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The representation of semantic information across human cerebral cortex during listening versus reading is invariant to stimulus modality

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1 **The representation of semantic information across human cerebral cortex**
2 **during listening versus reading is invariant to stimulus modality**
3

4 Fatma Deniz^{a,b,c}, Anwar O. Nunez-Elizalde^a, Alexander G. Huth^{a,1}, Jack L. Gallant^{a,d}

5
6 ^aHelen Wills Neuroscience Institute, University of California, Berkeley, CA 94720, USA

7 ^bBerkeley Institute for Data Science, University of California, Berkeley, CA 94720, USA

8 ^cInternational Computer Science Institute, Berkeley, CA 94704, USA

9 ^dDepartment of Psychology, University of California, Berkeley, CA 94720, USA

10
11 ¹ Present address: Departments of Computer Science and Neuroscience, University of Texas, Austin, TX 78712,
12 USA

13
14 Correspondence should be addressed to:

15 Jack L. Gallant

16 **2121 Berkeley Way**

17 **University of California, Berkeley**

18 **Berkeley, CA 94720-1650**

19
20 E-mail: <gallant@berkeley.edu>.

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42 **ABSTRACT**

43 An integral part of human language is the capacity to extract meaning from spoken and written words, but the
44 precise relationship between brain representations of information perceived by listening versus reading is
45 unclear. Prior neuroimaging studies have shown that semantic information in spoken language is represented
46 in multiple regions in the human cerebral cortex, while amodal semantic information appears to be
47 represented in a few broad brain regions. However, previous studies were too insensitive to determine whether
48 semantic representations were shared at a fine level of detail rather than merely at a coarse scale. We used
49 fMRI to record brain activity in two separate experiments while participants listened to or read several hours of
50 the same narrative stories, and then created voxelwise encoding models to characterize semantic selectivity in
51 each voxel and in each individual participant. We find that semantic tuning during listening and reading are
52 highly correlated in most semantically-selective regions of cortex, and models estimated using one modality
53 accurately predict voxel responses in the other modality. These results suggest that the representation of
54 language semantics is independent of the sensory modality through which the semantic information is
55 received.

56
57 **Keywords**

58
59 fMRI; BOLD; listening; reading; semantics; regression; representation; cross-modal representation
60

61 **SIGNIFICANCE STATEMENT**

62
63 Humans can comprehend the meaning of words from both spoken and written language. It is therefore
64 important to understand the relationship between the brain representations of spoken or written text. Here we
65 show that although the representation of semantic information in the human brain is quite complex, the
66 semantic representations evoked by listening versus reading are almost identical. These results suggest that the
67 representation of language semantics is independent of the sensory modality through which the semantic
68 information is received.

69 INTRODUCTION

70
71 Humans have the unique capacity to communicate and extract meaning through both spoken and written
72 language. Although the early sensory processing pathways for listening and reading are distinct, listeners and
73 readers appear to extract very similar information about the meaning of a narrative story (Diakidoy et al.,
74 2005; Rubin et al., 2000). This suggests that the human brain represents semantic information in an amodal
75 form that is independent of input modality (for reviews see (Binder et al., 2009; Price, 2010, 2012; Vigneau et
76 al., 2006)). There is evidence that several cortical regions are activated during both listening and reading (for
77 reviews see (Price, 2010, 2012)). However, the demonstration of some common activation during listening and
78 reading is necessary but not sufficient evidence of a common amodal semantic representation.

79
80 A direct and convincing way to determine if listening and reading involve a common underlying semantic
81 representation would be to compare directly the semantic selectivity maps obtained during listening and
82 reading of natural text, in single participants. However, to date no study has performed this crucial
83 comparison. Most imaging studies of the semantic system have examined only one input modality, either
84 spoken or written words (Booth et al., 2002; Démonet et al., 1994, 1992; Devlin et al., 2004; Nakamura et al.,
85 2005; Rissman et al., 2003; Scott et al., 2000; Vandenberghe et al., 1996). Relatively few have studied cross-
86 modal representations by presenting the same stimuli in both modalities (Buchweitz et al., 2009; Chee et al.,
87 1999; Jobard et al., 2007; Liuzzi et al., 2017; Michael et al., 2001; Petersen et al., 1989; Spitsyna et al., 2006).
88 Most of these cross-modality studies observed activity in left lateralized regions such as the left anterior
89 temporal lobe, left superior temporal sulcus (STS), left middle temporal gyrus (MTG) and left inferior frontal
90 gyrus (IFG). Most of these studies used tightly controlled stimuli, such as a set of single isolated words,
91 sentences or curated passages, and an explicit lexical semantic task (Buchweitz et al., 2009; Chee et al., 1999;
92 Liuzzi et al., 2017; Michael et al., 2001). A study that used narrative speech in a listening and reading task
93 demonstrated amodal brain activity in left pSTG, left IFG, bilateral Precuneus, medial prefrontal cortex, and
94 angular gyrus (Regev et al., 2013). However that study did not model semantic information, but only showed
95 that voxel activations in these regions tend to be correlated across these two modalities. Furthermore, previous
96 studies were too coarse grained to determine whether listening and reading shared semantic representations at
97 the level of a single voxel. For example, the semantic representation of listening and reading might have been
98 modal at a fine scale (i.e. single voxel), although amodal at a coarse scale. In sum, the evidence available
99 currently is insufficient to determine whether semantic information obtained during listening and reading are
100 represented in the same way.

101
102 To address this issue we used functional magnetic resonance imaging (fMRI) to record blood-oxygen-level
103 dependent (BOLD) activity in human participants while they listened to and read the same narrative stories.
104 We then used voxelwise modeling (VM) combined with banded ridge regression (Nunez-Elizalde et al., 2019) to
105 characterize the semantic selectivity of each voxel in each presentation modality and for each individual
106 participant (see **Materials and Methods** and (Çukur et al., 2013; Huth et al., 2012, 2016; Lescroart et al.,
107 2015; Nishimoto et al., 2011; Stansbury et al., 2013)). Finally, we compared the semantic tuning of each voxel
108 in the two modalities by creating semantic maps (Huth et al., 2016) for both modalities and each individual
109 participant. In addition, we identified modality independent cortical representation of semantic information by
110 predicting voxel responses cross-modally. Comparison of the fit semantic models and semantic maps obtained
111 by listening versus reading provides a sensitive and objective means to determine whether and how semantic
112 selectivity changes depending on the modality with which semantic information is perceived.

114 MATERIALS and METHODS

116 **Participants**

117
118 Functional data were collected from six male participants and three female participants: S1 (male, age 31), S2
119 (male, age 31), S3 (female, age 28), S4 (female, age 25), S5 (male, age 30), S6 (male, age 25), and S7 (male, age
120 36), S8 (female, age 24), S9 (male, age 24). Two of the participants were authors on the paper (AGH and
121 AONE). All participants listened to and read all the stories. Listening and reading presentations were

122 counterbalanced across participants. All participants were healthy and had normal hearing, and normal or
123 corrected-to-normal vision. One participant was left handed, all other participants were right handed or
124 ambidextrous according to the Edinburgh handedness inventory (Oldfield, 1971) (laterality quotient of -100:
125 entirely left-handed, +100: entirely right-handed). Laterality scores were +90 (decile R.7), +70 (decile R.3),
126 +10 (ambidextrous), +80 (decile R.5), +80 (decile R.5), +80 (decile R.5), -60 (decile L.3), +90 (decile R.7) and
127 +95 (decile R.9) for S1-9, respectively. To stabilize head motion during scanning sessions participants wore a
128 personalized headcase that precisely fit the shape of each participant's head (<https://caseforge.co/>).
129

130 **Natural Speech Stimuli**

131
132 The speech stimuli consisted of ten 10- to 15-minute stories taken from *The Moth Radio Hour* and used
133 previously (Huth et al., 2016). In each story, a speaker tells an autobiographical story in front of a live
134 audience. The ten selected stories cover a wide range of topics and are highly engaging. The model validation
135 dataset consisted of one 10-minute story. This story was played twice for each participant (once during each
136 scanning session), and then the two responses were averaged (see Huth et al. (2016) for more details).
137

138 Speech stimuli were played over Sensimetrics S14 in-ear piezoelectric headphones (Sensimetrics, Malden, MA,
139 USA). A Behringer Ultra-Curve Pro hardware parametric equalizer was used to flatten the frequency response
140 of the headphones based on calibration data provided by Sensimetrics. All stimuli were played at 44.1 kHz
141 using the pygame library in Python. All stimuli were normalized to have peak loudness of -1 dB relative to max.
142 However, the stories were performed by different speakers and were not uniformly mastered, so some
143 differences in total loudness remain.
144

145 **Story transcription and preprocessing**

146
147 Each story was manually transcribed by one listener, and this transcription was checked by a second listener.
148 Certain sounds (e.g. laughter, lip-smacking and breathing) were also marked in order to improve the accuracy
149 of the automated alignment. The audio of each story was downsampled to 11.5 kHz and the Penn Phonetics Lab
150 Forced Aligner (P2FA; Yuan & Liberman, 2008) was used to automatically align the audio to the transcript.
151 The forced aligner uses a phonetic hidden Markov model to find the temporal onset and offset of each word
152 and phoneme. The Carnegie Mellon University (CMU) pronouncing dictionary was used to guess the
153 pronunciation of each word. The Arpabet phonetic notation was used when necessary to manually add words
154 and word fragments that appeared in the transcript but not in the dictionary.
155

156 After automatic alignment was complete, Praat (Boersma and Weenink, 2014) was used to check and correct
157 each aligned transcript manually. The corrected aligned transcript was then spot-checked for accuracy by a
158 different listener.
159

160 Finally the aligned transcripts were converted into separate word and phoneme representations using Praat's
161 TextGrid object. The phoneme representation of each story is a list of pairs (P, t) , where P is a phoneme and t is
162 the onset time in seconds. Similarly the word representation of each story is a list of pairs (W, t) , where W is a
163 word and t is the onset time in seconds.
164

165 **Natural Reading Stimuli**

166 The same stories from listening sessions were used for reading sessions. Praat's word representation for each
167 story (W, t) was used for generating the reading stimuli. The words of each story were presented one-by-one at
168 the center of the screen using a rapid serial visual presentation (RSVP) procedure (Buchweitz et al., 2009;
169 Forster, 1970). During reading, each word was presented for a duration precisely equal to the duration of that
170 word in the spoken story. RSVP reading is different than natural reading because during RSVP the reader has
171 no control over which word to read at each point in time. Therefore, in order to make listening and reading
172 more comparable we matched the timing of the words presented during RSVP to the rate at which the words
173 occurred during listening.

174
175 The pygame library in Python was used to display text on a gray background at 34 horizontal, and 27 vertical
176 degrees of visual angle. Black letters were presented at average 6 (min=1, max=16) horizontal and 3 vertical
177 degrees of visual angle. A white fixation cross was present at the center of the display. Participants were asked
178 to fixate while reading the text. These data were collected during two 3-hour scanning sessions that were
179 performed on different days. Participants' eye movement were monitored at 60 Hz throughout the scanning
180 sessions using a custom-built camera system equipped with an infrared source (Avotec) and the ViewPoint
181 EyeTracker software suite (Arrington Research). The eye tracker was calibrated before the first run of data
182 acquisition. Certain auditory sounds (laughter and applause) were presented as text to provide cues about the
183 ambiance of each story.

184 185 **Semantic model construction**

186
187 To account for response variance caused by the semantic content of the story stimuli a 985-parameter semantic
188 feature space based on word co-occurrence statistics in a large corpus of text (Deerwester et al., 1990; Huth et
189 al., 2016; Lund and Burgess, 1996; Mitchell et al., 2008) was used. In short, a word co-occurrence matrix, M ,
190 with 985 rows and 10,470 columns was created. The 985 rows describe 985 basic words from Wikipedia's *List*
191 *of 1000 basic words*, the 10,470 columns are words selected from a very large corpora of 13 transcripts of Moth
192 stories (including the 10 used as stimuli in the experiments described in this paper), 604 popular books
193 available through Project Gutenberg, 2,405,569 Wikipedia pages, 36,333,459 reddit.com user comments (see
194 Huth et al., 2016 for a detailed description).

195
196 Iterating through the text corpus, we added 1 to $M_{i,j}$ each time word j appeared within 15 words of basis word i .
197 Once the word co-occurrence matrix was complete, we log-transformed the counts, replacing $M_{i,j}$ with
198 $\log(1 + M_{i,j})$. Next, each row of M was z-scored to correct for differences in basis word frequency, and then
199 each column of M was z-scored to correct for word frequency. Each column of M is now a 985-dimensional
200 semantic vector representing one word in the lexicon.

201
202 The semantic model stimulus matrix was then constructed from the stories: for each word-time pair (w, t) ,
203 within each story the corresponding column of M was selected, creating a new list of semantic vector-time
204 pairs, (M_w, t) . These unevenly-sampled lists of vectors were resampled at times corresponding to the fMRI
205 acquisitions using a 3-lobe Lanczos filter with the cutoff frequency set to the Nyquist frequency of the fMRI
206 acquisition (0.249 Hz).

207 208 **Motion-energy model construction**

209
210 A spatiotemporal Gabor pyramid was used to extract low-level visual features from the sequence of word
211 frames used in the reading experiment (Adelson and Bergen, 1985; Watson and Ahumada, 1985). The word
212 frames were first cropped to 400x400 pixels (14 horizontal, and 14 vertical degrees of visual angle) to include
213 mainly the words and then downsampled to 96x96 pixels to minimize computational cost. The word frames
214 were then converted to the CIE L*A*B* color space (McLaren, 1976) and the color information was discarded.
215 The spatiotemporal Gabor pyramid consisted of a total of 39 three-dimensional Gabor filter pairs of orthogonal
216 quadrature spanning a square grid that covered the screen. The filters consisted of two spatial and one
217 temporal dimension and were created using five spatial frequencies (0, 2, 4, 6, and 8 cycles/image), three
218 temporal frequencies (0, 2 and 4 Hz), and four directions of motion (0, 90, 180, and 270 degrees). Each of the
219 filters was convolved with the sequence of word frames. The resulting filter activations were squared and
220 summed for each quadrature pair, resulting in a 39-dimensional feature vector for each word frame. The
221 output was downsampled to the functional image acquisition rate (2.0045 s) using sinc interpolation
222 (Oliphant, 2007). See (Nishimoto et al., 2011) for more details. However, note that only five spatial frequencies
223 and four directions of motion were used here.

224 225 **Spectral model construction**

227 A cochleogram model that accounts for the logarithmic filtering of the mammalian coclea described in (de Heer
228 et al., 2017) was used to create the low level auditory features (80 parameters). This model was selected based
229 on an earlier study showing that it outperforms other low level acoustical models (de Heer et al., 2017). The 80
230 waveforms of the coclear filter bank were between 264 and 7360 Hz, spaced at 25% of the bandwidth. The
231 spectral features were downsampled to the rate of acquisition of the functional images (2.0045 s) using a
232 Lanczos filter.

233 **Syntax model construction**

234
235 The syntactic properties of each spoken word were labeled. A pre-trained neural network was used to create a
236 parse tree for each sentence of the stories (Andor et al., 2016). Two feature spaces were extracted from the
237 parse trees. The first was constructed from the part-of-speech tags (e.g. noun, verb) by assigning a value of one
238 to each entry in which the part-of-speech tag appeared and all other entries were set to zero (12 parameters).
239 The second feature space captured the word dependencies in the sentence (i.e. direct object, indirect object,
240 etc.) and was constructed by assigning a value of one to each entry in which the word dependency appeared and
241 all other entries were set to zero (44 parameters). For each syntactic feature (e.g. noun), a time course was
242 created with a value of 1 whenever a word was labeled with that feature and 0 otherwise. The syntactic features
243 were then downsampled to the rate of acquisition of the functional images (2.0045 s) using a Lanczos filter.

245 **Phoneme model construction**

246
247 To account for response variance caused by the low-level phonemic content of the stories, a 39-parameter
248 model that captures how often each of the 39 phonemes in English was spoken over time was constructed. The
249 phoneme representation of the stories were used to construct this model: the lists of phoneme-time pairs (P, t)
250 were re-arranged into 39 lists, each of which contains only the times of a single phoneme. These lists of times
251 were then downsampled to the fMRI acquisition rate (2.0045 s).

253 **Letter model construction**

254
255 To account for response variance caused by the letters during reading a 26-parameter model that captures how
256 often each of the 26 letters in English was present on screen over time was constructed. This was constructed
257 by counting the number of times a letter was present within a word and then downsampled to the fMRI
258 acquisition rate (2.0045 s).

260 **Word rate, word length variation, phoneme rate, letter rate, and pauses model construction**

261
262 To account for the highly variable speech rate both within and across stories, single-feature models that simply
263 count the number of words, number of phonemes, number of letters, and number of story speaker's pauses that
264 occurred during the acquisition of each fMRI volume (2.0045 s) were constructed. To account for the variable
265 word lengths during the visual presentation a single-feature word length variation model was constructed by
266 taking the variance of word lengths that occurred during the acquisition of each fMRI volume.

268 **Stimulus downsampling**

269
270 Before downsampling to the fMRI acquisition rate, the phoneme and semantic models were represented as
271 unevenly-sampled impulse trains. A 3-lobe Lanczos filter with cutoff frequency set to the fMRI Nyquist rate
272 (0.249 Hz) was used to resample these impulse trains at evenly spaced time points corresponding to the middle
273 of each fMRI volume.

275 **Experimental Design and Statistical Analysis**

277 **fMRI data acquisition**

278 Each spoken and written story was presented during a separate fMRI scan. The length of each scan was the
279 same as the story. Each scan included 10 seconds (5 TR) of silence both before and after the story. These data

280 were collected during two 3-hour scanning sessions that were performed on different days.

281
282 MRI data were collected on a 3T Siemens TIM Trio scanner at the UC Berkeley Brain Imaging Center using a
283 32-channel Siemens volume coil. Functional scans were collected using gradient echo EPI water excitation
284 pulse sequence with repetition time (TR) = 2.0045s, echo time (TE) = 31ms, flip angle = 70 degrees, voxel size
285 = 2.24 x 2.24 x 4.1 mm (slice thickness = 3.5 mm with 18% slice gap), matrix size = 100 x 100, and field of view
286 = 224 x 224 mm. 30 axial slices were prescribed to cover the entire cortex and were scanned in interleaved
287 order. A custom-modified bipolar water excitation radiofrequency (RF) pulse was used to avoid signal from fat.
288 Anatomical data were collected using a T1-weighted multi-echo MP-RAGE sequence on the same 3T scanner.

289 **fMRI data pre-processing**

290
291
292 Each functional run was motion-corrected using the FMRIB Linear Image Registration Tool (FLIRT) from FSL
293 5.0 (Jenkinson and Smith, 2001; Jenkinson et al., 2002). All volumes in the run were then averaged across
294 time to obtain a high quality template volume. FLIRT was also used to automatically align the template volume
295 for each run to the overall template, which was chosen to be the temporal average of the first functional run for
296 each participant. The temporal average of the cross-modal runs (listening or reading) were also automatically
297 aligned to the same overall template. These automatic alignments were manually checked and adjusted as
298 necessary to improve accuracy. The cross-run transformation matrix was then concatenated to the motion-
299 correction transformation matrices obtained using MCFLIRT, and the concatenated transformation was used
300 to resample the original data directly into the overall template space.

301
302 Low-frequency voxel response drift was identified using a 3rd order Savitsky-Golay filter with a 120-second
303 window. This drift was subtracted from the signal. Responses of each story were z-scored separately, i.e., the
304 mean response for each voxel was subtracted and the remaining response was scaled to have unit variance.
305 Prior to the voxelwise modeling, 10 TRs from the beginning and 10 TRs at the end of each story were discarded.

306 **Cortical surface reconstruction and visualization**

307
308
309 Cortical surface meshes were generated from the T1-weighted anatomical scans using Freesurfer software (Dale
310 et al., 1999). Before surface reconstruction, anatomical surface segmentations were carefully hand-checked and
311 corrected using Blender software and pycortex (Gao et al., 2015) (<http://pycortex.org>). Relaxation cuts were
312 made into the surface of each hemisphere. Blender and pycortex were used to remove the surface crossing the
313 corpus callosum. The calcarine sulcus cut was made at the horizontal meridian in V1 using retinotopic mapping
314 data as a guide.

315
316 Functional images were aligned to the cortical surface using pycortex. Functional data were projected onto the
317 surface for visualization and analysis using the *line-nearest* scheme in pycortex. This projection scheme
318 samples the functional data at 64 evenly-spaced intervals between the inner (white matter) and outer (pial)
319 surfaces of the cortex, then averages together the samples. Samples are taken using nearest-neighbor
320 interpolation, wherein each sample is given the value of its enclosing voxel.

321 **Localizers for known ROIs**

322
323
324 Known regions of interest (ROIs) were localized separately in each participant using standard techniques
325 (Hansen et al., 2007; Spiridon et al., 2006). For all participants ROIs were defined using three experiments: a
326 visual category localizer, an auditory cortex localizer, and a motor localizer. For some participants retinotopic
327 visual ROIs using a retinotopic localizer and area MT+ using an MT localizer were defined.

328
329 **Visual category localizer.** Visual category localizer data were collected in six 4.5-minute scans consisting of
330 16 blocks, each 16 seconds long. During each block, 20 images of either places, faces, human body parts, non-
331 human animals, household objects, or spatially scrambled household objects were displayed. Each image was
332 displayed for 300 ms followed by a 500 ms blank. Occasionally the same image was displayed twice in a row, in
333 which case the participant was asked to respond with a button press.

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The contrast between faces and objects was used to define the fusiform face area (FFA) (Kanwisher et al., 1997) and occipital face area (OFA) (Halgren et al., 1999). The contrast between human body parts and objects was used to define the extrastriate body area (EBA) (Downing et al., 2001). The contrast between places and objects was used to define the parahippocampal place area (PPA) (Epstein and Kanwisher, 1998), occipital place area (OPA) (Nakamura et al., 2000), and retrosplenial cortex (RSC).

Auditory cortex localizer. Auditory cortex localizer data were collected in one 10 minute scan. The participant listened to 10 repeats of a 1-minute auditory stimulus, which consisted of 20-second segments of music (Arcade Fire), speech (Ira Glass), and natural sound (a babbling brook). To determine whether a voxel was responsive to auditory stimuli, the repeatability of the voxel response across the 10 stimulus repeats was calculated using an F -statistic. The F -statistic map was used to define the auditory cortex (AC).

Motor localizer. Motor localizer data were collected during one 10-minute scan. The participant was cued to perform six different motor tasks in a random order in 20-second blocks. For the hand, mouth, foot, speech, and rest blocks the stimulus was simply a word at the center of the screen (e.g. "Hand"). For the saccade block the participant was shown a pattern of saccade targets.

For the "Hand" cue the participant was instructed to make small finger-drumming movements with both hands for as long as the cue remained on the screen. Similarly for the "Foot" cue the participant was instructed to make small toe movements for the duration of the cue. For the "Mouth" cue the participant was instructed to make small mouth movements approximating the nonsense syllables *balabalabala* for the duration of the cue—this requires movement of the lips, tongue, and jaw. For the "Speak" cue the participant was instructed to continuously subvocalize self-generated sentences for the duration of the cue. For the saccade condition the written cue was replaced with a fixed pattern of twelve saccade targets, and the participant was instructed to make frequent saccades between the targets. A linear model was used to find the change in BOLD response of each voxel in each condition relative to the mean BOLD response.

Weight maps for the foot, hand, and mouth responses were used to define primary motor and somatosensory areas for the feet (M1F, S1F), hands (M1H, S1H), and mouth (M1M, S1M); supplementary motor areas for the feet (SMFA) and hands (SMHA); secondary somatosensory area for the feet (S2F) and, in some participants, the hands (S2H); and, in some participants, the ventral premotor hand area (PMVH) (Penfield and Boldrey, 1937). The weight map for saccade responses was used to define the frontal eye field (FEF) (Paus, 1996), frontal operculum eye movement area (FO) (Corbetta et al., 1998), intraparietal sulcus visual areas (IPS), and, in some participants, the supplementary eye field (SEF) (Grosbras et al.). The weight map for speech production responses was used to define Broca's area (BA) (Amunts et al., 2010; Zilles and Amunts, 2018) and the superior ventral premotor speech area (SPMv).

Retinotopic localizer. Retinotopic mapping data were collected in four 9-minute scans. Two scans used clockwise and counterclockwise rotating polar wedges, and two used expanding and contracting rings. Visual angle and eccentricity maps were used to define visual areas V1, V2, V3, V4, LO, V3A, V3B, and V7 (Hansen et al., 2007).

Area MT+ localizer. Area MT+ localizer data were collected in four 90-second scans consisting of alternating 16-second blocks of continuous and temporally scrambled natural movies. The contrast between continuous and temporally scrambled natural movies was used to define visual motion area MT+ (Tootell et al., 1995).

Voxelwise model fitting

A single joint model that included all feature spaces was estimated for each voxel in each dataset (listening and reading) separately using banded ridge regression (see below for details and (Nunez-Elizalde et al., 2019)).

386 Banded ridge regression assigns a different regularization parameter for every feature space and so reduces
 387 bias caused by correlations between feature spaces.

388 **Feature spaces**

389
 390
 391 The feature spaces were motion-energy features (39 parameters), spectral features (80 parameters), word rate
 392 (1 parameter), phoneme rate (1 parameter), phonemes (39 parameters), letter rate (1 parameter), letters (26
 393 parameters), word length variation per repetition time (1 parameter), syntactic features (56 parameters), and
 394 co-occurrence semantics (985 parameters). The motion-energy, spectral, word rate, phoneme rate, phonemes,
 395 letter rate, letters, and word length variation features were used to explain away low-level parameters that
 396 might otherwise contaminate the semantic model weights.

397
 398 Before doing regression, each feature channel was z-scored within each story (training and testing features
 399 were z-scored independently) by subtracting the mean and dividing by the standard deviation. This was done
 400 to match the features to the fMRI responses, which were also z-scored within each story. In addition, 10 TRs
 401 from the beginning and 10 TRs at the end of each story were discarded prior to voxelwise modeling.

402 **Banded ridge regression**

403
 404 We combine several feature spaces in the voxelwise modeling approach. In order to assign different levels of
 405 regularization to each feature space, we estimate all our models simultaneously using banded ridge regression
 406 (Nunez-Elizalde et al., 2019). Under banded ridge regression, brain responses are modeled as a linear
 407 combination of all the feature spaces. However, each feature space is assigned a different value of the
 408 regularization parameter. Banded ridge regression is a special case of the well-established statistical approach
 409 called Tikhonov regression (Tikhonov and Arsenin, 1977). The solution to the Tikhonov regression problem is
 410 given by $\hat{\beta} = \operatorname{argmin}_{\beta} [\|Y - X\beta\|_2^2 + \|\lambda C\beta\|_2^2]$, where C is the penalty matrix. In case of banded ridge regression,
 411 the matrix C is a diagonal matrix whose entries correspond to the regularization levels appropriate for each
 412 feature space. To find the optimal regularization parameter for every feature space a wide range of
 413 regularization parameters is explored using cross-validation. The regularization parameter is optimized based
 414 on prediction accuracy on a held-out data set. Note that in case of $\lambda = 0$ Tikhonov regression reduces to the
 415 ordinary least squares and in case of $C = I$ Tikhonov regression reduces to ridge regression.

416
 417 BOLD responses were modeled as a linear combination of all the feature spaces using linear regression with a
 418 non-spherical spatiotemporal multivariate normal prior on the weights (Nunez-Elizalde et al., 2019). This
 419 approach allows us to impose different levels of regularization on each feature space within the joint model for
 420 each voxel, which is important because of differences in feature space size and signal-to-noise levels. The
 421 regularization parameter for each feature space was estimated empirically via cross-validation on a held-out
 422 set.

423
 424 Within the same model, the hemodynamic response function was modeled using a finite impulse response
 425 (FIR) filter per voxel and for each subject and modality (listening and reading) separately. This was
 426 implemented by modeling the BOLD responses at ten temporal delays corresponding to 0, 2, 4, 6, ..., 16 and 18
 427 seconds. We also imposed a multivariate normal prior on the temporal covariance of the FIR filter. The
 428 temporal prior was constructed from a set of HRF basis functions (Penny et al., 2007).

429 **Cross-validation**

430
 431 We used cross-validation to find the optimal regularization parameter for each feature space in the joint model.
 432 Because evaluating k regularization parameters for m models leads to k^m combinations, conducting a grid-
 433 search in our high-dimensional parameter space is impractical (requiring 10^{10} model fits). To overcome this
 434 problem, we used a tree-structured Parzen search (Bergstra et al., 2011). We performed the search 25 times
 435 each time using different initialization values and stopped each search after 300 iterations. For every set of
 436
 437

438 regularization parameters tested in each iteration, we performed 5-fold cross-validation twice. We used the
439 coefficient of determination (R^2) between the predicted and the actual voxel responses as our performance
440 metric for each validation fold.

441 442 **Model estimation and evaluation**

443
444 We computed the mean prediction performance across cross-validation folds per voxel for each of the 7500
445 (300 x 25) regularization parameter sets tested. The regularization parameters that yielded the maximum
446 cross-validated prediction performance were selected for each voxel. These regularization parameters were
447 then used to estimate the model weights for each of the voxels in each modality independently for each of the
448 nine subjects.

449
450 The estimated model weights were then used to predict the voxel responses to the validation story. Model
451 prediction performance was computed per voxel as the Pearson correlation coefficient between predicted and
452 actual responses.

453
454 To validate the voxelwise models, estimated model weights were used to predict responses to a validation story
455 that was not used for model estimation. Only the estimated semantic model weights were used for model
456 predictions. Pearson's correlation coefficient was computed between the predicted responses and the mean of
457 the two validation datasets (291 time points).

458
459 Statistical significance was computed by a permutation test with 10,000 iterations and comparing estimated
460 correlations to the empirical null distribution of correlations for each participant and modality separately. At
461 each permutation iteration, the time course of the held-out validation dataset was permuted by blockwise
462 shuffling (10 TRs were blocked to account for autocorrelations in voxel responses), and then Pearson's
463 correlation coefficient between the permuted voxel response and the predicted voxel response was computed
464 for each voxel separately. This produced a distribution of 10,000 estimates of correlation coefficients for each
465 voxel, participant, and modality. These 10,000 estimates define an empirical distribution that was used to
466 obtain a p-value. Resulting p-values were corrected for multiple comparisons within each participant using the
467 false discovery rate (FDR) procedure (Benjamini and Hochberg, 1995).

468
469 Voxelwise model fitting and analysis was performed using custom software tikreg (Nunez-Elizalde et al., 2019)
470 written in Python, making heavy use of NumPy (Oliphant, 2006) and SciPy (Oliphant, 2007). Analysis and
471 visualizations were developed using iPython (Perez and Granger, 2007) and the interactive programming and
472 visualization environment jupyter notebook (Kluyver et al., 2016).

473 474 **Semantic PC projections**

475
476 Listening model weights and reading model weights were projected onto the semantic subspace that was
477 created in a previous study from our laboratory (Huth et al., 2016). That study recovered a low-dimensional
478 semantic subspace from an aggregated set of estimated semantic model weights using principal components
479 analysis. Taking the dot product of the estimated model weights with the low-dimensional semantic subspace
480 revealed for each voxel a projection along the 985 semantic principal components (PCs). To visualize which
481 semantic concepts are represented in each voxel we used an RGB color space to map the first three semantic PC
482 projections onto the cortical surface separately for the two modalities (Huth et al., 2012, 2016).

483 484 **Correlating the semantic principal components**

485
486 Pearson's correlation coefficient was computed between each semantic projection in listening and the
487 corresponding semantic projection in reading. To find out whether the semantic projections could be
488 correlated by chance, a permutation test with 10,000 iterations was performed for each individual participant
489 separately. The correlation was computed for the 10,000 best predicted voxels by the co-occurrence semantics
490 model in both modalities. The best predicted voxels were selected by taking an average of listening and reading
491 model prediction accuracies per voxel and selecting the 10,000 voxels with highest mean predictions. At each

492 permutation iteration (i) the time courses of the feature matrix was permuted (note that the feature matrix is
493 the same for listening and reading sessions), (ii) banded ridge regression was performed between the fMRI
494 responses and this permuted matrix, (iii) the estimated model weights were projected onto the semantic
495 principal component space, (iv) Pearson's correlation coefficient between projections of the listening and
496 reading weights onto the semantic subspace were computed separately for each PC. This results in a
497 distribution of 10,000 estimates of correlation coefficients for each semantic PC and participant. Statistical
498 significance was defined as any correlation coefficient that exceeded 95% of all of the permuted correlations.
499

500 **Cross-modality voxelwise model fitting**

501
502 Estimated model weights (see *Voxelwise model fitting*) from one modality (e.g. listening) were used to predict
503 voxel responses in the other modality (e.g. reading). Model prediction accuracy was then computed using
504 Pearson's correlation coefficient between cross-modal prediction responses (e.g. listening model estimates
505 predicting reading responses) and the mean of the two validation responses (e.g. reading responses).
506

507 **RESULTS**

508
509 We sought to determine whether and how the cortical representation of semantic information in narrative
510 language might depend on the modality with which it is perceived. Nine participants listened to and read
511 narrative stories while whole-brain BOLD activity were recorded by means of functional MRI (see **Figure 1**).
512 The experimental stimuli consisted of more than two hours of narrative stories from *The Moth Radio Hour*,
513 along with written transcriptions of the same stories. In the reading condition we used a rapid serial visual
514 presentation (RSVP) method (Buchweitz et al., 2009; Forster, 1970) to present the stories at precisely the same
515 rate as they occurred during listening. That is, in the reading condition each word was presented serially at
516 exactly the same time, and for exactly the same duration as when it was spoken. The semantic content of the
517 stories was estimated continuously by projecting the narrative into a word embedding space based on word co-
518 occurrence statistics (Church and Hanks, 1990; Lund and Burgess, 1996; Mitchell et al., 2008; Turney and
519 Pantel, 2010; Wehbe et al., 2014; Xu et al. 2016). We then used voxelwise modeling to estimate a set of weights
520 for each voxel that best characterize the relationship between the semantic features and the recorded BOLD
521 signals separately for each modality. These estimated model weights were then used to predict voxel responses
522 in a held-out validation dataset both within and across modalities. Finally, the semantic tuning of each voxel in
523 the two modalities was compared by projecting the estimated model weights onto the semantic space described
524 in Huth et al. (2016).
525

526 **Does the cortical distribution of semantically-selective voxels depend on stimulus modality?**

527
528 We used a voxelwise modeling procedure to determine whether the broad distribution of semantically-selective
529 voxels depends on presentation modality. Semantic features were extracted from the stories and these were
530 used to estimate voxelwise model weights for BOLD signals that were recorded while participants listened to
531 the stories in the training set. These estimated model weights were then used to predict fMRI voxel responses
532 to a separate held-out validation set. We repeated the same procedure for the reading sessions. Several low-
533 level features (low-level visual, spectral, word rate, letter rate, word length variation, phonemes, phoneme rate,
534 and pauses) and syntactic features were included alongside the semantic features as nuisance regressors (see
535 **Materials and Methods**), but these nuisance regressors were discarded after regression and the final model
536 predictions were based only on semantic model weight estimates. The correlation coefficient between the
537 actual responses in the held-out validation dataset and predicted responses were computed to give a measure
538 of model prediction accuracy. These were then mapped onto the cortical surface.
539

540
541 **Figure 2** shows voxelwise model prediction accuracy for listening and reading for all voxels in one participant
542 ($p < 0.05$, FDR corrected). **Figure 2a** shows that our semantic model predicts brain activity in a broadly
543 distributed semantic system when participants listen to natural stories, replicating a previous study from our
544 lab (Huth et al., 2016). This system extends across much of lateral temporal cortex (LTC), ventral temporal

545 cortex (VTC), lateral parietal cortex (LPC), medial parietal cortex (MPC), medial prefrontal cortex, superior
546 prefrontal cortex, and inferior prefrontal cortex. **Figure 2b** shows that when participants read natural stories
547 this network of brain regions are similarly well predicted by the semantic model. **Figure 2c** compares
548 prediction accuracy of semantic models fit to listening (depicted on the x-axis) versus reading (depicted on the
549 y-axis). The saturation of each point represents the number of voxels that fall into a given range of prediction
550 accuracy. Most voxels are approximately equally well predicted in both modalities. Overall, the semantic model
551 accurately predicts activity in most of the semantic system independent of the presentation modality.

552
553 **Figure 3** shows voxelwise model prediction accuracy for listening and reading for all voxels and across nine
554 participants in the standard MNI brain space. **Figure 3a** and **3b** show average prediction accuracy across all
555 participants in listening and reading, respectively. **Figure 3c** and **3d** show for each voxel the number of
556 participants where semantic model prediction accuracy is significant in listening and reading, respectively.
557 These results show that our semantic model predicts brain activity within the semantic system in all
558 participants. However, due to averaging across participants voxel prediction accuracies are lower than in
559 individual participant results (maximum prediction accuracy across all MNI voxels for listening 0.27 ± 0.03 ,
560 maximum prediction accuracy across all MNI voxels for reading: 0.28 ± 0.03).

561 **Does the representation of semantic information vary with sensory modality?**

562
563 In order to determine whether semantic representation is modality independent we compared the semantic
564 tuning of each voxel estimated during listening versus reading. The semantic tuning of each voxel is given by a
565 985-dimensional vector of weights, one weight for each of the 985 semantic features. Because there are
566 ~80,000 cortical voxels in each individual participant and 985 semantic features it is impractical to make
567 comprehensive comparisons for each feature. Therefore, to simplify interpretation the estimated semantic
568 model weights were projected into a low-dimensional semantic subspace that captures most of the information
569 about the semantic selectivity of the voxel population. This semantic subspace was created by applying
570 principal component analysis to an aggregated set of estimated semantic model weights from seven
571 participants included in a previous study from our laboratory (Huth et al., 2016). (Note that three of those who
572 participated in the earlier study are also included in the current study.) The resulting semantic principal
573 components (PCs) are ordered by how much variance they explain across the voxels. By projecting both the
574 listening model weights and the reading model weights separately into these semantic PCs, we ensure that
575 cortical voxels that represent similar concepts will project to nearby points in the semantic space.

576
577 To visualize which semantic concepts are represented in each voxel, we mapped the projections of the first
578 three semantic principal components onto each participant's cortical surface separately for the two modalities.
579 Each voxel was then colored according to a simple RGB color scheme, where the color red represents the first
580 semantic PC, the color green represents the second semantic PC, and blue the third semantic PC. Inspection of
581 the listening and reading semantic maps shown in **Figure 4** reveals that the semantic representations in both
582 modalities are very similar. The similarity between the listening and reading semantic maps indicate that
583 individual voxels within the semantic system are tuned for the same semantic concepts regardless of
584 presentation modality.

585
586 To quantify the similarity between the semantic maps shown in **Figure 4** for all participants, we correlated the
587 projections of the listening and reading model weights into the semantic PCs across the two modalities
588 (listening and reading). To reduce noise, the 10,000 voxels that were best predicted by the semantic model in
589 the two modalities were selected for this analysis. The listening and reading semantic PC projections were then
590 correlated for each semantic PC separately.

591
592 **Figure 5** shows these correlation coefficients for the first ten semantic PC projections and for all nine
593 participants. Each colored line shows the correlation between listening and reading semantic projections for
594 one participant. The dotted lines indicate the upper bound of the 95% confidence interval of the correlation
595 value under the null hypothesis. Hence, the dotted lines can be interpreted as a form of statistical significance
596 as estimated by a permutation test (see **Materials and Methods** for details). Inspection of **Figure 5** reveals
597 that the first five semantic PC projections are significantly correlated between listening and reading modalities.
598

599 The first three semantic PC projections are those that are mapped onto the cortical surface in **Figure 4**.
600 Correlations of the sixth PC projection and beyond are relatively weaker, but remain above chance level until
601 the seventh PC projection. Taken together, these results indicate that the cortical representation of semantic
602 information is consistent across input modalities.

603 604 **Is semantic tuning consistent across modalities at the single voxel level?**

605
606 Here we sought to determine whether all the dimensions of semantic representation depend on input modality
607 at the level of single voxels. To do this the 985 semantic model weights estimated for each voxel during
608 listening were correlated with those semantic model weights estimated during reading.

609
610 **Figure 6a** shows the correlation coefficient between estimated listening and reading model weights for each
611 voxel, mapped onto the cortical surface of one individual participant. Listening and reading model weights are
612 strongly correlated in many regions within the semantic system including bilateral temporal, parietal, and
613 prefrontal cortices (red voxels in **Figure 6a**). These voxels are also significantly well predicted by the semantic
614 model in both modalities. Voxels whose model weights are not correlated are located in few scattered voxels in
615 the bilateral sensory cortex, intraparietal sulcus, and in prefrontal cortex (white voxels). This suggests that
616 voxels that are semantically selective in Listening and Reading modalities (red) represent similar semantic
617 information. **Figure 6b** summarizes the relation between within-modality voxelwise model prediction
618 accuracy and semantic tuning, for each voxel. Each voxel is a single point in the scatterplot, and the correlation
619 between the estimated listening and reading model weights is indicated by the color saturation. Semantic
620 tuning is more similar for voxels that are semantically selective in both modalities (red) than for those that are
621 well predicted in one modality only (blue or green). Negatively correlated voxels are mostly in sensory regions
622 and are not well predicted by the semantic model in either modality. In general, individual voxels located
623 within the semantic system are selective to similar semantic features during both listening and reading.

624 625 **Can a voxelwise model fit to one modality predict responses to the other modality?**

626
627 If the semantic representation in most of the semantic system is modality-invariant then voxel models fit to
628 one modality should accurately predict responses in the other modality. **Figure 7** and **Figure 8** show cross-
629 modal predictions for all voxels in all participants. **Figure 7** shows prediction accuracy for a model fit to voxel
630 responses evoked during listening, but predicting responses evoked during reading. **Figure 8** shows prediction
631 accuracy for a model fit to responses evoked during reading, but predicting responses evoked during listening.
632 In both figures voxels whose predictions were not statistically significant are shown in gray ($p > 0.05$, FDR
633 corrected). In both cases, voxels in bilateral temporal, parietal, and prefrontal cortices are well predicted across
634 modalities. Voxels that are not well predicted cross-modally are located in sensory cortices.

635
636 **Figure 9** shows a summary map of the relationship between cross-modality predictions and within-modality
637 predictions, for each voxel and all participants. Summary statistics for the two cross-modality predictions were
638 computed by taking the average cross-modality prediction accuracy (per voxel average of **Figure 7** and **Figure**
639 **8**). Summary statistics for the two within-modality predictions were computed by taking the maximum within-
640 modality prediction accuracy (per voxel maximum of **Figure 2a** and **Figure 2b**). The mean cross-modality
641 prediction accuracy and the maximum within-modality prediction accuracy per voxel were then mapped onto
642 the same participant's flattened cortical surface. Inspection of **Figure 9** allows us to identify voxels that are
643 well predicted both within and across modality. Most voxels that are well predicted within and across modality
644 are located in the semantic system (white voxels in **Figure 9**). Outside the semantic system, some voxels on
645 the border to visual cortex and voxels surrounding the temporal parietal junction are well predicted within
646 modality but not across modality (orange voxels in **Figure 9**). (Note, however, that within-modality data were
647 collected largely within sessions, and between-modality data were collected across sessions. Thus, within-
648 modality prediction accuracy is likely to be somewhat higher than between-modality accuracy for this reason
649 alone.) This result demonstrates that the distribution of semantically selective voxels in most of the semantic
650 system is independent of the modality.

651 652 **DISCUSSION**

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The experiments presented here were designed to determine whether semantic information obtained during listening and reading are represented within a common underlying semantic system. In separate fMRI sessions participants listened to a spoken story and read a stream of words visually (RSVP using time-locked transcripts of spoken stories). We used voxelwise modeling to estimate semantic selectivity across the entire cerebral cortex, in individual participants, in each voxel separately and in two different presentation modalities (listening and reading).

Our experiments provide three lines of evidence in support of the hypothesis that semantic representations throughout most of the semantic system are invariant to presentation modality. First, voxels in most of the semantic system (temporal, parietal, and prefrontal cortices) are well predicted by the semantic model in each modality independently (**Figure 2-3**). Second, the estimated model weights and the semantic maps are similar between listening and reading (**Figure 4-6**). Third, voxelwise models estimated from one modality (e.g. listening) accurately predict responses in the other modality (e.g. reading) throughout most of the semantic system (**Figure 7-9**).

Our results demonstrate in a single study that semantically amodal voxels span most of the bilateral semantic system. It has been previously proposed that subsequent to early sensory processing, the pathways for processing information by listening or reading converge in semantically-selective regions (Booth et al., 2002; Buchweitz et al., 2009; Carpentier et al., 2001; Chee et al., 1999; Cohen et al., 2004; Constable et al., 2004; Jobard et al., 2007; Liuzzi et al., 2017; Patterson et al., 2007; Spitsyna et al., 2006). Different studies have emphasized different brain regions such as the left anterior temporal lobe, left ventral angular gyrus, left inferotemporal cortex, a region left lateral to the visual word form area (VWFA), left MTG, and the left IFG. Bilateral activations have been reported previously in epileptic patients (Carpentier et al., 2001) or when complex stimuli such as narrative has been used (Jobard et al., 2007; Regev et al., 2013; Spitsyna et al., 2006). Our study shows that semantically amodal voxels are bilaterally distributed across many regions of the temporal, parietal and prefrontal cortices (**Figure 3-6**). Specifically, we show amodal semantic representation in bilateral precuneus, temporal parietal junction (TPJ), angular gyrus (AG), anterior to posterior superior temporal sulcus (STS), superior ventral premotor cortex (sPMv), Broca's area and inferior frontal gyrus (IFG).

One previous report noted that listening and reading evoke different levels of brain activity in anterior and posterior left DLPFC (Regev et al., 2013). However, Regev et al. (2013) did not model linguistic features directly. Therefore, it is unclear whether the differences they identified within left DLPFC are due to differences in semantic representation or some other aspect of linguistic information (e.g. syntax). In our study, we focused solely on semantic representations and our results suggest that semantic representations do not differ between listening and reading in left DLPFC. However, it is possible that this structure may represent other types of linguistic information differently during listening and reading.

One striking difference between our results and those reported in earlier studies is that we find a large network of semantically-selective regions that are independent of the presentation modality, whereas previous studies reported a few amodal semantic regions located mostly in the left hemisphere (Buchweitz et al., 2009; Chee et al., 1999; Jobard et al., 2007; Liuzzi et al., 2017; Petersen et al., 1989). There are three possible factors that contribute to this discrepancy. First, we used rich narrative language as stimuli to study cross-modal semantic representation (**Figure 1**). Previous studies have shown that complex linguistic stimuli such as narrative stories activate many more brain regions than single words or short sentences (Jobard et al., 2007; Lerner et al., 2011; Mazoyer et al., 1993; Xu et al., 2005). Hence, differences in signal-to-noise ratio can account for fewer number of amodal regions identified in previous cross-modality studies that use single words or short sentences.

Second, our voxelwise modeling approach used explicit semantic features, which allowed us to identify brain regions that consistently respond to specific semantic information across different modalities (**Figure 1-6**). To our knowledge, only one previous study of cross-modal representation has used explicit semantic features to model brain activity patterns related to semantics (Liuzzi et al., 2017). That study used as stimuli twenty-four

703 single words derived from only six animate categories, and showed cross-modal representations within left
704 pars triangularis. However, the most likely reason that the Luizzi et al. (2017) study only identified one region
705 as semantically amodal is that single word presentations elicit little brain activity.
706

707 Third, the present study is the first that reveals the amodal representation of semantic information during
708 listening and reading in single participants (**Figure 1**). In contrast, most previous neuroimaging studies of
709 language perform comparisons at the group level after transforming individual participant data into a
710 standardized brain space (e.g. MNI or Talairach space). However, the anatomical normalization procedures
711 used in these studies tend to smooth and mask the substantial individual variability in language processing
712 (Caramazza, 1986; Fedorenko and Kanwisher, 2009; Steinmetz and Seitz, 1991). Therefore, studies performing
713 inter-subject averaging might average away meaningful signal and fail to find significant relationships
714 (Fedorenko and Kanwisher, 2009). Indeed, projecting our results into a standard brain space and averaging
715 across individuals reduces prediction performance within modality across much of the brain (compare **Figure**
716 **3a** and **Figure 2**). This result already demonstrate that it is important to study cross-modal language
717 representations in individual participants.
718

719 Our naturalistic experiment and voxelwise modeling provides a powerful and efficient method for identifying
720 amodal representations in individual human brains. However, the semantic feature space that we used here is
721 only one possible way of representing semantics (Huth et al., 2016; Mitchell et al., 2008; Pereira et al., 2018),
722 and it has some limitations. For example, when people listen to or read a story they likely employ conceptual
723 knowledge at long time scales beyond those using for computing semantic features (Yeshurun et al., 2017).
724 Furthermore, semantic comprehension involves metaphors, humor, sarcasm and narrative information that is
725 not reflected in the current semantic model. It is possible that these unmodeled properties of natural language
726 might have different, modality-specific representations in the brain.
727

728 In sum, we demonstrate modality-independent semantic selectivity in most of the bilateral semantic system.
729 The semantic maps recovered in this study show that semantic tuning in individual participants is very similar
730 across the two modalities. Our findings are consistent with the view that sensory regions process unimodal
731 information related to low-level processing of spoken or written language, whereas high-level regions process
732 modality invariant semantic information. Furthermore, our results reveal that modality invariant semantic
733 representations are not isolated in a few left-lateralized regions, but are instead present in many bilaterally
734 distributed regions of the semantic system.

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908

909 **Figure Legends**
910

911 **Figure 1: Experimental procedure and voxelwise modeling.** Nine participants listened to and read over two hours
912 of natural stories in each modality while BOLD responses were measured using fMRI. The presentation time of single
913 words was matched between listening and reading sessions. Semantic features were constructed by projecting each word
914 in the stories into a 985-dimensional word embedding space independently constructed using word co-occurrence statistics
915 from a large corpus. These features and BOLD responses were used to estimate a separate finite impulse response (FIR)
916 banded ridge regression model for each voxel in every individual participant. These estimated model weights were used to
917 predict BOLD responses for a separate held-out story that was not used for model estimation. Predictions for individual
918 participants were computed separately for listening and reading sessions. Model performance was quantified as the
919 correlation between the predicted and recorded BOLD responses to this held-out story. Within-modality prediction
920 accuracy was quantified by correlating the predicted responses from one modality (e.g. listening) with the recorded
921 responses to the same modality (e.g. listening). Cross-modality prediction accuracy was quantified by correlating the
922 predicted responses for one modality (e.g. listening) with the recorded responses of the other modality (e.g. reading).

923 **Figure 2: Semantic model prediction accuracy across the cortical surface.** Voxelwise modeling was used to
924 estimate semantic model weights in two modalities, listening and reading. Prediction accuracy was computed as the
925 correlation (r) between the participant's recorded BOLD activity to the held-out validation story and the responses
926 predicted by the semantic model. **a.** Accuracy of voxelwise models estimated using listening data and predicting withheld
927 listening data. The flattened cortical surface of one participant is shown. Prediction accuracy is given by the color scale
928 shown at bottom. Voxels that are well predicted appear yellow or white, voxel predictions that are not statistically
929 significant are shown in gray ($p > 0.05$, FDR corrected; LH, left hemisphere; RH, right hemisphere; NS, not significant;
930 EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex; LPC, lateral
931 parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex). **b.** Accuracy of voxelwise models estimated using
932 reading data and predicting withheld reading data. The format is the same as panel **a.** Estimated semantic model weights
933 accurately predict BOLD responses in many brain regions in the semantic system, including lateral temporal cortex (LTC),
934 ventral temporal cortex (VTC), lateral parietal cortex (LPC), medial parietal cortex (MPC), and prefrontal cortex (PFC) in
935 both modalities. In contrast, voxels in the early sensory regions such as the primary auditory cortex and early visual cortex
936 are not well predicted. **c.** Log transformed density plot of the listening (x-axis) versus reading (y-axis) model prediction
937 accuracy. Purple points indicate all voxels. Darker colors indicate a higher number of voxels in the corresponding bin.
938 Voxels with listening prediction accuracy < 0.17 and reading prediction accuracy < 0.19 are not significant. Most voxels
939 are equally well predicted in listening and reading indicating that these voxels represent semantic information
940 independent of the presentation modality.

941 **Figure 3: Semantic model prediction accuracy across all participants in standard brain space.** Voxelwise
942 modeling was used to assess semantic model prediction accuracy in the listening and reading modalities for all nine
943 participants as described in **Figure 2a** and **Figure 2b**. Prediction accuracies computed in individual subject's space were
944 then projected into a standard MNI brain space. **a.** Average listening prediction accuracy across nine participants was
945 computed for each MNI voxel in the standard brain space and is mapped onto the cortical surface of the MNI brain.
946 Average prediction accuracy is given by the color scale. Voxels that are well predicted appear brighter. Across all
947 participants the estimated semantic model weights in the listening modality accurately predict BOLD responses in many
948 brain regions in the semantic system, including lateral temporal cortex (LTC), ventral temporal cortex (VTC), lateral
949 parietal cortex (LPC), medial parietal cortex (MPC), and prefrontal cortex (PFC). (LH: Left hemisphere, RH: Right
950 hemisphere, EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex;
951 LPC, lateral parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex) **b.** Average reading prediction accuracy
952 across nine participants was computed for each MNI voxel in the standard brain space and is mapped onto the cortical
953 surface of the MNI brain. The format is the same as in **a.** Across all participants, estimated semantic model weights in the
954 reading modality accurately predict BOLD responses in the semantic system. **c.** Significant prediction accuracy in each
955 voxel in the listening modality was determined in the subject space and then projected to the standard MNI brain space.
956 The number of subjects with significant semantic model prediction accuracy for a given MNI voxel is then mapped onto
957 the cortical surface of the MNI brain. Number of participants is given by the color scale shown at bottom. Dark red voxels
958 are significantly well predicted in all participants. Dark blue voxels are not significantly predicted in any participant. **d.**
959 Significant prediction accuracy in each voxel in the reading modality was determined in the subject space and then
960 projected to the standard MNI brain space. The number of subjects with significant semantic model prediction accuracy
961 for a given MNI voxel is then mapped onto the cortical surface of the MNI brain. The format is the same as in **c.** Most of
962 the voxels in the semantic system are significantly predicted by all participants in both modalities.

963 **Figure 4: Semantic tuning maps for listening and reading.** The semantic maps for both modalities are displayed
964 on the cortical surface of one participant. **a.** Voxelwise model weights for the listening sessions were projected into a

semantic space created by performing principal component analysis on estimated semantic model weights acquired during a listening experiment published earlier (Huth et al., 2016). Each voxel is colored according to its projection onto the first (red), second (blue) or third (green) semantic PC. The color wheel legend at center indicates the associated semantic concepts. Voxels whose within-modality prediction was not statistically significant are shown in gray ($p > 0.05$, FDR corrected; LH, left hemisphere; RH, right hemisphere; EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex; LPC, lateral parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex). **b.** Voxelwise model weights for the reading sessions projected into the semantic space, and colored using the same procedure as in **a.** Comparison of panels a and b reveals that semantically selective voxels are tuned for similar semantic concepts during both listening and reading.

Figure 5: Similarity between listening and reading semantic PC projections. The correlation coefficient between listening and reading semantic PC projections are shown for the first ten semantic PCs and each individual participant separately. Each colored diamond shape indicate one participant and the mean correlation coefficient across participants is indicated by the black solid line. Error bars are standard error of the mean across the correlation coefficients for all participants. The colored dotted lines at the bottom indicate chance level correlation for each semantic PC and participant as computed by a permutation test. At least the first five semantic PC projections are significantly correlated between listening and reading. This shows that the individual dimensions of the semantic maps in **Figure 4** where the first three semantic PCs are displayed are similar across the two modalities.

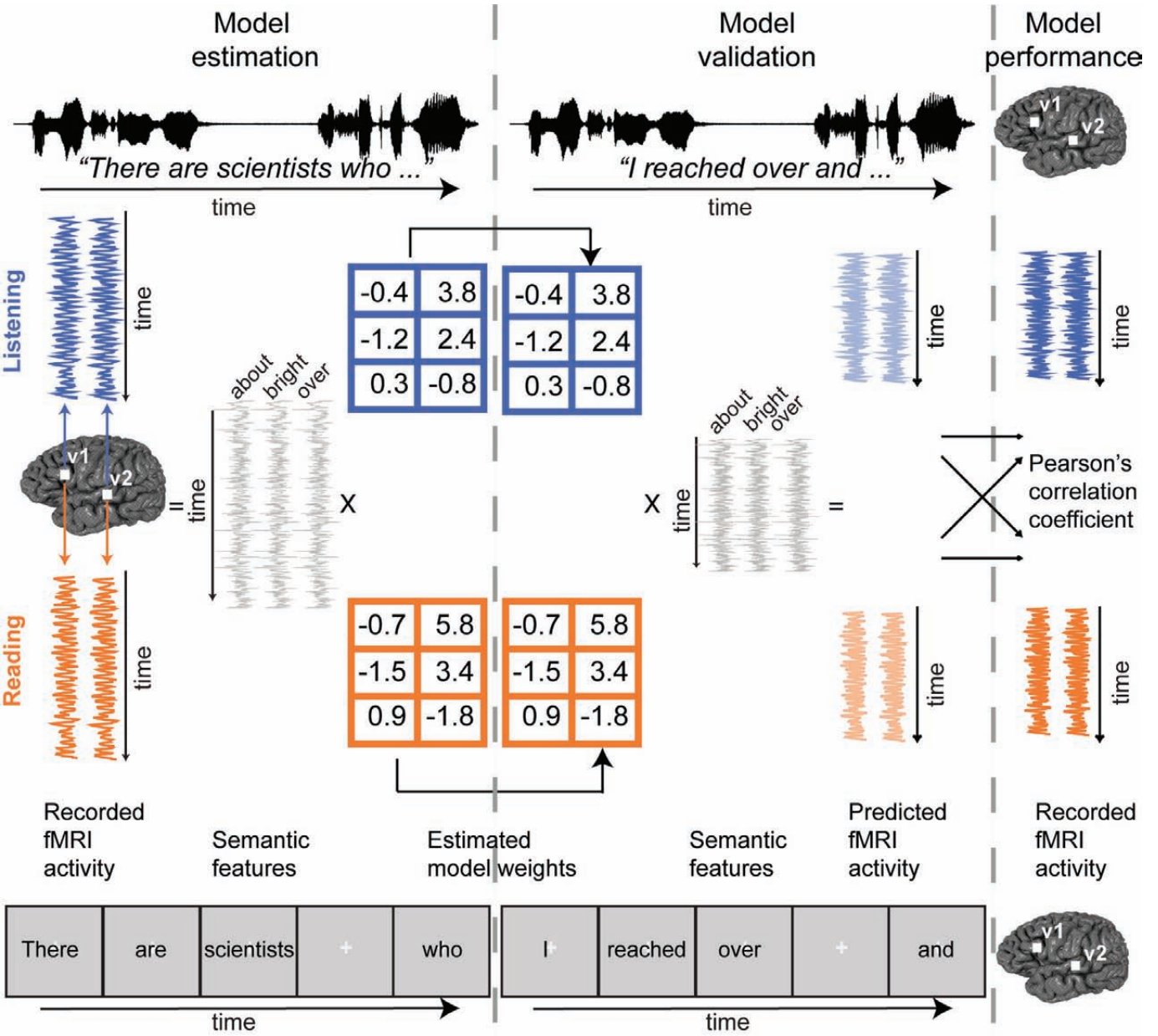
Figure 6: Voxelwise similarity of semantic tuning across listening and reading. Semantic model weights estimated during listening and reading were correlated for each voxel separately. **a.** Correlation coefficient between listening and reading model weights are shown on the flattened cortical surface of one participant. Red voxels are those that are semantically selective in both modalities. Blue voxels are those that are semantically selective in listening, but not reading. Green voxels are those that are semantically selective in reading, but not listening. Gray voxels are not semantically selective in either modality. Color saturation describes the strength of voxel weight correlations. The stronger the color the higher is the correlation between listening and reading model weights. Voxels in the semantic system have similar semantic tuning across all the semantic features. (LH, left hemisphere; RH, right hemisphere; NS, not significant; EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex; LPC, lateral parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex) This suggests that across the 985 semantic features semantic information is represented similarly in both modalities in the semantic system. **b.** The relation between within-modality model prediction accuracy and semantic tuning. Listening (x-axis) versus reading (y-axis) prediction accuracy is shown in a scatterplot where each point corresponds to a single voxel in panel **a.** The correlation between the listening and reading model weights is indicated by color saturation and is the same as in panel **a.** Semantic tuning is more similar for voxels that are semantically selective in both modalities (red) than for those that are selective in one modality only (blue and green). Gray voxels are not semantically selective in either modality. This suggests that voxels that are well predicted in both modalities represent similar semantic information.

Figure 7: Semantically amodal voxels as shown by cross-modal predictions (Listening predicting Reading) in all participants. Estimated semantic model weights in the listening modality were used to predict BOLD activity to the held-out validation story in the reading modality. **a.** Accuracy of voxelwise models estimated during listening predicting reading responses, shown on the same participant's flattened cortical surface as in Figure 2. Prediction accuracy is given by the color scale. Voxels that are well predicted appear yellow or white, voxel predictions that are not statistically significant are shown in gray ($p > 0.05$, FDR corrected; LH, left hemisphere; RH, right hemisphere; NS, not significant; Si: Subject i; EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex; LPC, lateral parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex). **b.** Accuracy of voxelwise models estimated during listening predicting reading responses, shown for all other participants. The format is the same as panel **a.** The semantic model estimated in listening accurately predicts voxel responses in reading within the semantic system including bilateral temporal (LTC, VTC), parietal (LPC, MPC), and prefrontal cortices (PFC).

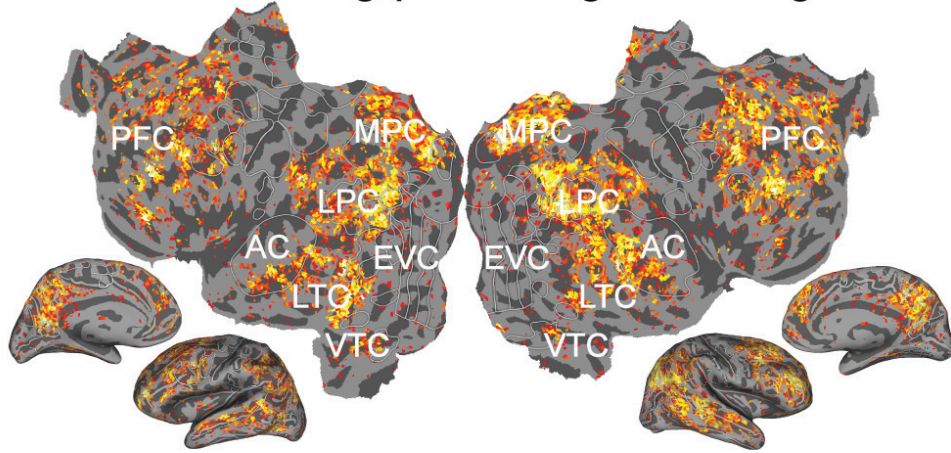
Figure 8: Semantically amodal voxels as shown by cross-modal predictions (Reading predicting Listening) in all participants. Estimated semantic model weights in the reading modality were used to predict BOLD activity to the held-out validation story in the listening modality. **a.** Accuracy of voxelwise models estimated during reading predicting listening responses, shown on the same participant's flattened cortical surface as in Figure 2. Prediction accuracy is given by the color scale. Voxels that are well predicted appear yellow or white, voxel predictions that are not statistically significant are shown in gray ($p > 0.05$, FDR corrected; LH, left hemisphere; RH, right hemisphere; NS, not significant; Si: Subject i; EVC, early visual cortex; AC: auditory cortex; LTC, lateral temporal cortex, VTC, ventral temporal cortex; LPC, lateral parietal cortex; MPC, medial parietal cortex; PFC, prefrontal cortex). **b.** Accuracy of voxelwise models estimated during reading predicting listening responses, shown for all other participants. The format is the same as panel **a.** The semantic model estimated in reading accurately predicts voxel responses in listening within the semantic system including bilateral temporal (LTC, VTC), parietal (LPC, MPC), and prefrontal cortices (PFC).

021 **Figure 9: Semantically amodal voxels for all participants.** Comparison of voxels that are well predicted across
022 modalities versus within modalities. **a.** The average cross-modality prediction accuracy and the maximum of the within-
023 modality prediction accuracy per voxel are both plotted on the flattened cortical surface of the same participant's flattened
024 cortical surface as in Figure 2. (L2R: Listening predicting Reading, R2L: Reading predicting Listening; L2L: Listening
025 predicting Listening, R2R: Reading predicting Reading; Si: Subject i; LH, left hemisphere; RH, right hemisphere; NS, not
026 significant). Orange voxels are well predicted only within-modality. White voxels are well predicted both within and across
027 modality (in most of the semantic system). Blue voxels are well predicted only across modality. Voxels that are not
028 significant in within- or cross-modality predictions are shown in gray. **b.** The same comparison is plotted for all other
029 participants. The format is the same as panel **a.** Voxels within the semantic system represent semantic information
030 independent of modality.

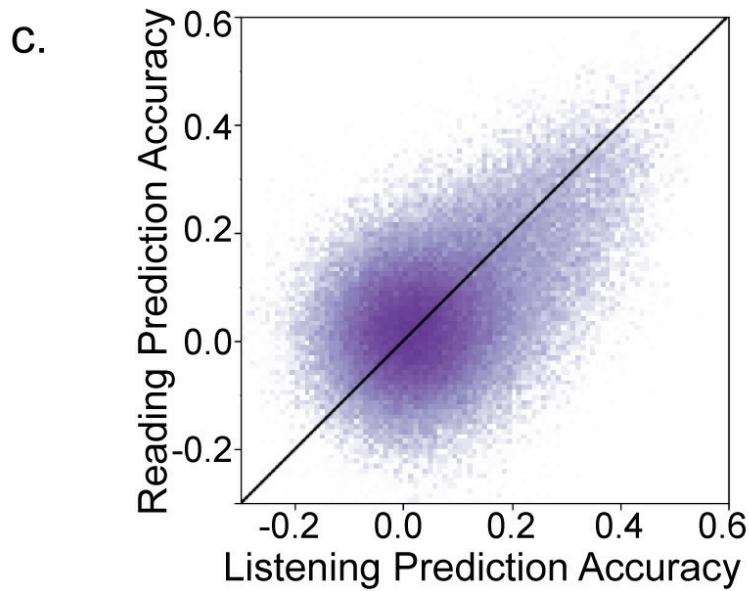
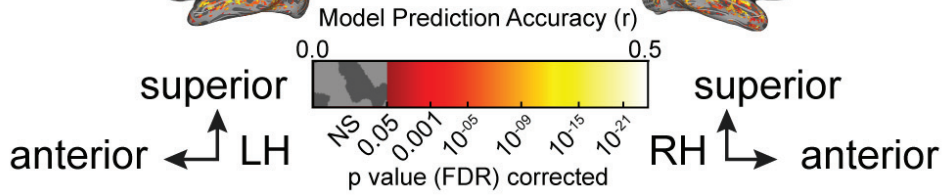
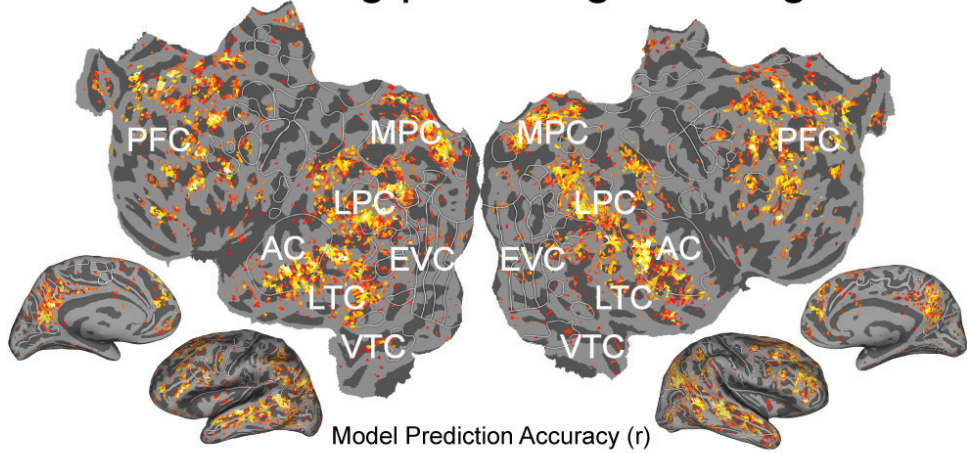
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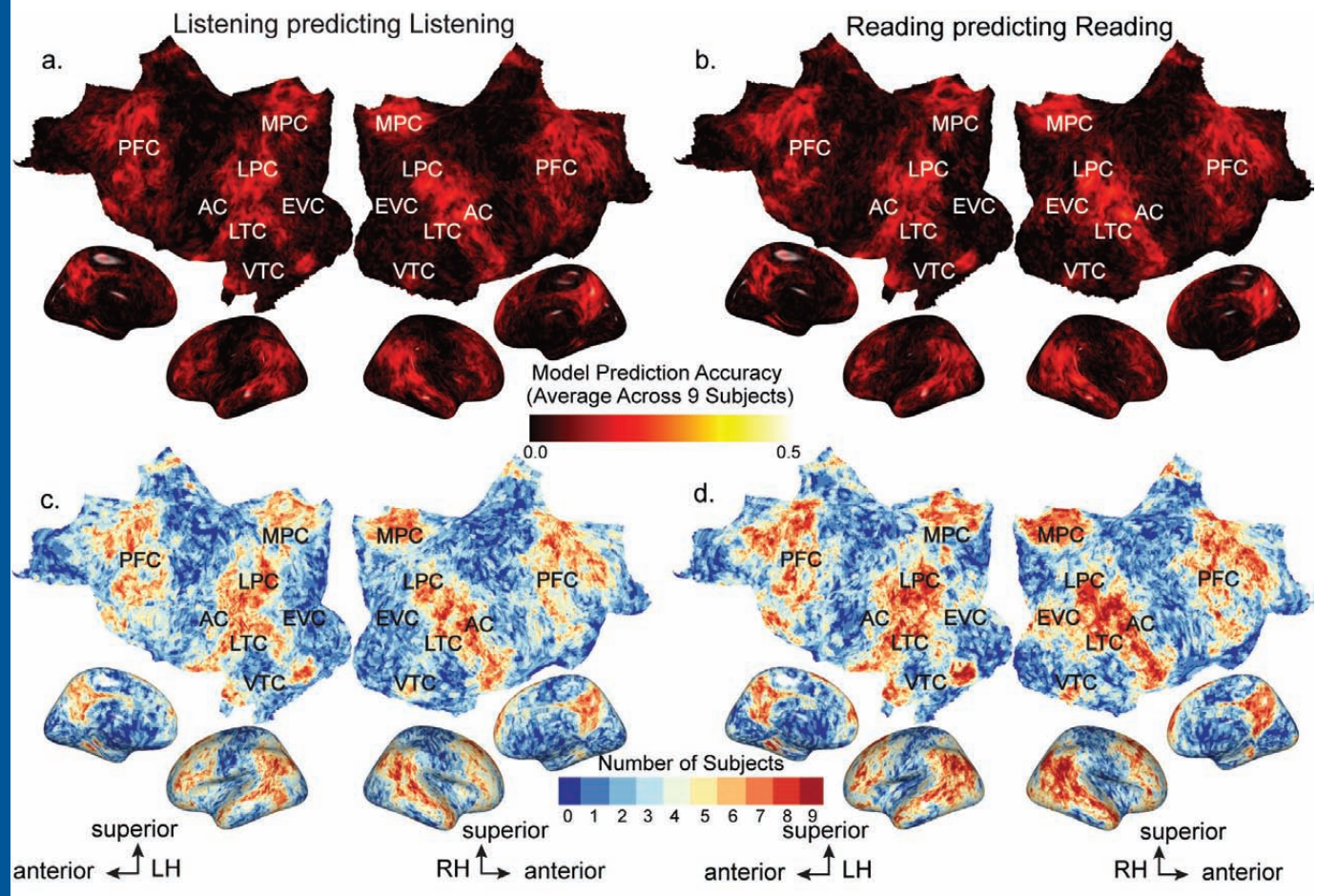


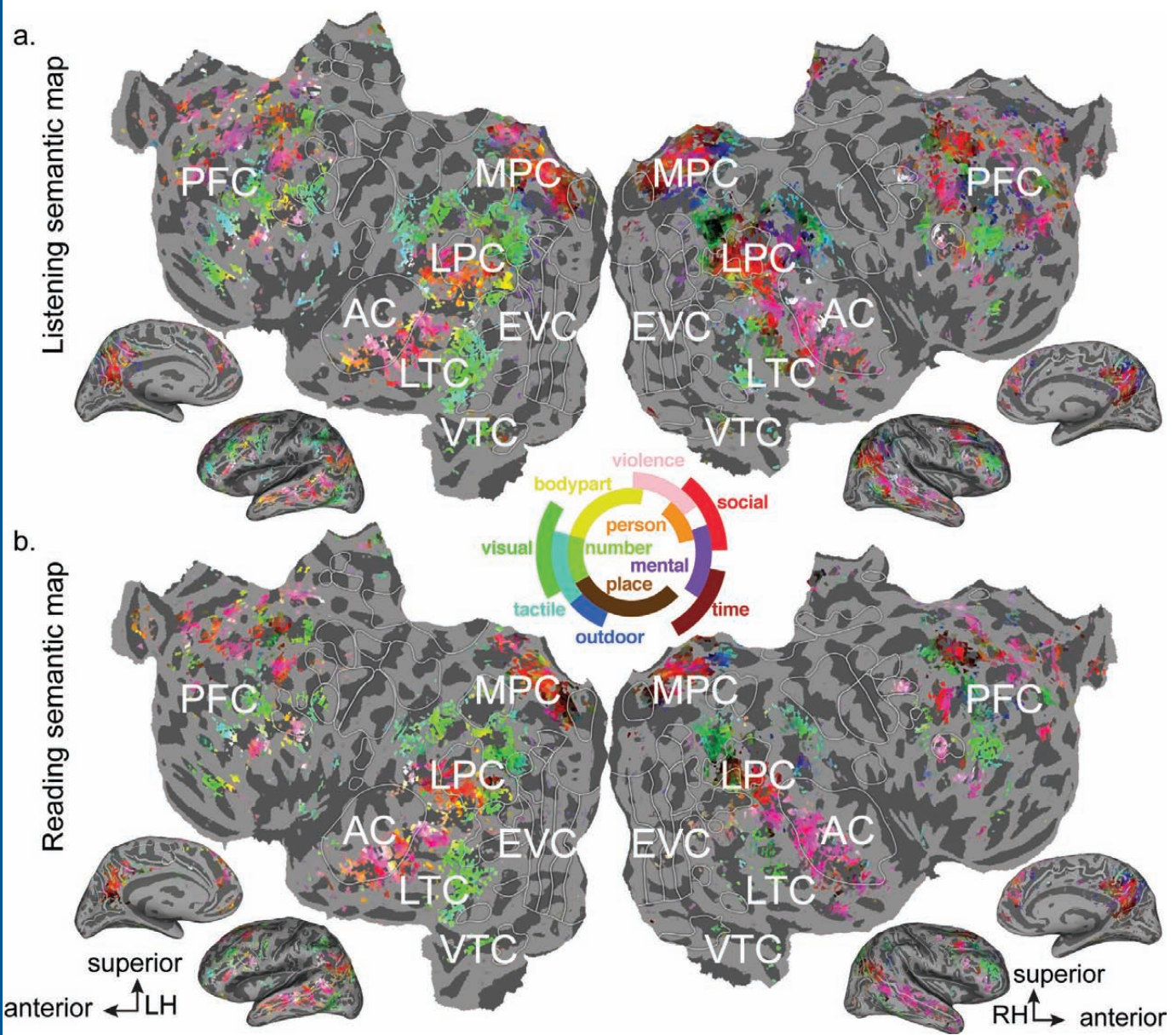
a. Listening predicting Listening

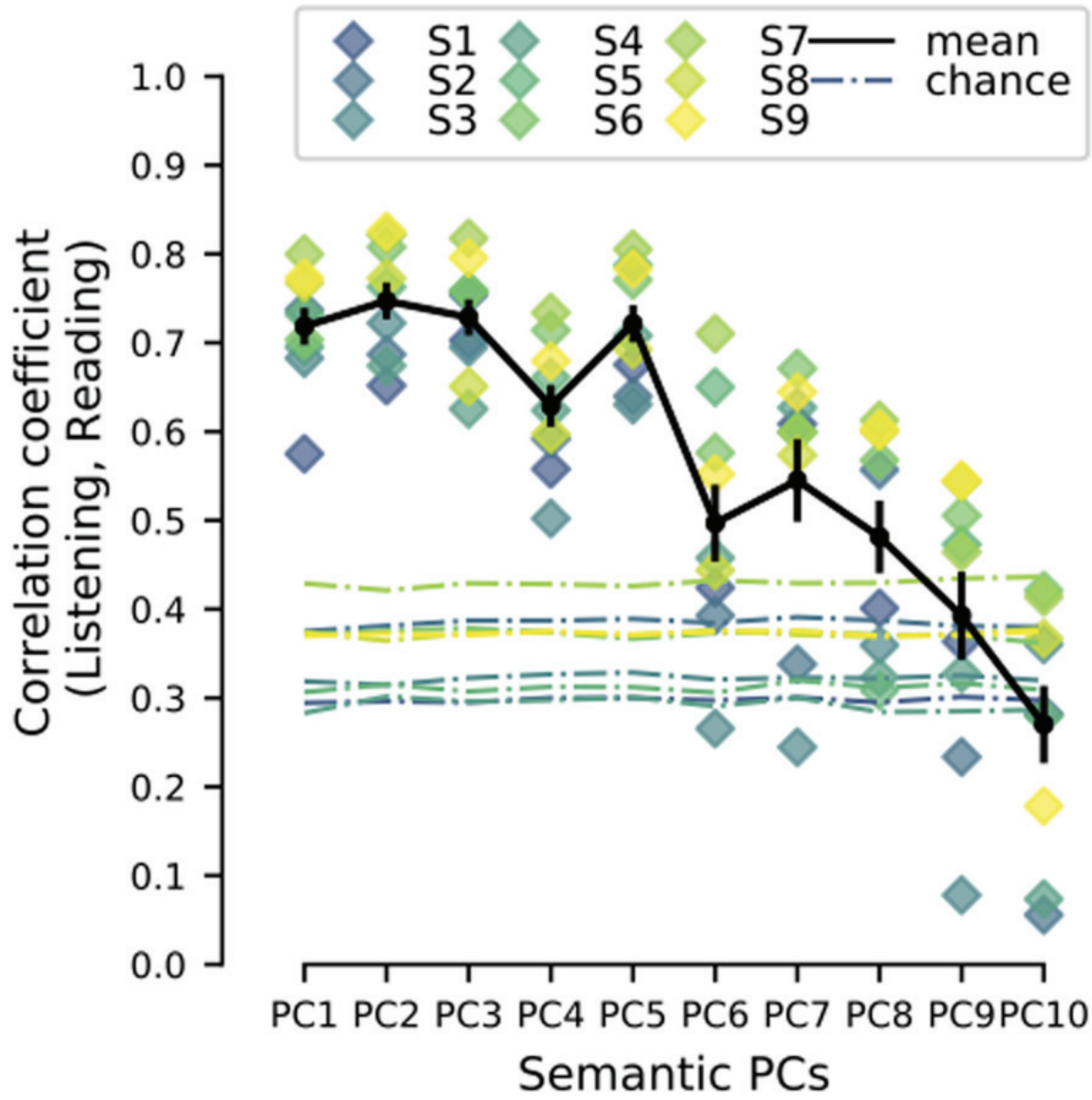


b. Reading predicting Reading









a. Correlation between listening and reading model weights

