of the first bursting episode.

Overall, the spike-mediated mechanism we unravel is robust to the exact nature and parameter values of the model and displays a much higher resistance to transient episodes of inhibition, compared with subthreshold-based bistabilities (Washburn et al., 2000; Loewenstein et al., 2005; Carrillo-Reid et al., 2009). Sensitivity to inhibitory interference was used to discard the possible role of intrinsic bistability in maintaining persistent activity (Sanchez-Vives and McCormick, 2000; McCormick et al., 2003). Our results indicate that this reasoning does not apply to spike-mediated mechanisms, because they preserve resistance to inhibition, as does synaptic reverberation.

Previously described bistabilities are rigid, requiring strong/long stimuli to be turned on/off and producing long, high-frequency discharges primarily independent of the background input (Haj-Dahmane and Andrade, 1997; Egorov et al., 2002; Tahvildari et al., 2007; Zhang and Séguéla, 2010; Gee et al., 2012). By contrast, CB exhibits a rich repertoire of computational operations. It expresses as a memoryless discharge or subserve transient or stable conditional memory, depending on input parameters. Moreover, mnemonic activities can be initiated by short events because of the moderate CAN activation time constant (Haj-Dahmane and Andrade, 1997). Furthermore, the duration and frequency of mnemonic discharges are controlled by the delay input at low frequencies. Finally, under *in vivo*-like inputs, this diversity expresses as bursting/nonbursting episodes with variable frequencies and durations, resulting in a large variability of the discharge structure across trials, as found during WM (Shafi et al., 2007).

In response to asynchronous inputs, CB increases discharge irregularity, because smaller ISIs during bursting episodes and larger ISIs during nonbursting episodes increase the ISI distribution variance. The CV/CV₂ are highest at low firing frequencies i.e., under excitation/inhibition balance, two factors increasing irregularity; Compte et al., 2003. In such conditions, the CV is >1 and CV₂ ~1 in CB neurons during the delay, being higher than during the event, as in WM (Compte et al., 2003), properties previous models are unable to account for robustly (Barbieri and Brunel, 2008). This effect happens in CB neurons, because bursting/nonbursting episodes can alternate during delays of several seconds, but not during shorter events (0.2 s).

Besides, while CB clearly increases the CV, its effect on the CV₂ is mild. This results because whereas frequency changes at the transitions of episodes increase CV₂, the more regular discharge within bursting episodes decreases it. Synaptic inputs are not stationary *in vivo* (Shafi et al., 2007; Ostojic, 2014), which could explain the slightly higher CV/CV₂ observed experimentally (Compte et al., 2003), compared with the situation reported here. This could also explain the larger difference in CV₂ values between the delay and the event (Compte et al., 2003), as changes in the synaptic input rates have more time during the delay to exert their effect on successive ISIs and thus on the CV₂.

Interestingly, the overall increase in irregularity in CB neurons required an AHP current, which balanced the CAN current in the model (CAN alone decreased irregularity; data not shown). Finally, our conclusion that bursting/nonbursting alternations underlie irregularity is additionally supported by the finding that very slow CAN currents—driving very long

bursts without alternations—decrease the CV (Sidiropoulou et al., 2009).

What roles may CB play at the network scale during maintenance? Here, CB requires a subthreshold constant background input from the network to memorize a transient event. However, inputs are not stationary in PFC networks and cellular CB should affect, in turn, network dynamics. Therefore, interactions between local cellular CB and global network recurrence may provide a rich repertoire of dynamics.

Hence, following an event, bursting in CB neurons may be sustained by the prolonged synaptic feedback due to bursting in other CB neurons. Such synergistic CB bursting recruitment may determine the extent to which activity is amplified and prolonged, possibly resulting in decaying, stable, or ramping temporal firing patterns of WM (Shafi et al., 2007). Synergy between CB neurons may also provide a realistic biophysical basis for WM of parametric information, which requires bistable elements to emerge robustly (Koulakov et al., 2002; Goldman et al., 2003). Such collective dynamics are plausible because CB is gradual in essence, by contrast to AB. WM-related drives during the delay and the regulation state of synaptic strengths and spike-mediated excitability should be fundamental in setting the gradual synergetic recruitment of CB neurons.

Within a recurrent network, CB neurons can discharge during the delay even when they have not received the event input, because of the subthreshold recurrent input provided by other neurons of the network actively maintaining the memory of that event (Fig. 4c, fuschia curve). This could be problematic if presynaptic and postsynaptic neurons belong to different populations encoding distinct memories (i.e., Hebbian assemblies), as memory would “bleed over” across populations (i.e., memory interference). This problem may arise even with monostable postsynaptic neurons, although CB neurons would discharge at higher rates for a similar recurrent delay input, enhancing interference. However, different mechanisms have been imagined that may circumscribe interference between memory representations [e.g., mutual (Miller and Wang, 2006) or global (Brunel and Wang, 2001) inhibition between assemblies]. Besides, enhanced “bleeding” due to CB could also improve pattern completion within Hebbian assemblies, because the easier recruitment of CB neurons not activated by the event (because of incomplete input pattern presentation) would facilitate complete memory retrieval through associative synaptic reverberation.

Besides, during WM delays, PFC networks encounter transitions between stable collective states of quasi-stationary firing at the second timescale, reflecting mental states during the exploration of computational solutions, as cognitive processes wander from stimulus encoding to decision-making and action (Seidemann et al., 1996; Cossart et al., 2003). Bursting/nonbursting episodes in CB neurons share similar quasi-stationary firing and generate maximal irregularity at this timescale. We suggest that CB may promote the emergence of stable collective states and the complexity of PFC neuronal operations, providing a basis for exploring computational solutions during WM. Intrinsic plasticity and neuromodulation would represent strategic processes to regulate spike-mediated mechanisms for the emergence of adapted WM-related cognitive processes.

While CB relies on a weak spike-mediated positive feedback, it is precisely this “weakness” that underpins the computational richness and flexibility it brings, compared with what was previously thought. We suggest that the traditional view should be overcome in favor of a reconciling perspective whereby synaptic reverberation and conditional bistability concur with the emer-

gence of the highly flexible persistent activity required for elaborating adaptive WM-related cognitive processes and intelligent behavior.

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