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Exposing pathological sensory predictions in tinnitus using auditory intensity deviant evoked responses

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1 **Exposing pathological sensory predictions in tinnitus using auditory**
2 **intensity deviant evoked responses**

3
4 **Abbreviated title:** Sensory predictions in tinnitus

5
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32 **Competing interests**

33 The authors declare no competing interests.

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38 **Abstract**

39 We tested the popular, unproven theory that tinnitus is caused by resetting of auditory
40 predictions towards a persistent low-intensity sound. Electroencephalographic mismatch
41 negativity responses, which quantify the violation of sensory predictions, to unattended
42 tinnitus-like sounds were greater in response to upward than downward intensity deviants
43 in 26 unselected chronic tinnitus subjects with normal to severely-impaired hearing, and in
44 15 acute tinnitus subjects, but not in 26 hearing and age-matched controls ($p < 0.001$, ROC
45 AUC 0.77), or in 20 healthy and hearing-impaired controls presented with simulated
46 tinnitus. The findings support a prediction resetting model of tinnitus generation, and may
47 form the basis of a convenient tinnitus biomarker, which we name Intensity Mismatch
48 Asymmetry (IMA), that is usable across species, that is quick, tolerable and requires no
49 training.

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53 **Significance statement**

54 In current models, perception is based around the generation of internal predictions of the
55 environment, which are tested and updated using evidence from the senses. Here, we test
56 the theory that auditory phantom perception (tinnitus) occurs when a default auditory
57 prediction is formed in order to explain spontaneous activity in the subcortical pathway,
58 rather than ignoring it as noise. We find that chronic tinnitus patients show an abnormal
59 pattern of evoked responses to unexpectedly loud and quiet sounds that both supports this
60 hypothesis and provides fairly accurate classification of tinnitus status at the individual
61 subject level. This approach to objectively demonstrating the predictions underlying
62 pathological perceptual states may also have a much wider utility, for instance in chronic
63 pain.

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66

67 **Introduction**

68 Tinnitus, the persistent perception of an illusory sound, affects 13%, and significantly
69 impairs the quality of life of 2%, of the population. The search for effective treatments is
70 greatly hampered by limited understanding of its mechanisms. Its major risk factor is
71 hearing loss, which leads to increased central gain (i.e. increased firing rate and/or
72 synchrony in for a given input), though a review of current evidence suggests that these
73 changes may be contributory to tinnitus, but not sufficient to cause it, while other evidence
74 suggests that gain increases may be irrelevant, or even protective, with respect to tinnitus,
75 and the presence or absence of hyperacusis can confound results. We have recently
76 proposed a theory of tinnitus causation, which shares some features with an earlier theory,
77 in which a crucial process is the learning of a default ‘tinnitus prediction’ by higher
78 perceptual centres. Specifically, we suggested that the origin of the tinnitus signal is
79 spontaneous firing in the ascending auditory pathway, but that this is usually successfully
80 ignored as irrelevant noise. Furthermore, we proposed that once the brain has recognised
81 the tinnitus signal as a sound source, it forms a default prediction of that sound continuing
82 which prevents the spontaneous activity being ignored as noise, and that prediction ensures
83 the persistence of tinnitus once present for a sufficient length of time. Similar *predictive*
84 *coding* models have been proposed for many perceptual disorders, but actually
85 demonstrating the aberrant predictions themselves is a much greater challenge, hence
86 these models rely on circumstantial evidence. The present work aimed to search for
87 evidence of the existence of a default auditory prediction that might underpin chronic
88 tinnitus. We focused on the mismatch negativity (MMN) evoked response, which occurs

89 across many sensory modalities in response to stimuli that differ (for instance in frequency
90 or intensity) from a series of preceding stimuli. Moreover, MMN magnitude quantitatively
91 indicates the extent to which a particular stimulus violates a prior prediction of what that
92 stimulus will be, making it a useful tool for inferring the content of sensory predictions. In
93 this study, we compared MMN responses, obtained from a roving oddball paradigm
94 featuring pure tones close to the tinnitus frequency, to upward and downward intensity
95 deviants in order to expose alterations of auditory predictions that might be associated with
96 tinnitus (Figure 1). Specifically, because tinnitus is a quieter sound than those used in the
97 experiment, we hypothesised that the tinnitus prediction should skew predictions of
98 intensity downwards, meaning that downward intensity deviants should produce smaller
99 MMN responses, and upward intensity deviants produce larger responses, compared to
100 matched controls. Although there have been numerous MMN studies in tinnitus, the
101 present study differs importantly in that it both targets the tinnitus frequency and features
102 deviants in intensity, and thus is uniquely able to address this hypothesis. Our results
103 showed a striking asymmetry of MMN responses of exactly the type predicted, compared to
104 age and hearing matched controls. This supports the prediction hypothesis of tinnitus
105 (though other interpretations are possible), and can classify individual subjects' tinnitus
106 status with a fair degree of accuracy. The work thus introduces a new potential tinnitus
107 biomarker for further human and animal work.

108

109 **Materials and methods**

110 **Subjects**

111 Unselected chronic tinnitus subjects ($n = 26$) were recruited from local research volunteer
 112 mailing lists, with the only inclusion criteria being age 18 or over, persistent tinnitus for
 113 longer than six months, ability to perform experiments, and absence of structural brain
 114 pathology or profound hearing loss in the tinnitus ear(s). Non-tinnitus controls (matched $n =$
 115 26, and simulated tinnitus $n = 20$) were recruited from the same lists and subjected to pure-
 116 tone audiometry, with the best matches being invited to take part in the full study on a
 117 separate occasion. Acute tinnitus subjects ($n = 15$) were recruited via paid advertising on an
 118 Internet search engine, with the same inclusion criteria as for chronic subjects, but with
 119 tinnitus duration of less than six weeks. Group sizes were chosen as the minimum necessary
 120 to give a high chance of demonstrating the predicted effects. Subject characteristics can be
 121 found in Table 1 of the main text. No significant differences in hearing thresholds (see Figure
 122 5) at any frequency were present between chronic tinnitus subjects and matched controls,
 123 except at 0.5 and 1 kHz in the right ear, which were remote from the stimulus and tinnitus
 124 frequencies ($p < 0.05$).

125 Recruitment and data collection occurred between November 2017 and October 2018, with
 126 additional simulated tinnitus data being collected in August 2019. The study was given a
 127 favourable opinion by the Newcastle University Research Ethics Committee, and all
 128 participants provided written informed consent according to the Declaration of Helsinki.

129

130 **Clinical and psychophysical assessment**

131 All research activity occurred within the Institute of Neuroscience, Newcastle University.
 132 Subjects completed a short questionnaire covering demographic details, health conditions
 133 and medications. Tinnitus subjects also indicated the duration, character and laterality of

134 their tinnitus, along with visual analogue scale (VAS) ratings of their average and current
 135 tinnitus loudness, average annoyance, and completed the Tinnitus Handicap Inventory (THI).
 136 All subjects underwent pure tone audiometry at octave intervals from 0.25 to 8 KHz, with
 137 the addition of 6 kHz.

138 Tinnitus subjects performed five rounds of tinnitus matching, using custom-made tools in
 139 Matlab (Mathworks, Natick, MA, USA), based on interactively tuning narrowband noise with
 140 a Hanning-shaped spectrum in terms of its centre frequency (CF), bandwidth (BW), intensity,
 141 and laterality balance. Each round used random starting parameters for CF and BW. Subjects
 142 were allowed to discard matches they regarded as sub-optimal, and the mean CF and BW
 143 across remaining matches were used as a starting point for stimulus generation. Control
 144 subjects used their matched tinnitus-subject's data for stimulus generation.

145 For each subject, two pure tone stimuli of different frequencies were created: one at the
 146 tinnitus match centre, and one at the lower edge of the Hanning passband. Tinnitus subjects
 147 had one opportunity to tune the frequency of these until perceived as in the centre of the
 148 tinnitus frequency band ('centre'), and the other as close as possible to the tinnitus
 149 frequency while being distinctly lower in frequency ('edge'). The rationale for using these
 150 frequencies was to test whether any tinnitus-related effects were tightly locked to the
 151 tinnitus frequency, and whether precise tinnitus frequency matching would be required to
 152 observe these effects. All subjects then iteratively tuned the following parameters in
 153 sequence, until a full round passed with no further changes: laterality balance (centre then
 154 edge), balancing the subjective loudness of both frequencies, tuning overall intensity of
 155 both frequencies. Control subjects were allocated the stimulus frequencies of the tinnitus
 156 subject with the closest audiometric thresholds in stimulus ear/frequency, and were asked

157 to make stimuli as loud as possible without resulting in even minor discomfort, or producing
 158 distortions from the headphones. The additional constraint for tinnitus subjects was that
 159 tinnitus must remain audible in the gaps between stimuli (i.e. tinnitus not be totally
 160 attenuated by residual inhibition).

161

162 **Experimental design**

163 In a soundproof room, 64 channel electroencephalography (EEG) was recorded from
 164 participants, using a Biosemi ActiTwo system (Biosemi, Amsterdam, The Netherlands),
 165 while they were passively presented with the experimental stimuli through Sennheiser HD
 166 380 pro headphones, and watched a silent subtitled movie. Electrode offset (equivalent to
 167 impedance) was kept within manufacturer-recommended limits of ± 40 mV.

168 The paradigm was a roving mismatch negativity (MMN) paradigm, in which 300 ms pure
 169 tones (with 10 ms onset/offset ramps) were presented isochronously with a stimulus onset
 170 asynchrony of 600 ms. Stimuli were presented to the tinnitus ear if entirely or mainly
 171 unilateral (including to the matched control), and bilaterally in other cases. The roved
 172 parameter was stimulus intensity, which randomly alternated between 0 and -6 dB (relative
 173 to the subject-calibrated intensity) every four to eight stimuli. One block of the experiment
 174 comprised 21 such intensity changes, and a total of 50 blocks were presented, alternating
 175 between the centre and edge frequency. A control deviant condition was superimposed on
 176 these sequences, whereby one in ten stimuli (1/6 probability, after minimum separation of
 177 four stimuli) were duration deviants of 150 ms.

178 Simulated tinnitus subjects were simultaneously presented with ongoing narrowband noise
179 on alternate blocks ('tinnitus on' condition). This noise had the spectrum of the tinnitus
180 match of the acute or chronic tinnitus subject with the closest hearing thresholds at
181 frequencies adjacent to their tinnitus frequency. To prevent the non-representative scenario
182 of the stimuli and 'tinnitus' being perceptually identical, the bandwidth for simulated pure
183 tone tinnitus was set to 1/40 octave. Intensity of the noise stimulus was set at the tinnitus
184 match intensity initially, and the subject was asked to adjust the intensity, if necessary, to
185 ensure it was loud enough to be audible over quiet speech, and quiet enough to not prevent
186 a normal volume conversation. Such adjustments were not required in most cases.

187

188 **EEG data processing**

189 Data analysis was performed in Matlab, using the FieldTrip toolbox. EEG data were recorded
190 at 1024 Hz, downsampled to 256 Hz and high-pass filtered from 0.3 Hz. Data were re-
191 referenced to combined P9/P10, roughly corresponding to M1 and M2 locations. Bad
192 channels were identified visually and reconstructed by interpolation. Data were epoched
193 between -0.5 and 1 s peristimulus time, with demeaning and detrending. Epochs with
194 grossly outlying maximum amplitudes, based on visual inspection, were excluded, followed
195 by removal of ocular and muscle artefacts using independent component analysis (ICA). A
196 mean of 23 components was removed per subject, with no significant difference in the
197 number of components removed between tinnitus and control groups. Epochs were
198 baseline corrected to -100-0 ms peri-stimulus time, and each epoch was summarised by four
199 values derived from its (normalised within channel) time series: largest absolute amplitude
200 in any channel at any time point; largest mean absolute deviation across channels at any

201 time point; largest mean absolute amplitude across time at any channel; largest mean
 202 absolute amplitude across time and channels. Histograms were plotted of the four values,
 203 and thresholds for trial rejection specified manually based on the point where the upper tail
 204 deviates from a normal distribution. Epochs were rejected if any of their four values
 205 exceeded its threshold, and approximately 10% of trials were rejected for each subject.
 206 Visual inspection of a subset of epoch waveforms confirmed that this method removed bad
 207 epochs successfully. Surviving epochs were averaged within their respective stimulus
 208 conditions, followed by low-pass filtering at 35 Hz.

209 Based on evoked peak topographies observed in pilot experiments, FCz was chosen as the
 210 sole channel from which to present time-domain data, and three time windows were
 211 determined that maximally captured the three deflections characterising the evoked
 212 response. The mean evoked potential within each time window was taken as the basis for
 213 statistical analysis.

214 Because we had no hypothesis about MMN latency, the duration of MMN responses were
 215 relatively long, and there were no clear differences in MMN latency, we did not subject
 216 MMN latency to any formal analysis. The primary outcome measure was MMN amplitude,
 217 with MMN-timeframe response magnitudes to standards, and N1 and P50 magnitudes as
 218 secondary outcome measures.

219

220 **Statistical analysis**

221 Statistical analysis was performed in Matlab. On account of Lillefort's test not indicating
 222 more datasets deviating from a normal distribution than expected by chance, ANOVA was

223 used as the basis for statistical analysis. For comparison of chronic tinnitus subjects and
 224 controls, a three-way ANOVA with full interaction terms was applied, with group (tinnitus or
 225 control), frequency (edge or centre) and intensity (low or high) as the factors of interest. As
 226 the acute tinnitus group was not matched to a control group, it was subject to a two-way
 227 ANOVA, with interaction term, with frequency and intensity as the factors of interest. The
 228 simulated tinnitus group was subject to a two-way ANOVA, with interaction term, with state
 229 ('tinnitus' on or off) and intensity as the factors of interest. Each ANOVA was performed
 230 separately on standards and deviants (deviants minus standards). The receiver-operator
 231 characteristic (ROC) curve was generated using standard Matlab functions.

232

233 **Results**

234 **Subject characteristics**

235 Subject groups comprised 26 unselected chronic tinnitus subjects, 26 age and hearing-
 236 matched controls, 15 acute tinnitus subjects, with repeat assessment of seven of these in
 237 the chronic phase, and 20 healthy controls studied with and without the simultaneous
 238 presentation of simulated tinnitus based on tinnitus subjects' psychophysical tinnitus
 239 matches. Their characteristics, along with their individual tinnitus matches and derived
 240 stimulus parameters, are summarised in Table 1. Due partly to prioritising audiometric
 241 matches at the stimulus frequencies, there were significant differences, between chronic
 242 tinnitus and matched control groups, in sex and stimulus intensity. The latter may have
 243 reflected the matching procedure, or (appropriate) compensation for hyperacusis in the
 244 tinnitus group. Stimulus loudness at the tinnitus edge frequency was, on average, higher in

245 the control than chronic tinnitus group (Table 1), but overlap between groups was high. To
 246 ensure that this did not lead to spurious results, we repeated the primary analysis after
 247 excluding the six tinnitus subjects with the lowest stimulus intensities (in dB SL) at the edge
 248 frequency; this balanced the group means for the edge frequency stimulus intensity (41.0
 249 vs. 42.7 dB SL, $p = 0.75$), and increased the statistical significance of the main finding
 250 (discussed in its respective section) from $p = 0.0009$ to $p = 0.0001$. The inclusion of
 251 unselected tinnitus subjects, including those with severe high-frequency hearing loss, older
 252 volunteers, and both tonal and narrowband noise types of tinnitus, potentially may have
 253 added noise and variance to the data, but we considered this inclusivity important to prove
 254 the applicability of any findings to the broader tinnitus population as opposed to a particular
 255 subset.

256

257 **Spatiotemporal organisation of stimulus response**

258 In a roving MMN paradigm (Figure 1), with isochronous 300ms pure tones matched to either
 259 the centre frequency or lower edge (subjectively defined as ‘just outside’ the tinnitus sound)
 260 of the tinnitus frequency band as the stimuli, and stimulus intensity as the roved parameter,
 261 the event-related potential was characterised (Figure 2) by approximately equally sized P50
 262 and N100 responses, and a prolonged late negative potential, peaking at 200-450ms in
 263 keeping with the timeframe of mismatch negativity (MMN). This is long for MMN in general,
 264 but we note that the one study to examine intensity deviants in tinnitus showed later
 265 responses to these than other deviants, in keeping with what we observed here.
 266 Furthermore, it is recognised that smaller perceptual changes are associated with later
 267 MMN responses (17).

268

269 **Early auditory evoked potentials (P50 and N100) are unaffected by tinnitus**

270 There were no differences in standard or deviant P50 responses related to subject group,
271 stimulus frequency or stimulus intensity. In a three-way ANOVA (subject group, stimulus
272 frequency, and stimulus intensity), N100 response magnitudes to standard stimuli showed a
273 main effect of larger responses to high intensity stimuli ($p < 0.05$), which was an expected
274 and trivial finding. An equivalent analysis of deviant-minus-standard responses showed a
275 main effect of larger responses to the tinnitus edge (lower) than tinnitus centre (higher)
276 frequency ($p < 0.005$). The lack of differences between tinnitus and control groups in these
277 early responses makes simple acoustic differences in stimuli, such as loudness, an unlikely
278 explanation for the tinnitus-related changes described below.

279

280 **Tinnitus-irrelevant duration deviants**

281 To exclude broad differences in predictive processes not specifically related to tinnitus or
282 the underlying hypothesis, we incorporated occasional shorter 150 ms stimuli to serve as
283 duration deviants. Duration deviants, in the absence of intensity changes, elicited clear
284 MMN responses, which showed no significant differences on account of stimulus frequency
285 or intensity, or subject group.

286

287 **Late (MMN timeframe) responses to standard stimuli show small differences due**
288 **to tinnitus**

Standard responses in the MMN time window showed a main effect of being larger for high as opposed to low intensity stimuli ($p < 0.005$), which was expected. As shown in Figure 3A, there was a group x frequency interaction ($p < 0.05$), whereby the control group, but not the tinnitus group, had larger responses to the lower (edge) frequency standards.

Asymmetry of MMN responses to intensity deviants differentiates tinnitus subjects from controls

There was a main effect of larger deviant minus standard responses to the lower (edge) than higher (centre) frequency ($p < 0.0001$). This mirrored the equivalent difference seen in the N1 responses to deviants, and is likely to be for the same reason. As shown in Figure 3B, our principal finding was in line with our hypothesis, in that there was a group x direction interaction ($p < 0.001$), whereby tinnitus subjects had larger responses to upward deviants (minus standards), while matched controls had larger responses to downward deviants (minus standards). The effect, which we term Intensity Mismatch Asymmetry (IMA), applied to both tinnitus centre and tinnitus edge frequencies but, in keeping with the main effect of frequency, the absolute effect appeared larger at the edge frequency, though the contribution of frequency to this interaction was not statistically significant. Repeating the analysis after excluding the six tinnitus subjects with the least intense edge frequency stimuli (in order to balance mean intensity with the control group) showed the same finding, but with the greater level of statistical significance of $p = 0.0001$.

To assess whether IMA can serve as a biomarker for tinnitus, we used the simple metric (averaged across stimulus frequencies) of upward deviants (minus standards) minus downward deviants (minus standards). Figure 4 shows the receiver-operator characteristic

312 (ROC) curve for this metric, which results in an area under the curve of 0.77, indicating the
 313 favourable end of 'fair' diagnostic accuracy. We aimed to avoid the use of a more
 314 complicated classifier metric, which might have produced greater accuracy, to constrain our
 315 findings to those that might be ported directly to animal studies. No significant linear
 316 correlations were observed between this metric and either THI or VAS loudness score.

317

318 **Tinnitus-related MMN changes are present in the acute, as well as chronic, stages**

319 We have previously hypothesised that there is a window of reversibility following initial
 320 tinnitus onset, before the tinnitus prediction becomes pervasive, though the length of this
 321 window would be unclear, potentially ranging from a scale of days to months. In a 2-way
 322 ANOVA (intensity and frequency), the group of 15 subjects with new-onset tinnitus (usually
 323 within the past 3-4 weeks) showed a main effect of upward intensity deviants yielding larger
 324 MMN responses than downward deviants ($p < 0.05$).

325

326 **Absence of equivalent changes in simulated tinnitus**

327 The above finding of IMA could theoretically be for the reason hypothesised, that the
 328 aberrant prediction responsible for tinnitus skews sensory predictions, or for the more
 329 trivial, but still diagnostically useful, reason that the presence of *any* quiet continuous sound
 330 alongside the stimuli skews predictions towards that quiet intensity. To distinguish these
 331 possibilities, we conducted the same experiment in 20 healthy controls, with and without
 332 hearing loss, with half the blocks containing the addition of simulated tinnitus based on
 333 tinnitus subjects' matching data. To maintain a sufficient number of trials, only stimuli at the

tinnitus centre frequency were used. No significant differences were found between the 'tinnitus on' and 'tinnitus off' state; in a two-way ANOVA featuring deviant direction (up or down) and state (on or off), the p values for main effects of state and state x direction interaction were 0.81 and 0.77 respectively.

Discussion

Intensity Mismatch Asymmetry (IMA) differentiates tinnitus subjects from controls

We tested the hypothesis that development of chronic tinnitus requires formation of a pervasive 'default' prediction of a (usually quiet) constant sound within a specific frequency band, and that this prediction favours perceptual recognition of tonotopically-specific spontaneous firing in the auditory pathway as a real sound (i.e. tinnitus) rather than ignoring as noise. Processing of auditory stimuli within or close to the relevant frequency band, might be altered by skewing of all predictions towards the characteristics of the default prediction (Figure 1). We hypothesised that these skewed predictions would be detectable in MMN responses to intensity deviants around the tinnitus frequency; because downward deviations in intensity involve stimuli becoming quieter, therefore more similar to the default prediction, tinnitus subjects would show reduced response magnitudes. Conversely, upward deviations in intensity involve stimuli becoming louder, hence more distant from the default prediction, tinnitus subjects would show increased response magnitudes. Thus we hypothesised that contrast between upward and downward intensity

deviants might serve as an objective marker of tinnitus, and our results support this hypothesis in both the acute (around 4 weeks from onset) and chronic stages of tinnitus.

The IMA effect reflects tinnitus specifically

In theory, differences in MMN responses might occur simply because of an ongoing sound filling in the inter-stimulus gaps, in which case IMA would be an epiphenomenon of tinnitus, rather than a causative factor. To differentiate these possibilities, we studied 20 non-tinnitus controls with and without the simultaneous presentation of narrowband noise derived from subjects' tinnitus matches. Short-term simulated tinnitus should not alter default predictions of the kind hypothesised to underlie tinnitus, because: 1) we only presented it for around 60 seconds at a time, which would not be a long enough timescale to form pervasive default predictions; 2) not everybody would necessarily change their default prediction even after a sufficiently long duration.

The addition of simulated tinnitus within this second control group did not produce any appreciable change in MMN responses, suggesting a specific role in tinnitus.

Mechanisms potentially underlying IMA

Auditory MMN is generated by a bilateral network of primary and non-primary auditory cortex and inferior frontal gyrus (IFG). Reciprocal interaction between these centres is argued to comprise the bottom-up propagation of prediction errors, which signal discordance between prior prediction and sensory input, and the top-down updating of sensory predictions in light of this new evidence, though other explanations include sensory

377 memory, local adaptation to a stimulus and change detection. MMN amplitude is also
378 sensitive to higher level statistical structure in stimulus sequences, and therefore also
379 provides a quantitative indication of the improbability of a stimulus based on prior
380 predictions. Ventrolateral prefrontal cortex (including IFG) has been argued to form part of a
381 'tinnitus core' network, which also includes auditory, inferior parietal and parahippocampal
382 cortex (PHC). PHC has shown altered resting-state activity contralateral to the tinnitus ear
383 and resting-state fMRI correlation with auditory cortex, and based on its prominent role in
384 auditory memory is a potential source of persistent auditory predictions. While these
385 networks are likely contributors to the IMA effect we observed here, as the present study
386 does not provide source-resolved activity, it does not in itself specify the brain basis of the
387 effect. Future work might address this issue with imaging modalities with higher spatial
388 resolution.

389 MMN magnitudes might be affected by changes in central gain, including related to
390 hyperacusis, or deficient noise cancellation via frontostriatal gating which amounts to a gain
391 control mechanism. P50 suppression is often used as a marker cortical input gating, and
392 might have been expected to be a sensitive marker of any gating changes if present.
393 However, there were no differences in any evoked response magnitudes to standard stimuli
394 between tinnitus and control groups, suggesting against a straightforward gain or
395 hyperacusis-related explanation. There are, however, more nuanced aspects of gain, such as
396 dynamic range adaptation, and so we cannot altogether rule out changes in gain in the
397 broader sense as a contributory factor.

398 We attempted to standardise attention by having all subjects watch a subtitled movie they
399 found engaging, and all subjects claimed they were able to largely ignore the auditory

400 stimuli and attend to the movie. However, this was not formally quantified, hence some
401 differences between groups cannot be ruled out. Similarly, subjects with substantial
402 tinnitus-related distress might attend more to auditory stimuli, or perceive intensity
403 increases in a more threatening way. However, we observed no correlation between
404 magnitude of IMA effect and THI score

405

406 **Previous MMN studies in tinnitus**

407 Previous MMN and equivalent studies, have varied according to the type of deviant, the
408 paradigm used, control matching for hearing loss and, importantly, whether stimulus
409 frequencies were standardised or targeted to subjects' tinnitus. Studies with non-targeted
410 stimulus frequencies have reported slightly smaller MMN responses to deviants of all types
411 tested, and minor differences in P300 oddball responses to auditory and visual stimuli. At
412 the audiometric (not tinnitus) edge frequency, tinnitus patients showed larger MMN
413 responses (in the N1 timeframe) to downward frequency deviants than hearing unmatched
414 controls, and unchanged responses one octave lower. Frequency deviants, with the deviant
415 at the tinnitus match frequency, and the control frequency 10% different, have been found
416 to be increased compared to controls, with partial resolution of the difference following
417 successful tinnitus retraining therapy. Using standardised stimulus frequencies around 8 kHz
418 (irrespective of tinnitus frequency), smaller MMN responses were observed in tinnitus
419 patients with high levels of distress only. These studies set a precedent for there being small
420 differences in sensory, mnemonic and/or predictive processing relevant to the MMN in
421 tinnitus. Our present study is the first to feature intensity deviants targeted to the tinnitus

422 frequency, and as such our results show a much stronger effect, and may provide a way
423 forward for this specific field in tinnitus research.

424

425 **Potential use as a biomarker**

426 Successful animal research into tinnitus mechanisms and treatments requires knowing
427 which animals experience tinnitus. Numerous methods have been developed to determine
428 this, and broadly fall into two categories. Conditioned behaviour models are often regarded
429 as the more accurate, and require lengthy prior training of animals to perform or refrain
430 from certain behaviours, such as licking, during the presence of an ongoing sound.
431 Automatic response methods have the advantage of requiring no training, and exploit
432 involuntary responses, such as the acoustic startle response, in conjunction with stimuli
433 related to the possible tinnitus (such as a short gap in an ongoing pure tone) to modify this
434 depending on tinnitus status, but are subject to caveats and controversies, and show
435 inconsistent replicability in humans. The two types of approach have shown limited
436 correlation with each other, and with the presence or absence of an auditory insult
437 potentially sufficient to induce tinnitus. However, because there is no gold standard in
438 animals against which to test the sensitivity and specificity of a diagnostic tinnitus test, the
439 performance of these measures remains unquantified. Potential biomarkers derived from
440 human tinnitus studies have mainly focused on whole-brain resting-state imaging of
441 electrical activity or large scale correlations in cerebral blood flow, but these measures are
442 inherently non-transferrable to animals. The IMA technique, as reported here, has the
443 potential to constitute a diagnostic test that is quantifiable in its diagnostic performance, on
444 account of being developed in humans, applicable across species, free from training

445 requirements and quick to perform. The presence of the IMA effect even just outside the
446 tinnitus frequency suggests that its success does not depend upon highly specific tinnitus
447 matching. Another recent study has had the same aim, based on quantifying the acoustic
448 change complex, an evoked response to a change during a stimulus. It yielded only slightly
449 lower ROC performance, but we note that the study was subject to numerous limitations,
450 including only yielding this result at uncomfortably loud stimulus levels, and excluding
451 subjects who were older or had significant hearing loss. Although there are a number of
452 factors to address in follow-up studies (e.g. tuning curves over stimulus frequency and
453 intensity, optimising stimulus timing and duration, standardised diagnostic cut-offs), we
454 believe the IMA technique might have the potential to serve as a convenient and robust
455 biomarker for future animal studies of tinnitus.

456

457 **Parallels with other perceptual disorders**

458 Predictive coding accounts of perception, are popular in neuroscience, and our predictive
459 coding tinnitus model joins other predictive coding models of tinnitus, and other
460 pathological perceptual states including chronic pain, musical hallucinosis, psychosis, and
461 functional neurological disorder. These theoretical models generally lack support by
462 measurement of the pathological predictions themselves. Here, we demonstrate proof of
463 concept that pathological predictions can be measured using cheap, widely-available tools.
464 As it shares many parallels with tinnitus, chronic pain would be a logical condition to extend
465 this approach to next.

466

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591 Figure legends

592 **Figure 1:** Experimental hypothesis and paradigm. The paradigm is a roving mismatch
 593 negativity (MMN) paradigm, with 300ms pure tones (black bars) interspersed with 300ms
 594 intervals. Stimulus frequency is matched to within or adjacent to the individual tinnitus
 595 frequency band. Intensity is the roved parameter, between 0 and -6 dB relative to an
 596 individualised reference intensity (R). We hypothesised that control subjects would make
 597 optimal predictions of upcoming stimuli (blue line) based on recent stimulus history, the
 598 presence of a tinnitus prediction (T and grey line) would result in tinnitus subjects forming
 599 an intermediate prediction (red line) between the optimal stimulus-based prediction and
 600 the tinnitus prediction. This would result in an asymmetry between MMN responses to
 601 upward and downward intensity deviants in tinnitus subjects (red arrows) compared to
 602 controls (blue arrows). Note that many aspects of stimulus sequences are predicted, but
 603 illustrated predictions here refer only to the intensity of the next upcoming stimulus. Also
 604 note that because control subjects' default prediction is of no sound at all, rather than an
 605 auditory percept (such as tinnitus) but with zero intensity, this does not impact the
 606 predicted intensity of upcoming stimuli.

607

608 **Figure 2:** Spatiotemporal distribution of evoked responses. (A): group mean scalp
 609 topographies within colour-coded time windows capturing the three dominant waveforms.
 610 Illustrative responses are shown for the high intensity standards, and upward deviant minus
 611 high standard responses, only. Std. = standard. Dev. = deviant. (B): Evoked waveforms from
 612 the FCz electrode, highlighted in red in (A), to both standard (dashed) and intensity deviant

613 (solid) stimuli at the tinnitus centre (black) and edge (red) frequencies. Grey horizontal bars
 614 indicate stimulus presentation, and coloured vertical bars indicate the colour-coded time
 615 windows corresponding to P50, N100 and MMN, as shown in (A), and forming the basis of
 616 statistical analyses.

617

618 **Figure 3:** Mismatch negativity (MMN) amplitudes in chronic tinnitus and control subjects.
 619 Bars indicate group mean and standard error. Colour coding indicates subject group, with
 620 red denoting chronic tinnitus and blue matched controls. The upper plot indicates MMN
 621 timeframe responses to standard stimuli, while the lower plot indicates MMN responses to
 622 deviant minus standard responses. Significant differences relevant to tinnitus status are
 623 indicated by p values and nested brackets, with black brackets indicating variables, or
 624 interactions, associated with significant effects based on ANOVA analyses, and grey brackets
 625 indicating variables not significantly contributing to effects. The core finding was a
 626 significant ($p < 0.001$) group (chronic tinnitus vs. control) by direction (upward vs.
 627 downward) interaction in deviant MMN responses.

628

629 **Figure 4:** Receiver-operator characteristic (ROC) curve for classification of subjects as
 630 chronic tinnitus or matched control.

631

632 **Figure 5:** Pure tone audiometry of subject groups. Plots indicate group mean and standard
 633 error at each frequency/ear. Asterisks indicate differences between chronic tinnitus (T)

634 subjects and matched controls significant at $p < 0.05$ uncorrected, which were only present
635 at frequencies remote from any experimental stimuli used.

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639 Tables

Mean (SD)	Chronic T	Control	p = (T vs C)	Acute T	Simulated T
Demographics					
Age	55.4 (13.6)	59.7 (15.3)	0.31	53.8 (12.5)	45.0 (19.1)
Sex	13F 13M	19F 7M	0.014 *	6F 9M	10F 10M
Tinnitus characteristics					
Duration	15.5 (16.7) years			4.2 (1.7) weeks	
THI	31 (28.1)			27 (23.2)	
T ear	11/15/0 L/C/R			4/8/3 L/C/R	
T character	13/13 T/N			9/6 T/N	
VAS loudness	5.0 (2.1)			4.8 (1.9)	
VAS distress	4.8 (2.9)			4.8 (2.8)	
% awareness	55.2 (34.3)			44.6 (23.7)	
T match CF (Hz)	6777 (2009)			7047 (2536)	
T match BW (oct)	0.25 (0.25)			0.17 (0.20)	
Stimulus and hearing characteristics					
Centre F (Hz)	7709 (2706)			7582 (2517)	7164 (2861)
Edge F (Hz)	5901 (1948)			6028 (2418)	
Edge F to centre F (oct)	0.37 (0.27)			0.39 (0.27)	
Edge F to match lower bound (oct)	0.078 (0.27)			0.18 (0.18)	
Thresh centre (dB)	44.8 (26.1)	37.9 (21.1)	0.19	34.3 (20.6)	20.3 (19.6)
Thresh edge (dB)	40.3 (21.1)	35.4 (17.0)	0.25	31.6 (22.7)	
SPL centre (dB)	78.1 (18.4)	78.2 (11.2)	0.99	79.5 (13.0)	79.0 (14.1)
SPL edge (dB)	72.8 (16.4)	78.9 (9.68)	0.043 *	76.3 (12.6)	
SL centre (dB)	33.3 (23.3)	40.2 (20.6)	0.15	45.2 (23.6)	58.7 (20.6)
SL edge (dB)	32.5 (20.6)	43.4 (18.3)	0.012 *	44.7 (26.8)	

640 **Table 1:** Subject, tinnitus and stimulus characteristics. Numbers inside and outside of
641 parentheses indicate mean and standard deviation, respectively, unless otherwise indicated.

642 T = tinnitus. C = control. THI = Tinnitus Handicap Inventory. VAS = visual analogue scale. CF =
643 centre frequency. BW = bandwidth. Oct = octaves. Thresh = hearing threshold (at specified
644 frequency). SPL = sound pressure level (of stimulus). SL = sensation level (of stimulus). L/C/R
645 = left (predominant)/centre/right (predominant). T/N = tonal/narrowband noise. F = female.
646 M = male. * indicates $p < 0.05$. Shaded cells indicate measures not applicable to particular
647 groups.

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